

AWARD NUMBER: W81XWH-15-1-0118

TITLE: Antimicrobial Silk Ocular Drug Delivery Implant for Chronic Posterior Segment Diseases

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REPORT DATE: June 2016
~~October 2016~~
~~October 2016~~

TYPE OF REPORT: Annual Technical Progress Report

PREPARED FOR: U.S. Army Medical Research and Materiel Command
Fort Detrick, Maryland 21702-5012

DISTRIBUTION STATEMENT: Approved for Public Release;
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REPORT DOCUMENTATION PAGE					Form Approved OMB No. 0704-0188	
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PLEASE DO NOT RETURN YOUR FORM TO THE ABOVE ORGANIZATION. 15 May 2015 - 14 May 2016						
1. REPORT DATE (DD-MM-YYYY) June 2016 01/09/2016		2. REPORT TYPE Annual Technical Progress Report		3. DATES COVERED (From - To) May 2015 August 2016		
4. TITLE AND SUBTITLE Antimicrobial Silk Ocular Drug Delivery Implant for Chronic Posterior Segment Diseases				5a. CONTRACT NUMBER		
				5b. GRANT NUMBER W81XWH-15-1-0118		
				5c. PROGRAM ELEMENT NUMBER		
				5d. PROJECT NUMBER		
6. AUTHOR(S) David L. Kaplan, Irmgard Behlau email: david.kaplan@tufts.edu				5e. TASK NUMBER		
				5f. WORK UNIT NUMBER		
7. PERFORMING ORGANIZATION NAME(S) AND ADDRESS(ES) Tufts University 4 Colby Street Medford, MA 02155				8. PERFORMING ORGANIZATION REPORT NUMBER		
9. SPONSORING/MONITORING AGENCY NAME(S) AND ADDRESS(ES) US Army Medical Research and Materiel Command Fort Detrick, MD 21702				10. SPONSOR/MONITOR'S ACRONYM(S)		
				11. SPONSOR/MONITOR'S REPORT NUMBER(S)		
12. DISTRIBUTION/AVAILABILITY STATEMENT Approved for Public Release, Distribution Unlimited						
13. SUPPLEMENTARY NOTES						
14. ABSTRACT An intracocular insert based on silk fibroin was designed and optimized. The insert contains a hollow channel that was preloaded with the anti-VEGF antibody bevacizumab. The device was covalently coated with the antibacterial polymer HMPEI to protect against biofilm formation and the transmission of harmful bacteria to the interior of the ocular chamber. The device is first of its kind to be designed for sustained release of a large-molecule drug into the vitreous humor for the prevention of posterior segment diseases such as diabetic retinopathy and age-related macular degeneration. An in vitro model and an in vivo rabbit eye model were developed for determining the release profile of the therapeutic antibody from the device. Through the combination of the aqueous processing of a naturally occurring biodegradable protein (fibroin) into the device mold, antibacterial chemical modification of the device exterior, and the optimization of the delivery medium, the present system offers a compelling alternative to the standard-of-care for the treatment of posterior segment diseases.						
15. SUBJECT TERMS Silk, drug delivery, intraocular implant, eye, diabetes, chronic posterior segment diseases, antimicrobial, ocular, sustained release						
16. SECURITY CLASSIFICATION OF:			17. LIMITATION OF ABSTRACT		18. NUMBER OF PAGES	
a. REPORT U	b. ABSTRACT U	c. THIS PAGE U	UU		11	
19a. NAME OF RESPONSIBLE PERSON USAMRMC					19b. TELEPHONE NUMBER (Include area code)	

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Introduction:

Posterior segment diseases, e.g., diabetic retinopathy and age-related macular degeneration, are a leading cause for the loss of sharp visual acuity for patients in the U.S. and worldwide, especially in the elderly population. Most of these diseases are associated with the formation of aberrant blood vessels in the posterior segment, especially in the macula. A promising treatment for tackling some of these diseases involves the release of an anti-VEGF antibody, such as bevacizumab, into the vitreous humor to prevent the formation of such blood vessels. For the present project, a protein-based biodegradable drug-delivery system was developed for the sustained release of bevacizumab into the vitreous humor. The system comprises an intraocular insert with antibacterial coating with the drug loaded in a hollow channel within. The design of the device was optimized and a protocol for the surgical insertion of the device into rabbit eyes was developed. The device was proven to be biocompatible and mechanically robust.

Keywords

Silk; fibroin; diabetic retinopathy; macular degeneration; HMPEI; rabbit model; bevacizumab.

