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## **5. INTRODUCTION**

This research is to develop a large database of digitized mammograms that will be distributed free of charge to interested researchers. It is being funded by the USAMRMC as an infrastructure award and as such it does not represent a research project per se. That is, there is no hypothesis that we are trying to prove. Therefore, this report is structured slightly different from a normal scientific research report -- heavy on the method and light on actual results. In this project, the procedure is the most important component, which is applied continuously in a straightforward manner to achieve the goal of creating the database of mammograms.

### **5.1 Nature of the Problem**

In 1992, the National Cancer Institute identified digital mammography as an important area of research for reducing breast cancer mortality [1]. As a result, there has been a sharp increase in the number of researchers developing computerized methods for analyzing mammograms. This is due in part to the substantial potential benefit from developing an automated computerized system for assisting radiologists in interpreting mammograms. With a large number of investigators developing computerized analysis techniques, the likelihood of an accurate method being developed is high. Unfortunately, a major obstacle to rapid progress in developing a technique is that each investigator uses his or her own set of mammograms (database) to develop and evaluate the performance of his or her technique. As a result, it is not possible to compare the accuracy of different methods because the measured performance is dependent on the cases used for testing [2]. For example, by using "easy" cases for testing, a computer technique would apparently have a higher accuracy than if "hard" cases were used. A common database of mammograms that could be used by all investigators in the field would solve this problem.

### **5.2. Background: Previous work in the field**

At a Biomedical Image Processing meeting held February 1993, in San Jose CA, 12 panelists discussed the design of a common database for research in mammographic image analysis [3]. Two of the panelists are investigators on this proposal. Important considerations in developing the database are: (a) the cases selected, (b) the digitizer used, (c) organization of the database, (d) associated information to be included with images, (e) "truth" for each case, (f) format of image files, (g) distribution of the database, and (h) rules on using the database.

There have been several small databases released for general use. However, all have several limitations due to insufficient spatial resolution, insufficient grey-scale resolution, and/or too small a number of cases. The database that we are developing will have none of these limitations. There is now underway the development of another mammographic database. This database differs from the one being developed in this project because a smaller pixel size is being used and they are not including previous films as is being done in this project. While it may seem that a smaller pixel size is desirable, at spatial frequencies above 10 cycles/mm (which corresponds approximately to 50-micron pixel size), the amount of noise in the image is large compared to the amount of signal [4-6]. As a result, very little additional information is gained by digitizing at a pixel size less than 50 microns [7]. In addition, the smaller pixel size makes the amount of data excessive. At a 50-micron pixel size, a digitized mammogram is approximately 40 Megabytes (MB). A 21-micron pixel image would be 227 MB. This large increase in size adds greatly to the cost of storing, transmitting, and analyzing the images. For a 227-MB image, the end user would need at least 554-MB of computer memory (RAM) just to read in the image and manipulate it once. (This does not include the memory requirements of the operating system or the program itself.) Most computers do not have this much memory. Therefore, we believe that the large increase in cost and logistics in going to a smaller pixel size does not justify a small gain in image quality.

Furthermore, direct digital mammography systems that are currently being commercialized have pixel sizes of approximately 50 microns. This database will not be outdated when completed.

### **5.3. Purpose**

The purpose of this proposal is to develop a database of digital mammograms that can be used by researchers who (1) are trying to determine the image quality requirements of detectors for digital mammography; (2) are developing image processing techniques to optimize the displayed digital mammogram; (3) are developing computerized methods for analyzing mammograms; (4) are studying the effects of image compression methods on image quality; (5) are developing methods for remote transmission of mammograms; and (6) are studying the relationship between image quality and diagnostic accuracy. This database also could be used as a resource for teaching radiology residents and for testing the performance levels of mammographers.

The specific aims of this proposal are:

1. Collect and digitize 200 cases in each of 5 different categories, mammograms exhibiting: (i) clustered microcalcifications, (ii) masses, (iii) architectural distortions, (iv) asymmetric densities, and (v) no lesions (i.e. normals).
2. Make these cases available to other researchers either over computer network (Internet) or by sending images on computer tape or CD. The database will be distributed as widely as possible so that comparisons of different computerized analysis techniques can be standardized.