Accomplishments

The major goals for the projects as stated in the SOW were: (a) “design of a refillable and long-term intraocular silk-based device for the delivery of anti-VEGF drugs to the posterior eye”, (b) “Silk Drug Delivery Implant Design”, (c) “In vitro Silk-based anti-VEGF Drug Delivery and Pharmacokinetic Studies”, (d) “Development of an antimicrobial, N,N-hexyl, methyl-polyethylenimine (HMPEI) derivatized intraocular silk drug delivery implant”, (e) “Maximization of HMPEI-bound silk surface area, host cell biocompatibility, and antimicrobial efficacy”, (f) “HMPEI-silk implant mechanical stability and in vitro drug release studies”, (g) “Assessment of the anti-VEGF HMPEI-silk drug delivery implant system in the rabbit in vivo”, (h) “Assessment of the anti-VEGF HMPEI-silk drug delivery implant system in normal pigmented rabbit models in vivo”, and (i) “Assessment of the anti-VEGF HMPEI-silk drug delivery implant system in a diabetic retinopathy rabbit models in vivo”. In the following paragraphs, our progress towards these goals are described.

1. After numerous iterations, we developed the format of the intraocular implant (a silk-fibroin-based hollow gel-spun tube) and the format of the drug-delivery medium (a silk fibroin based lyophilized hydrogel). **Figure 1** depicts the dimensions and the make-up of the device. Spinning a concentrated 15 % (w/v) silk solution over a steel wire (diameter = 500 μ m), then lyophilizing it yielded a silk tube with consistent inner diameter. Then the silk tubes (still wrapped around the steel wire) were submerged in methanol for 1 h to induce β -sheet formation. Then the tubes were separated from the wire by sliding the tubes over the wire. The gel-spun tube was then cut into smaller pieces (5 mm in length). Although the inner diameter of the device is fixed by the outer diameter of the steel wire, the outer shape of the device is determined by the deposition pattern of silk solution. Instead of a uniform outer surface, we chose to prepare a peanut-shaped device for ease of placing the device into the target organ. The device is based on a single format and has thus no junctions that may affect the mechanical integrity. The device has a consistent and well-defined delivery channel for storing the drug-releasing material.

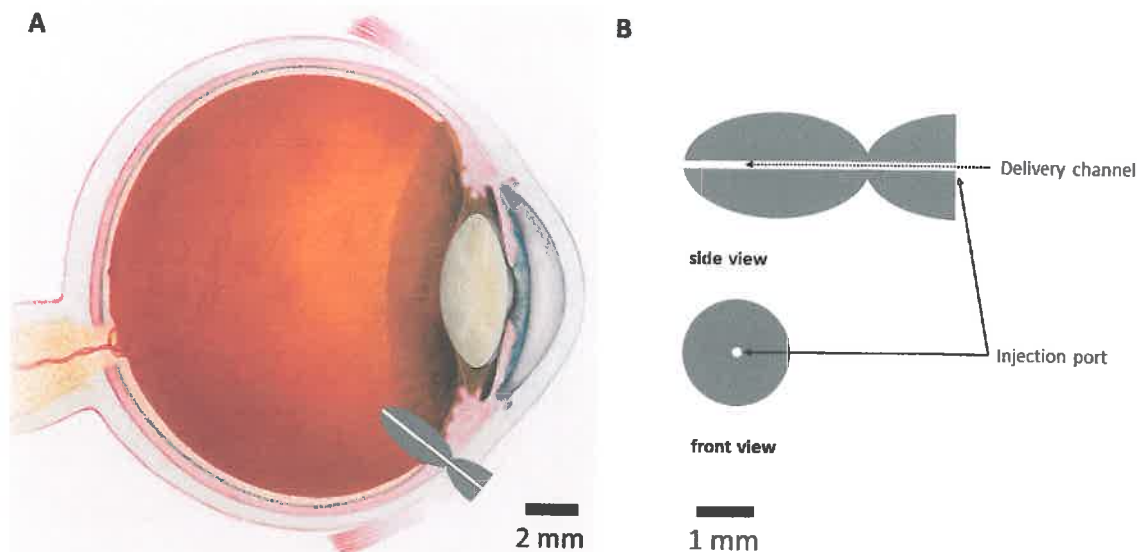


Figure 1. Cartoon depiction of the silk-based intraocular device. (A) The placement of the device into the intraocular space through *pars plana*. The graphic of the eye has been adapted from an image by National Eye Institute: <https://www.flickr.com/photos/nationaleyeminstitute/7544656020/in/album-72157646829197286/> (Creative Commons 2.0 license). (B) Detailed view of the device (4-5 mm long) from side and front.

2. Silk fibroin in the device was successfully functionalized covalently with the antimicrobial polymer N,N-hexyl,methyl-polyethylenimine (HMPEI) in three steps. The chemical reactions involved are depicted in **Figure 2**. Briefly, the devices were placed in borate buffer at 0°C and diazonium salt solution (prepared from 4-aminobenzoic acid, p-toluenesulfonic acid and sodium nitrite solution) was added to it. The samples turned bright orange. The samples were washed with distilled water and air-dried. Next, the devices were placed in a solution of 217 kDa polyethylenimine (PEI) in aqueous dimethylformamide. We then added 1-hydroxy-benzotriazole (HOBT) and N-(3-dimethylamino)propyl-N'-ethylcarbodiimide (EDC) to promote the formation of amide linkage between the polymer and the sponge surface tyrosine residues. The resulted sponges were washed and reacted with a mixture of 1-bromohexane, trimethylamine, and t-amyl alcohol. Finally, the samples were washed and added to a mixture of t-amyl alcohol and iodomethane to complete the formation of positively charged quaternary ammonium groups in the polymer chains, resulting in HMPEI-functionalized azo-silks. No difference in color was observed between the azo-silk and HMPEI-azo-silk devices (both were bright orange). A few photographs of the device are shown in **Figure 3**.