### **5.4. Method of Approach**

**Task 1:** Collect and digitize mammograms, Months 1-48. (See Figure 1.)

- a. Retrieve from film library cases with pathologically-proven lesions (clustered microcalcifications, breast masses, architectural distortion, asymmetric densities), 100 cases of each type and 100 normals (cases without lesions) from each site [University of Chicago (UofC) and University of North Carolina (UNC)] for a total of 1000 cases during the entire funding period.
- b. At each site, digitize retrieved films and outline the location of the lesion in each abnormal image. The outline will be stored together with the images but in a separate file.
- c. Send normal cases and asymmetric density cases that were digitized at UofC to UNC; and send cases containing masses, microcalcifications, and architectural distortion that were digitized at UNC to UofC.
- d. Selectively randomize 200 cases for each lesion type into one of two sets (training and testing), based on lesion subtlety. Similarly, selectively randomize 200 normal cases into two sets based on breast density.
- e. Place testing set in off-line storage and training cases in on-line storage.
- f. On average 250 cases (2500 image -- see text for details) will be done per year for 4 years for a total of 1000 cases (10,000) images.

**Task 2:** Establish protocol for transmitting database. Months 1-24

- a. Test protocols for different modes of transferring data between the UNC and UofC (FTP, 8-mm tape, and CD). A data structure designed for portability will be provided to contain the patient text data; this data structure will be made available along with the data to the requesting sites. Use of ACR/NEMA DICOM protocol will be investigated and incorporated as an optional transfer mechanism.

Task 3: Maintain database and distribute cases Months 12-48.

- a. Maintain computer, jukebox, and network connection including bug fixes and installation of vendor software updates.
- b. Distribute cases via computer network and by mass storage media (tape or CD) as requested.

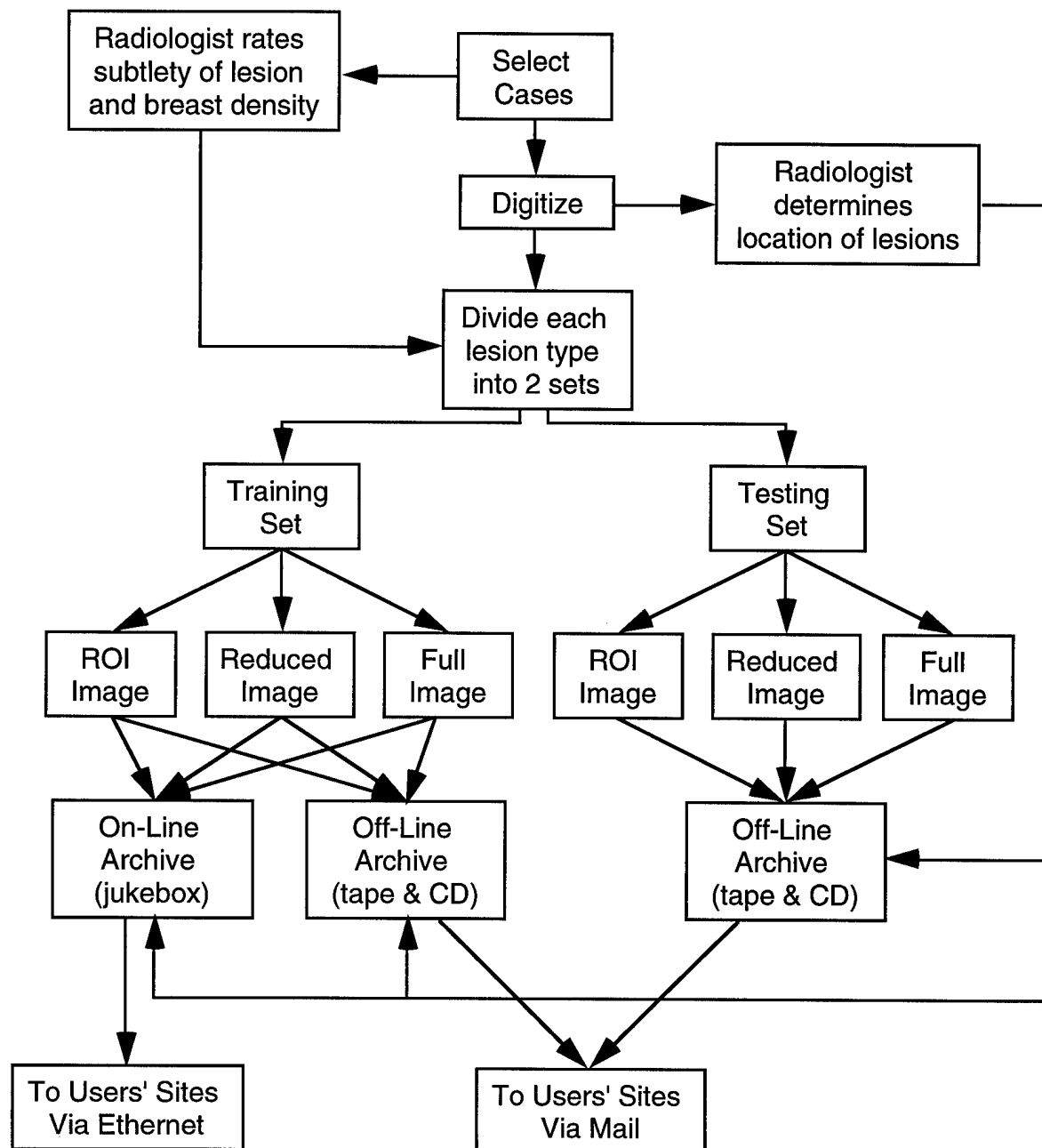


Figure 1. A flowchart of the steps required to collect, digitize, archive, and distribute the mammographic database. The 'Full Image' is the whole digitized mammogram at full resolution. The 'Reduced Image' is a minified version (reduced resolution) of the full image. The 'ROI Image' is a portion of the full image at full resolution.

## 6. PROGRESS TO DATE

### Task 1.

Last year at this time, we had digitized, classified and filed 178 cases. However, the 111 cases done at the University of Chicago (UofC) had problems. Our digitizer was sent back to the manufacturer for repairs in November. Upon return, we continued digitizing. In March, we noticed a very subtle artifact due to the digitizer. The digitizer was returned for repairs once again. The photomultiplier tube of the digitizer was replaced. The characteristics of the repaired digitizer were slightly different from the pre-repaired state. Therefore, in order to produce a consistent set of digitized images, we are in the process of redigitizing all cases from the UofC. This has delayed our anticipated first release of the database. We will accelerate our rate of digitization and case accrual to get back on schedule.

At each site, a calibrated test film is digitized daily to insure that the digitizer is within calibration. Calibration curves averaged over several repeated scans are shown in Fig. 2, for the digitizers at the two sites. The variation in calibration of the digitizer is less than 2% in the worst case. This value is less than the noise level in the image and it is also less than the variation in film optical densities between mammograms. Thus the small variation in the digitizer will have a negligible effect on the validity of the database. In addition, the calibration curves for the two digitizers are slightly different. We believe that these differences are not significant. First, where the differences are largest, at high film optical densities, very little information is present in the image, because the inherent contrast of the image is very low. Second, the differences (typically less than 0.1 in film density) are smaller than the variations from mammogram to mammogram, even mammograms from the same patient. Users of the database who may want to do precise

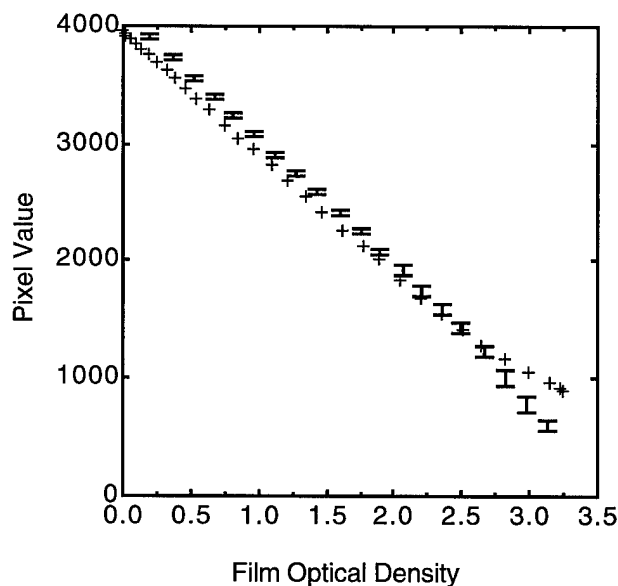


Figure 2. Calibration curves for the digitizer at the University of Chicago (crosses) and the University of North Carolina (dots with error bars). Error bars are shown only for one set of data for clarity. These types of curves are used to insure that the digitizer is stable from day to day. Also note that the digitizer output is actually proportional to film density, but the numbers have been converted by subtracting a constant (4095) from the actual digitizer output. This produces a scale that is consistent with the major laboratories working in the field, and is consistent with the digital scale used in computed tomography.

Table I. Breakdown of cases in the database as of October 1/96.

| <u>Type of Lesion</u>    | <u>Pathology</u> | <u>Subtlety</u> | <u># of Cases</u> |
|--------------------------|------------------|-----------------|-------------------|
| Mass                     | Malignant        | 1               | 19                |
| Mass                     | Benign           | 1               | 2                 |
| Mass                     | Malignant        | 2               | 12                |
| Mass                     | Benign           | 2               | 8                 |
| Mass                     | Malignant        | 3               | 11                |
| Mass                     | Benign           | 3               | 12                |
| Microcalcifications      | Malignant        | 1               | 15                |
| Microcalcifications      | Benign           | 1               | 14                |
| Microcalcifications      | Malignant        | 2               | 22                |
| Microcalcifications      | Benign           | 2               | 18                |
| Microcalcifications      | Malignant        | 3               | 19                |
| Microcalcifications      | Benign           | 3               | 21                |
| Asymmetric Density       | Malignant        | 1               | 7                 |
| Asymmetric Density       | Benign           | 1               | 0                 |
| Asymmetric Density       | Malignant        | 2               | 6                 |
| Asymmetric Density       | Benign           | 2               | 1                 |
| Asymmetric Density       | Malignant        | 3               | 3                 |
| Asymmetric Density       | Benign           | 3               | 1                 |
| Architectural Distortion | Malignant        | 1               | 6                 |
| Architectural Distortion | Benign           | 1               | 2                 |
| Architectural Distortion | Malignant        | 2               | 3                 |
| Architectural Distortion | Benign           | 2               | 1                 |
| Architectural Distortion | Malignant        | 3               | 2                 |
| Architectural Distortion | Benign           | 3               | 0                 |
| Normal                   | -                | -               | 1                 |
| TOTAL                    |                  |                 | 206               |

quantitative analysis will need to correct for the small non-linearity of the digitizer. We plan to make available the calibration curves of the digitizers.

Using the calibration curves, we were able to detect a change in calibration in our digitizer by comparing scans of the test film from before and after the repairs and thereby identify the need to redigitize all cases from that digitizer in order to produce a consistent set of images.

As of October 1, 1996, we have retrieved, digitized, classified and filed 95 cases, all from the University of North Carolina (UNC). In addition, we are redigitizing 111 cases from the UofC. These cases are tabulated in Table I. Furthermore, 46 cases have been collected and are being reviewed by the radiologist. These include lesions from all categories with the majority being masses and microcalcifications. The image subtlety has been ranked on a 5 point scale (1-5) with 1 being the most difficult to detect. All cases are archived on 8-mm tape.

The computer systems that will hold the database have been purchased and installed. Current capacity of each system is approximately 40 gigabyte (one system at each site). The total capacity of each system will be increased in the third year of the project.

## Task 2.

We originally considered the ACR/NEMA (DICOM) image format for our database. However, the ACR/NEMA format does not have a module for mammography, and it would be an extensive project to develop one at this time. Currently, then, we are storing the images as a binary

array of numbers with a simple 512-byte header. When an ACR/NEMA mammography module becomes available, it will be easy to convert our files to that format. Users of the database will be able to download ACR/NEMA converters via the internet.

We have tested transfer of images using 8-mm tape between the University of Chicago and the University of North Carolina. As expected, there were no difficulties in this mode of data transfer.

### Task 3.

Maintenance of the database and distribution of the database are at a minimum currently. These tasks will become important in the next and subsequent years as cases go "on-line".

## 7. CONCLUSIONS

The development of a common database of mammograms for digital mammography research is underway. Because of problems with our digitizer, the first release of a portion of the database has been delayed until the end of 1996. This release will include 100 cases of clustered microcalcifications.

A database of mammograms would also be useful for investigators doing research in other areas of digital mammography, such as x-ray detector development, telemammography, image compression, and image processing. For example, questions such as the required spatial resolution of a digital mammogram can be answered in part by conducting observer studies using the mammograms from the database displayed at different resolutions. Furthermore, the database would provide an excellent source of cases that could be used for teaching purposes.

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