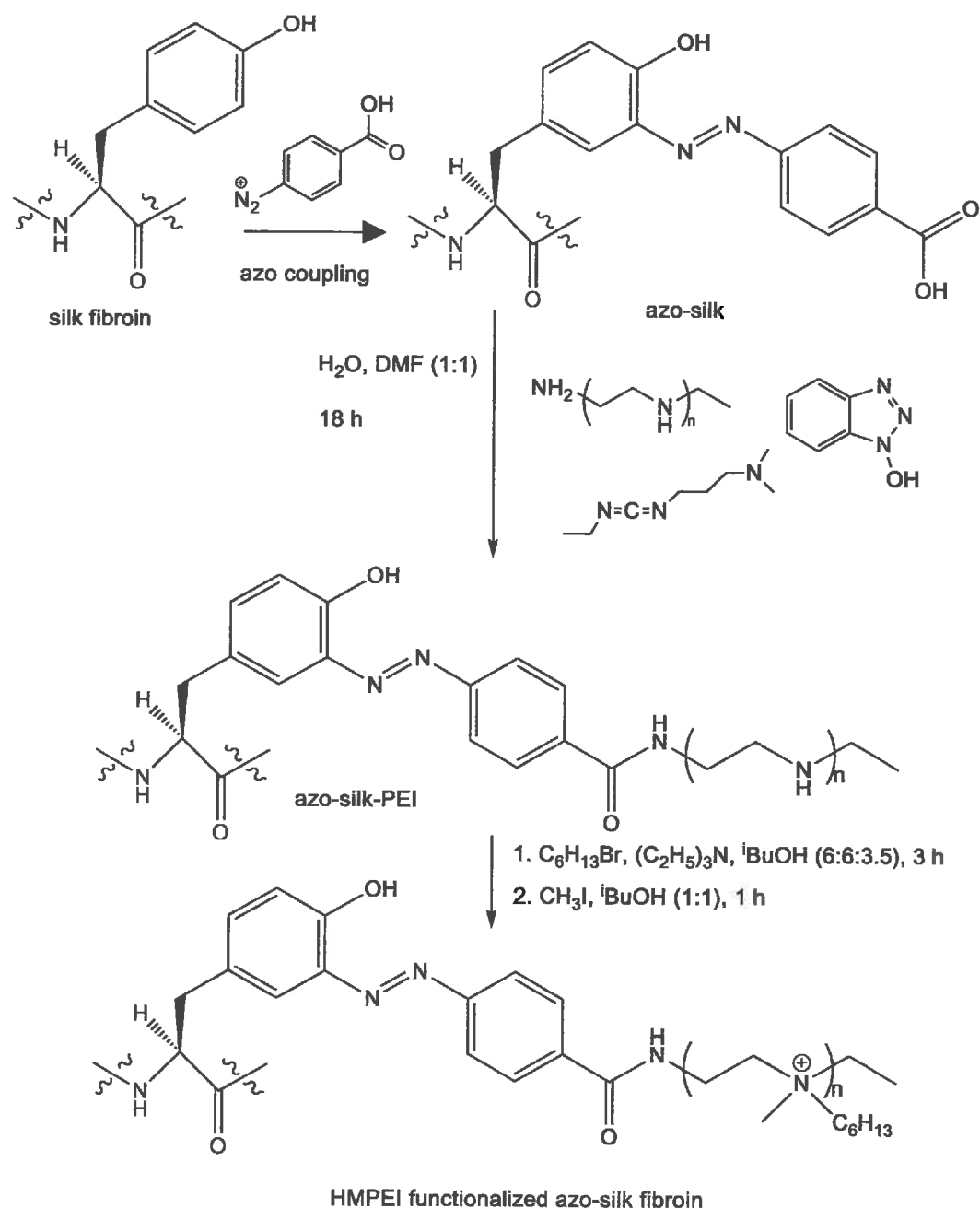


Figure 2. Three-step chemical functionalization of the silk fibroin-based device. The functionalization takes place on the exposed tyrosine residues in the silk protein.

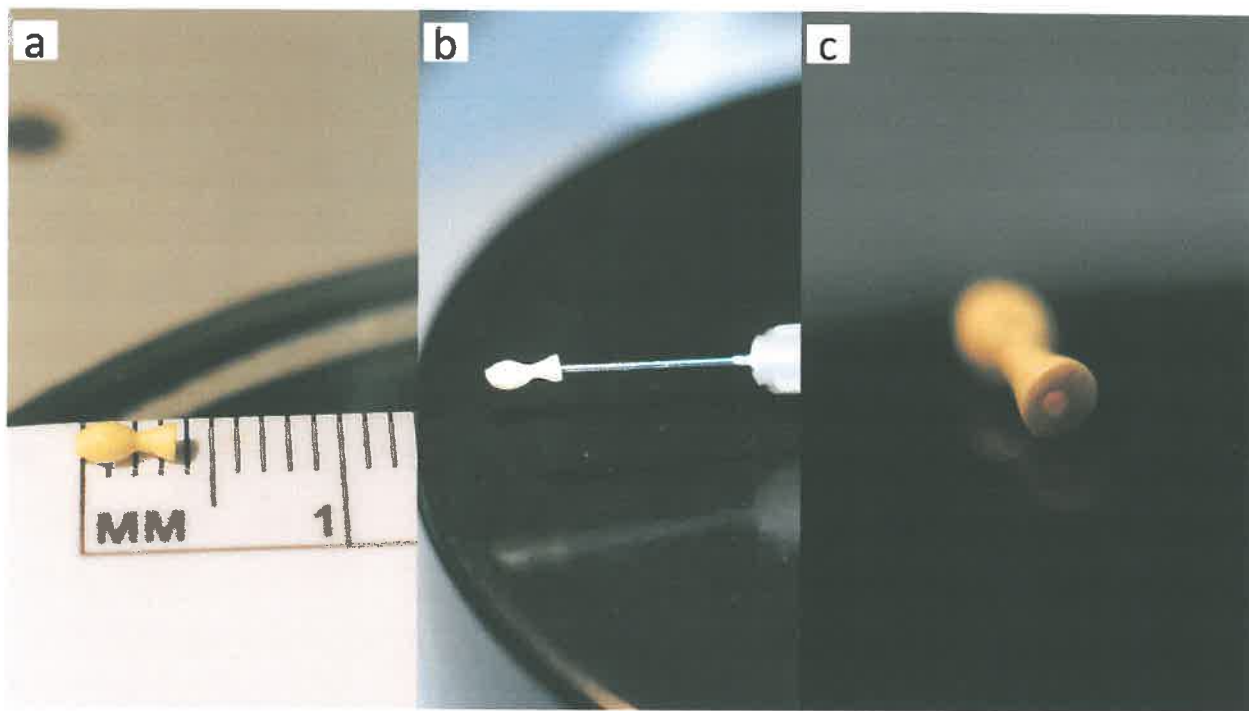


Figure 3. Photographs of the silk-based device after chemical functionalization and before loading the anti-VEGF drug, bevacizumab.



Figure 4. SEM image of the vertical section of the device, showing the inner channel.

3. By scanning electron microscopy (SEM), the change in morphology of the device surface and interior channel in response to the covalent chemical functionalization was investigated (**Figure 4**). The changes in device shape, channel width, and porous structure were minimal.
4. The anti-VEGF antibody, bevacizumab, was successfully incorporated into the inner channel of the hollow device in a lyophilized hydrogel (lyogel) format. First, we pipetted out 7 mL of 4.8 % *in vivo* grade silk fibroin solution in a 50 mL falcon tube. The silk fibroin solution was then sonicated for 20 seconds. The solution remains fluid. Then 1 mL of the sonicated solution was pipetted into a 10 mL tube and lyophilized powder of bevacizumab was added such that the final concentration of bevacizumab in the silk solution was 3.75 % (w/v). The solution was mixed by pipetting up and down, until no drug powder was visible. The solution was poured onto a petri dish and the devices were dipped into the solution in an upright fashion, such that the drug-loaded solution entered the device channel by capillary action. The sonicated solution of fibroin formed a hydrogel over time (approximately 2 hours) which could be observed in 6 mL of excess silk solution that was not used for dissolving the bevacizumab. After 2 hours, the devices were put in a freezer for 3 hours and then lyophilized overnight. A separate batch of sonicated silk solution was prepared and the ends of the devices were dipped in the solution to create hydrogel plugs, thereby sealing the device. The drug-loaded devices were treated with hydrogen peroxide gas plasma for disinfection.
5. A sterilization protocol for the drug-loaded device was finalized (plasma treatment).
6. An *in vitro* drug release study was carried out from the silk lyogel into a physiologically relevant buffer (1X DPBS) at physiological temperature (37 °C).
7. An *ex vivo* implantation of the functionalized device into pig eyes was performed to determine the optimal surgical protocol to insert the device into the intraocular vitreous.

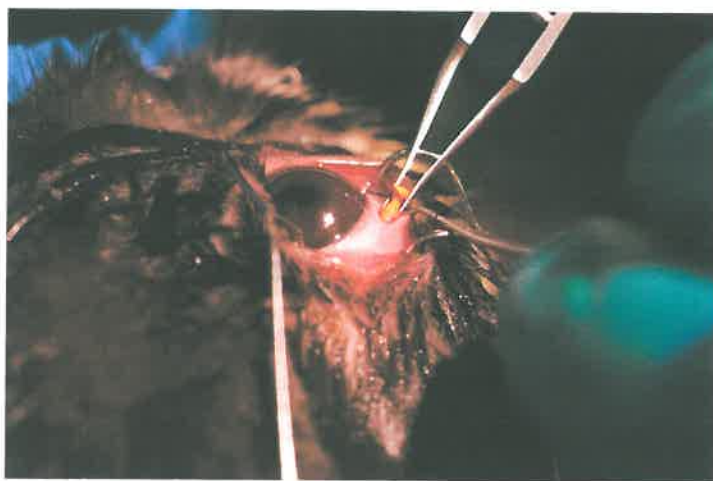


Figure 5. Surgical implantation of the drug-loaded device into rabbit eyes.



Figure 6. Use of the conjunctival flap to cover the outer surface of the device, further reducing the exposure of the device to microbes at the surface of the eye.

8. The antibody-loaded device was surgically implanted into rabbit eyes through pars plana (**Figure 5**). A conjunctival flap was used to minimize the outward exposure of the device (**Figure 6**).



Figure 7. A rabbit eye post-implantation. No sign of inflammation was observed. The yellow color of the device and the hollow inner delivery channel is apparent through the conjunctival flap.

9. Short-term (1 month) medical observation suggests that the device is biocompatible and no sign of bacterial biofilm formation was observed on the implanted device (**Figure 7**).

The current project was crucial for the professional development of Dr. Biplab Sarkar (postdoctoral training, gained expertise in design and antibacterial functionalization of drug-delivery devices) and Dr. Irmgard Behlau (presentation at a conference).

Detailed pharmacokinetic study of in vivo drug release will be reported in the next report.

Impact

The device could be a relatively easy way to administer the anti-VEGF drug into the vitreous humor of the patients and could alleviate the need for repeated injection schedule. Thus, the drug-delivery system could prevent the worsening of visual acuity for patients with posterior segment diseases. The design of the device could also be used in future as a template for the development of medical inserts/constructs with antibacterial coating. We have nothing to report at this stage on the impact on technology transfer and the impact on society beyond science and technology.

Changes/Problems

The device design was altered from the initial version proposed in the grant for ease of manufacturing as well as to improve the handling properties.

Products

Conference presentation: "Antimicrobial Silk Ocular Drug Delivery Implant for Chronic Posterior Segment Diseases", Ocular Microbiology and Immunology Group (OMIG) Meeting, October 14, 2016; Chicago, IL.

Techniques: non-uniform gel-spinning of silk fibroin, covalent antibacterial functionalization of silk fibroin.

Participants and Other Collaborating Organizations

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Funding Support:	<i>This grant</i>

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Funding Support:	<i>This grant</i>
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Funding Support:	<i>This grant</i>

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Nearest person month worked:	<i>1</i>
Contribution to Project:	<i>Dr. Kaplan had supervised all aspects of the project.</i>
Funding Support:	<i>Tufts University</i>

Special Reporting Requirements

Appendices: