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## Introduction

The long-term goal of our project is to develop a novel neuroprosthetic device to restore the functions of the urinary bladder for SCI people without further damaging the nervous system. Advanced technologies in electrical and computer engineering will be applied to design the novel neuroprosthetic device. Based on our previous studies [1-4], we propose in this project to use pudendal nerve stimulation (PNS) and blockade to restore both continence and micturition after SCI. Our strategy does not require sacral posterior root rhizotomy, preserves the spinal reflex functions of the bowel and sexual organs, and more importantly provides the opportunity for SCI people to benefit from any advance in neural regeneration and repair techniques in the future. During the last year, we have identified problems of our implantable stimulator in awake chronic SCI animals, improved the stimulator design, and tested its functionality in anesthetized animals. These results have laid the foundation for us to further test this implantable stimulator in chronic SCI animals.

## Body

During the last year, we have made significant progresses on all 3 tasks proposed in our original grant applications. Task #1: Design and develop an implantable stimulator to activate and/or block the pudendal nerves. Task #2: Test the implantable stimulator in awake chronic SCI animals. Task #3: Data analysis and publishing the results.

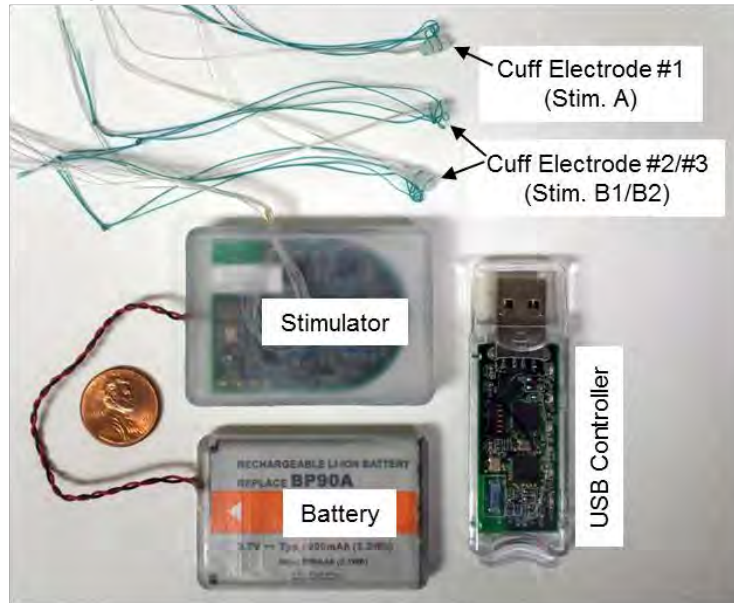
### Task #1: Design and develop an implantable stimulator to activate and/or block the pudendal nerves

During the last year, we have implanted the first prototype of our implantable stimulator in another 2 awake chronic SCI cats. However, we encountered problems including: 1. failure to recharge the battery in one animal; 2. failure to block the pudendal nerve and failure to recharge the battery in another animal. We found that the charging circuit of the stimulator could generate heat to increase the surface temperature of the Li-ion rechargeable battery to about 45 °C. At this temperature, most Li-ion rechargeable battery will be damaged. To fix this problem, we have re-designed the packaging method so that the stimulator circuits and the rechargeable battery were separately packaged (see Fig.1A). We also found that the failure to block the pudendal nerve was due to the interaction between the low frequency and the high frequency channels, because we used a single cuff electrode with 5 leads to deliver both low and high frequency stimulations to the pudendal nerve. To solve this problem, we now used 2 separate cuff electrodes (one bipolar and one tripolar, i.e., the electrode #1 and #2 in Fig.1A) to deliver the low and high frequency stimulations and implanted the 2 cuff electrodes on the pudendal nerve at least 1 cm apart (see Stim. A and Stim. B in Fig.1B). In order to make sure that these problems are now solved, we tested the new design in 5 cats under anesthesia. These tests are mainly designed to confirm the functionality of the re-designed stimulator before we move forward to implant it in awake SCI cats for chronic testing.

Fig.1A shows a picture of the re-designed implantable stimulator (dimensions: 5.6x4.0x0.8 cm) connected to a rechargeable battery (3.7 V and 900 mAh; dimensions: 5.4x3.6x0.6 cm). The stimulator has 2 output channels providing charge-balanced rectangular pulses (1-100 Hz, 0-11 V, 0.05-0.2 ms) to the bipolar cuff electrode #1 (i.e., Stim. A in Fig.1B)

and a high frequency (5-20 kHz, 0-11 V) biphasic square waveform (see Fig.1B) to the tripolar cuff electrodes #2 and #3 (i.e., Stim. B1 and B2 in Fig.1B). The stimulator can be wireless controlled within a 2-meter distance by a USB controller that is connected to a USB port of a

### A. Implantable Stimulator



### B. Experimental Setup

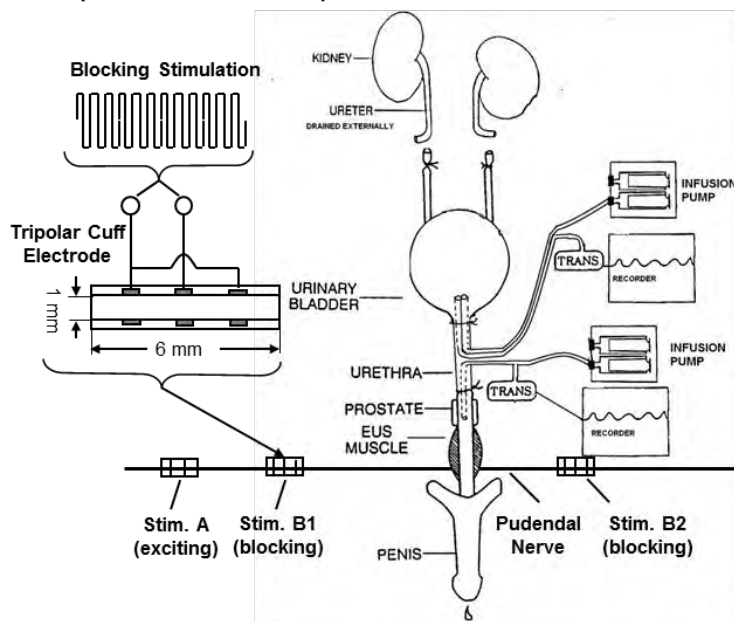


Fig.1. The implantable stimulator (A) and the locations of cuff electrodes implanted on the pudendal nerves in the cat (B). EUS – External Urethral Sphincter.

portable computer (the computer is not shown). The computer software can set stimulation parameters for each output channel and turn on/off each channel by wireless communication between the implanted stimulator and the USB controller. The stimulator and battery are implanted underneath the skin on the left side of the lower back of the cat along the sacral spine. The battery can be charged by the charging circuitry in the stimulator that can be powered wirelessly across the skin by an external charging coil. At the beginning of each experiment, the battery was fully charged from 2.8 V to 3.7 V in about 15-20 minutes and it could run for the entire experiment (5-6 hours) with repeated stimulation. After removing the stimulator and battery from the animal at the end of experiment, the battery power lasted for about 2-3 days before the stimulator stopped functioning and lost communication with the USB controller due to a low battery level (<2.8 V). Although the stimulator was not used to stimulate/block the pudendal nerve once it was removed from the animal, it is estimated that the battery should still be able to power the stimulator for the same amount of time (2-3 days) if it were used for PNS/block. This is because the electrical power used by PNS/block is only a very small portion of the total power consumption by the electrical circuits including wireless communication, microprocessor, and the output amplifiers. Therefore, it is expected that the implantable stimulator will continuously function after chronic implantation in SCI cats as long as we continue to charge it for 15-20 minutes every day.

A total of 5 cats were used to test this stimulator under anesthetized condition. Fig.1B shows the experimental setup. The temperature of the animal was maintained at 35 °C to 37 °C using a heating pad. The ureters were cut and drained externally. A double lumen catheter (5F)

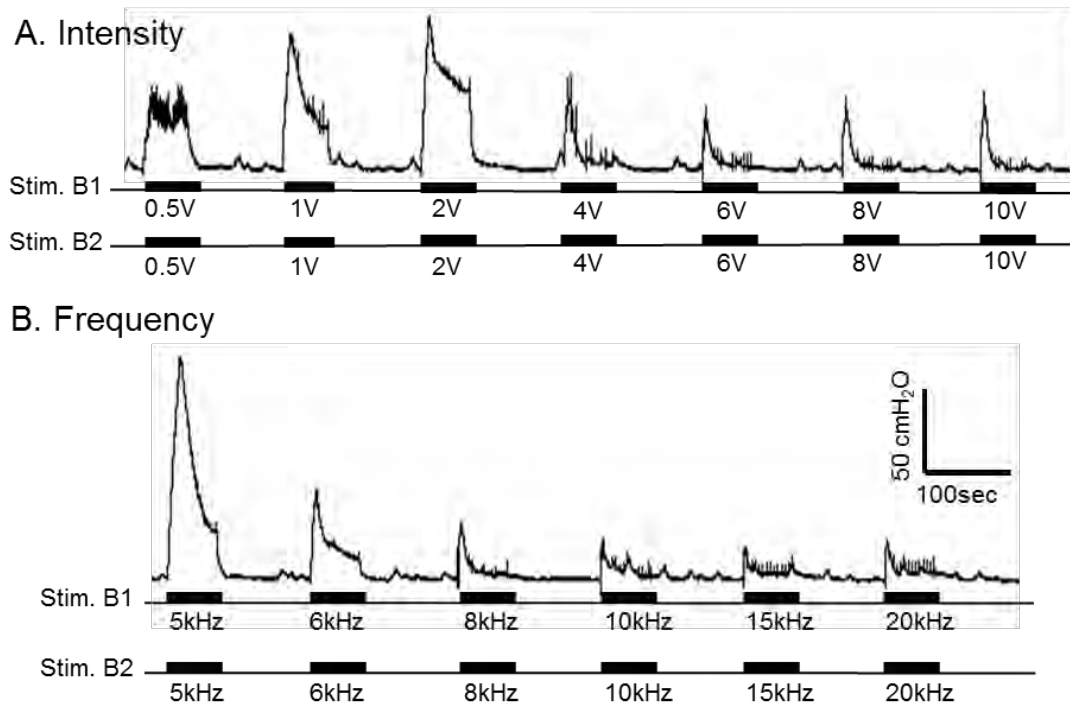


Fig.2. Urethral pressure induced by the high frequency biphasic electrical stimulation applied bilaterally on the pudendal nerves. A. Different intensities at 10 kHz frequency. B. Different frequencies at 6 V intensity. The urethral infusion rate is 1 ml/min. The black bars under the pressure traces indicate the stimulation duration.

was inserted into the bladder through a small incision in the proximal urethra and secured by a ligature (Fig.1B). One lumen of the catheter was attached to a pump to infuse the bladder with saline, and the other lumen was connected to a pressure transducer to monitor the bladder activity. Another catheter (5F) was also inserted at the same site in the proximal urethra but directed toward the distal urethra and secured by a ligature (Fig.1B). This catheter was attached to an infusion pump and to a pressure transducer via a T connector. The pudendal nerves were accessed posteriorly in the sciatic notch lateral to the tail. The three cuff electrodes (NCE112/113, MicroProbes Inc., Gaithersburg, MD) as shown in Fig.1A were tunneled underneath the skin from the stimulator to the exposed pudendal nerves and were placed around the left and right pudendal nerves as shown in Fig.1B. After implanting the stimulator, the battery, and the cuff electrodes, the muscle and skin were closed by sutures.

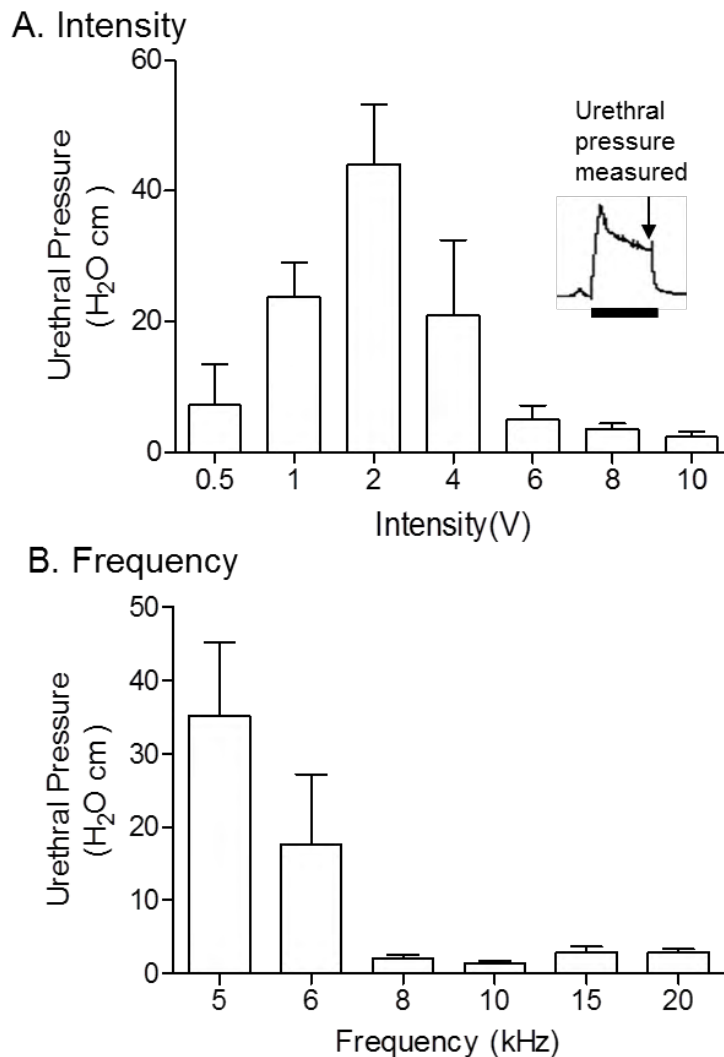


Fig.3. Urethral pressure measured at the end of high frequency biphasic electrical stimulation. A. Different intensities at 10 kHz frequency. B. Different frequencies at 6-10 V intensity. N = 5 cats. The inserted figure in A shows the time point for urethral pressure measurement.

*Pudendal nerve block by high frequency biphasic stimulation*

The high frequency biphasic PNS waveform generated by the implanted stimulator successfully blocked pudendal nerve conduction and eliminated the PNS evoked EUS contraction when applied bilaterally on the pudendal nerves (Figs.2-5). The high frequency biphasic PNS applied bilaterally at 10 kHz for 60 sec at locations Stim. B1 and Stim. B2 (Fig.1B) activated the pudendal nerves, induced a strong EUS contraction, and caused large increases in urethral pressure at intensities of 0.5-2 V (Fig.2A and Fig.3A). However, as the intensity was increased the urethral pressure response gradually decreased in amplitude and duration, and became minimal (<5 cmH<sub>2</sub>O) at the end of the 60 second high frequency stimulation when the intensity was 6-10 V (Fig.2A and Fig.3A). Within this range of intensities (6-10 V), the high frequency biphasic PNS also generated large urethral pressure responses at

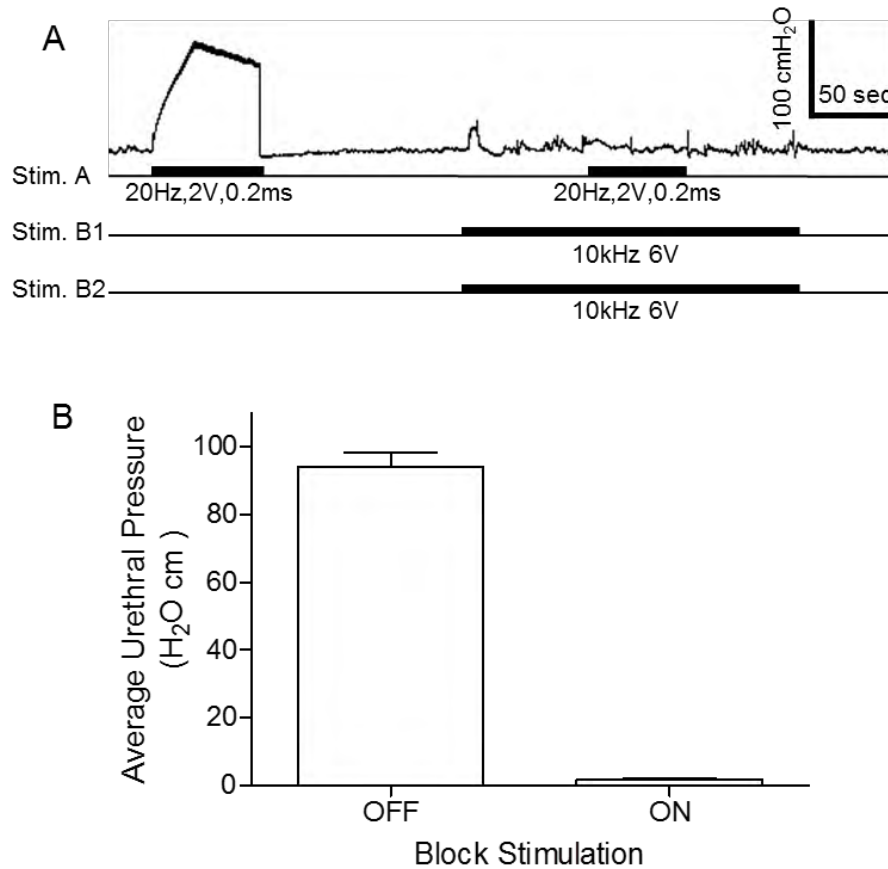


Fig.4. High frequency biphasic electrical stimulation blocked the pudendal nerves and eliminated the urethral pressure increase induced by pudendal nerve stimulation. A. High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely blocked the urethral pressure increase induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. B. Average urethral pressure measured during Stim. A when the high frequency stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 5 cats.

frequencies below 6 kHz, but the response was minimal (<5 cmH<sub>2</sub>O) at the end of the 60 second stimulation once the frequency was increased above 6 kHz (Fig.2B and Fig.3B).

In order to show that the high frequency biphasic PNS blocked pudendal nerve conduction when the urethral pressure response was diminished at the end of the 60 second stimulation, a 20 Hz PNS (2-5 V, 0.2 ms) was applied at Stim. A (Fig.1B) central to the high frequency stimulation site to induce a maximal (70-100 cmH<sub>2</sub>O) urethral pressure response (Fig.4 and Fig.5). This urethral response was completely blocked by the high frequency biphasic PNS (6-15 kHz, 6-10 V) (Fig.4 and Fig.5). The pudendal nerve conduction recovered quickly from the block once the high frequency PNS was terminated (Fig.5A).

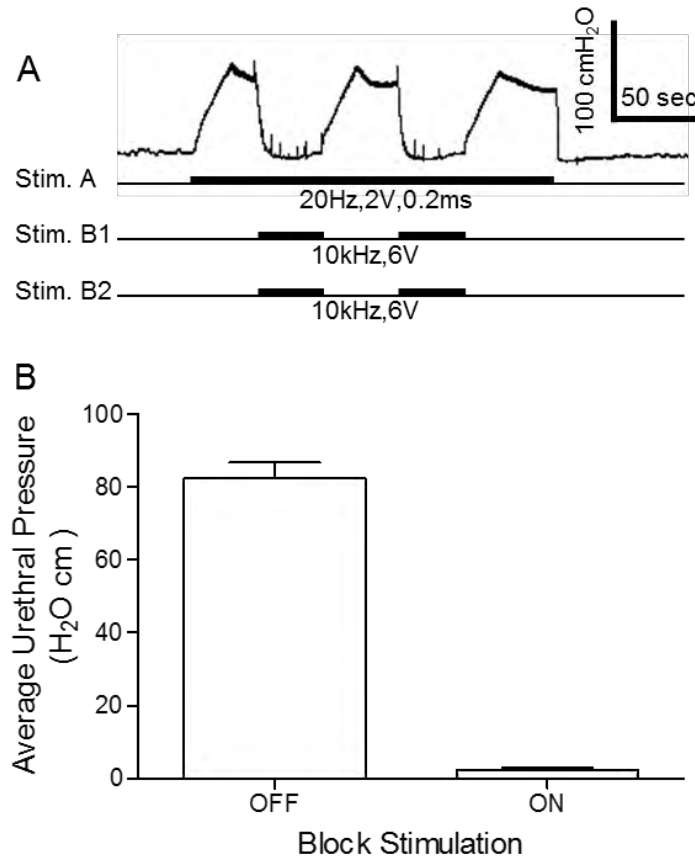


Fig.5. High frequency biphasic stimulation blocked the pudendal nerves and completely reduced the urethral pressure induced by pudendal nerve stimulation. A. High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely reduced the urethral pressure induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. B. Average urethral pressure induced by Stim. A when the high frequency stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 4 cats.

### Bladder excitation or inhibition by PNS

The implanted stimulator also generated rectangular pulses at the cuff electrode #1 (at Stim. A in Fig.1 A and B) that reflexively excited or inhibited the bladder depending on the frequency of stimulation (Fig.6 and Fig.7). Several CMGs were performed in each animal to determine the bladder capacity. In one group of experiments, 20-30 Hz PNS (2-8 V, 0.2 ms) induced a large amplitude ( $45.9 \pm 13.4$  to  $52.0 \pm 22$  cmH<sub>2</sub>O) sustained bladder contraction (Fig.6) when the bladder was filled to 90% of capacity. When the frequency was changed to 5 Hz, PNS (2-5 V, 0.2 ms) applied during CMG inhibited reflex micturition and significantly ( $P < 0.05$ ) increased bladder capacity to  $176.5 \pm 27.1\%$  of the control capacity (8.2  $\pm$  1.9 ml) (Fig.7).

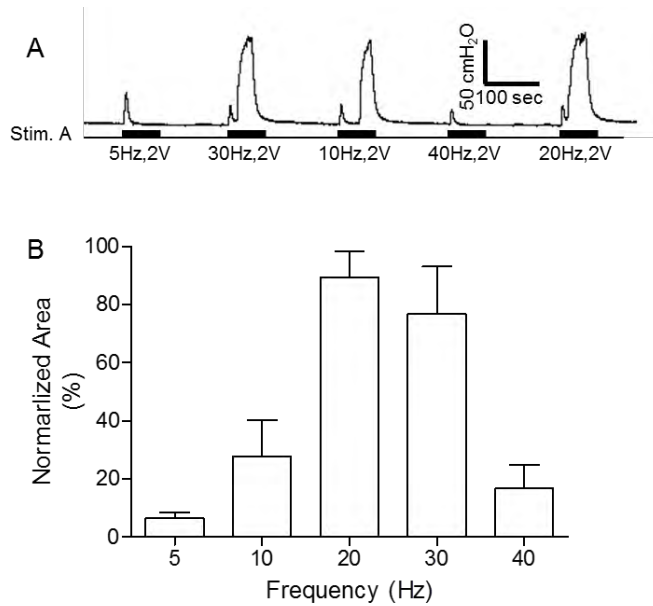


Fig.6. Bladder contraction induced by pudendal nerve stimulation at different frequencies. A. Bladder pressure trace. The black bars under pressure trace indicate the stimulation duration. B. Normalized area under bladder pressure curve during stimulation. The area under curve was normalized to the maximal response in each animal. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-8 V. N = 5 cats.

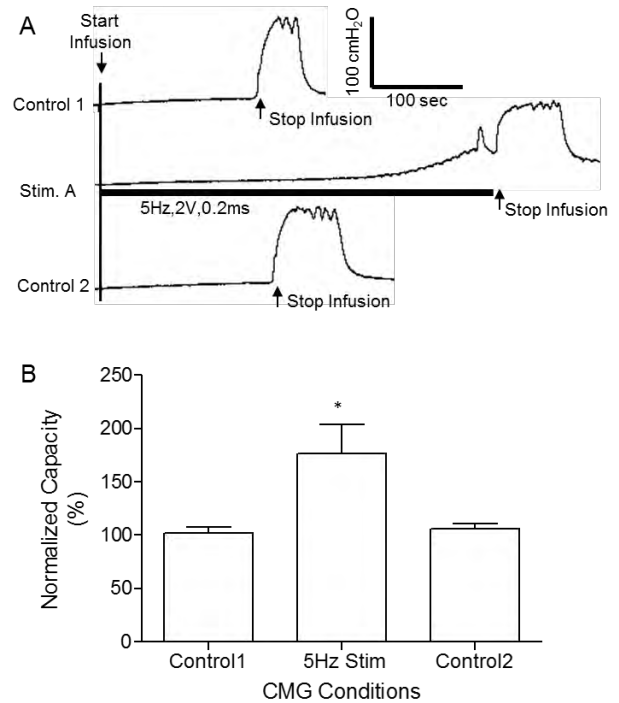


Fig.7. Bladder inhibition induced by 5 Hz pudendal nerve stimulation. A. Repeated CMG recordings. The black bar under the CMG trace indicate the stimulation duration. B. Normalized bladder capacity measured during different CMGs. The capacity was normalized to the measurement from control 1 CMG. \* indicates significantly different from the control 1. Stimulation: frequency 5 Hz, pulse width 0.2 ms, intensity 2-5 V. N = 4 cats.

During the last year, we re-constructed and successfully tested the implantable, wireless controlled, rechargeable battery powered stimulator that can now provide the required stimulation waveforms to: 1) block pudendal nerve conduction and relax the EUS (Figs.2-5), 2) induce a large sustained reflex bladder contraction (Fig.6), or 3) inhibit reflex bladder activity (Fig.7). These acute in vivo experiments in anesthetized cats establish the effectiveness of the device as well as stimulation parameters that will be used in long term experiments to modulate abnormal lower urinary tract function in awake chronic SCI cats.

## Task #2: Test the implantable stimulator in awake chronic SCI animals

After we successfully tested the first prototype of our implantable stimulator in one awake chronic SCI cat as reported in our previous progress report, we further tested the stimulator in additional 2 chronic SCI cats last year. However, the stimulator failed to be charged after each implantation (see the reasons as described in task #1). Although no data could be collected due to the failure of the implanted stimulator, these failures resulted in the redesign of our stimulator packaging (separating the battery and the stimulator, see Fig.1A) and the experimental re-testing in anesthetized cats as shown in Figs.2-7. We are now ready to implant this new stimulator as shown in Fig.1A in awake chronic SCI cats.

## Task #3: Data analysis and publishing the results

We have analyzed the data obtained during last year experiments. Based on these data (Figs.1-7), a manuscript has been written and submitted to the Journal of Urology for publication. We also conducted a computer model analysis of the post-stimulation effect of the high frequency nerve block and published the results as an abstract at the annual meeting of the Society for Neuroscience.

### **Key Research Accomplishments**

- Identified the problems that caused the failure of the first prototype of implantable stimulator
- Re-designed the second prototype of a wireless controlled, wireless chargeable, small implantable stimulator
- Successfully tested the functionality of the re-designed implantable stimulator in anesthetized cats.

### **Reportable Outcomes**

#### Manuscript

- [1] Guangning Yang, Jicheng Wang, Bing Shen, James R. Roppolo, William, C. de Groat, Changfeng Tai, “Pudendal nerve stimulation and block by a wireless controlled implantable stimulator in cats”, Journal of Urology, 2013, submitted.

#### Abstract

- [1] Guangning Yang, Jicheng Wang, James R. Roppolo, William C. de Groat, Changfeng Tai, “Simulation analysis of conduction block in unmyelinated axon after high-frequency electrical stimulation”. 43rd Annual Meeting of Society for Neuroscience, San Diego, 2013.

### **Conclusion**

Our progress in the second year has produce the re-designed implantable stimulator enabling us to further investigate novel PNS/block strategies to restore bladder functions in awake cats after chronic SCI. The success of our project will create a novel implantable

neuroprosthesis to restore both continence and micturition functions for SCI people. It will fundamentally change the current medical treatments for the lower urinary tract dysfunctions after SCI. Daily urethral catheterization will not be the norm for SCI. Frequent infection of the lower urinary tract will be eliminated. The quality of life will be improved greatly for both SCI people and their family.

### **References**

- [1] Changfeng Tai, James R. Roppolo and William C. de Groat , “Block of external urethral sphincter contraction by high frequency electrical stimulation of pudendal nerve”, *Journal of Urology*, Vol.172, PP2069-2072, 2004.
- [2] Changfeng Tai, Stanley E. Smerin, William C. de Groat and James R. Roppolo, “Pudendal-to-bladder reflex in chronic spinal cord injured cat”, *Experimental Neurology*, Vol.197, PP225-234, 2006.
- [3] Changfeng Tai, Jicheng Wang, Xianchun Wang, James R. Roppolo and William C. de Groat, “Voiding reflex in chronic spinal cord injured cats induced by stimulating and blocking pudendal nerves”, *Neurourology and Urodynamics*, Vol.26, PP879-886, 2007.
- [4] Changfeng Tai, Jicheng Wang, Xianchun Wang, William C. de Groat, and James R. Roppolo, “Bladder inhibition and voiding induced by pudendal nerve stimulation in chronic spinal cord injured cats”, *Neurourology and Urodynamics*, Vol. 26, PP570-577, 2007.

### **Appendices**

- [1] Guangning Yang, Jicheng Wang, Bing Shen, James R. Roppolo, William, C. de Groat, Changfeng Tai, “Pudendal nerve stimulation and block by a wireless controlled implantable stimulator in cats”, *Journal of Urology*, 2013, submitted.
- [2] Guangning Yang, Jicheng Wang, James R. Roppolo, William C. de Groat, Changfeng Tai, “Simulation analysis of conduction block in unmyelinated axon after high-frequency electrical stimulation”. 43rd Annual Meeting of Society for Neuroscience, San Diego, 2013.

# Pudendal Nerve Stimulation and Block by a Wireless Controlled Implantable Stimulator in Cats

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Key Words: pudendal nerve, stimulation, block, spinal cord injury, cat

## **ABSTRACT**

**Purpose:** To determine the functionality of a wireless controlled implantable stimulator designed for stimulation and block of the pudendal nerve.

**Materials and Methods:** In 5 cats under  $\alpha$ -chloralose anesthesia, the stimulator was implanted underneath the skin on the left side in the lower back along the sacral spine. Two tripolar cuff electrodes were implanted bilaterally on the pudendal nerves in addition to one bipolar cuff electrode that was implanted on the left side central to the tripolar cuff electrode. The stimulator provided high frequency (5-20 kHz) biphasic stimulation waveforms to the two tripolar electrodes and low frequency (1-100 Hz) rectangular pulses to the bipolar electrode. Bladder and urethral pressures were measured to determine the effects of pudendal nerve stimulation (PNS) or block.

**Results:** The maximal (70-100 cmH<sub>2</sub>O) urethral pressure generated by 20 Hz PNS applied via the bipolar electrode was completely eliminated by the pudendal nerve block induced by the high frequency stimulation (6-15 kHz, 6-10 V) applied via the two tripolar electrodes. In a partially filled bladder 20-30 Hz PNS (2-8 V, 0.2 ms) but not 5 Hz stimulation applied via the bipolar electrode elicited a large sustained bladder contraction (45.9±13.4 to 52.0±22 cmH<sub>2</sub>O). During cystometry the 5 Hz PNS significantly ( $P<0.05$ ) increased bladder capacity to  $176.5 \pm 27.1\%$  of the control capacity.

**Conclusions:** The wireless controlled implantable stimulator successfully generated the required waveforms for stimulation and block of pudendal nerve, which will be useful for restoring bladder functions after spinal cord injury (SCI).

## INTRODUCTION

After SCI above the lumbosacral level, the coordinated action between bladder and external urethral sphincter (EUS) disappears.<sup>1</sup> Instead, the bladder and EUS contract simultaneously (termed detrusor sphincter dyssynergia or DSD), which generates high bladder pressure, prevents complete elimination of urine, and requires daily urethral catheterization.<sup>1,2</sup> High bladder pressure can cause vesicoureteral reflux and renal failure in the long-term. Residual urine in the bladder and frequent urethral catheterization can cause infection.<sup>2,3</sup> In addition, detrusor overactivity (DO) induces poor bladder storage function and frequent incontinence.<sup>1-3</sup> Currently, no medication can treat both DSD and DO.

Our previous studies<sup>4-6</sup> in chronic SCI cats under anesthesia have revealed a frequency-dependent pudendal-to-bladder spinal reflex. PNS at 5 Hz can inhibit reflex bladder activity and increase bladder capacity, but at 20 Hz it can excite the bladder and induce a large bladder contraction.<sup>4-6</sup> In addition, our previous studies<sup>7-9</sup> in cats have shown that high frequency (>6 kHz) biphasic stimulation can block the pudendal nerve and completely relax the EUS. When the 20 Hz PNS was combined with high frequency pudendal nerve block in anesthetized chronic SCI cats, a large bladder contraction was induced simultaneously with an EUS relaxation, resulting in efficient voiding.<sup>10</sup> These results indicate that both micturition and continence functions could be restored after SCI by stimulation and block of the pudendal nerve.

However, to test the stimulation/block strategy in a future clinical trial to restore bladder functions after SCI, an implantable stimulator is needed to generate the

required 5 Hz and 20 Hz PNS as well as the high frequency (>6 kHz) biphasic waveform for pudendal nerve block. Currently, such an implantable stimulator is not commercially available. Therefore, in this study we designed and constructed a small, wireless controlled, battery powered, implantable stimulator, that we showed in anesthetized cats can generate the required stimulation waveforms to reflexively excite or inhibit the bladder, and block axonal conduction in the pudendal nerve. This study represents the first step in developing a device for future testing in awake chronic SCI animals, and eventually in SCI human subjects.

## **MATERIALS AND METHODS**

All protocols involving the use of animals in this study were approved by the Animal Care and Use Committee at the University of Pittsburgh. Fig.1A shows a picture of the implantable stimulator (dimensions: 5.6x4.0x0.8 cm) connected to a rechargeable battery (3.7 V and 900 mAh; dimensions: 5.4x3.6x0.6 cm). The stimulator has 2 output channels providing charge-balanced rectangular pulses (1-100 Hz, 0-11 V, 0.05-0.2 ms) to the bipolar cuff electrode #1 (i.e., Stim. A in Fig.1B) and a high frequency (5-20 kHz, 0-11 V) biphasic square waveform (see Fig.1B) to the tripolar cuff electrodes #2 and #3 (i.e., Stim. B1 and B2 in Fig.1B). The stimulator can be wireless controlled within a 2-meter distance by a USB controller that is connected to a USB port of a portable computer (the computer is not shown). The computer software can set stimulation parameters for each output channel and turn on/off each channel by wireless communication between the implanted stimulator and

the USB controller. The stimulator and battery are implanted underneath the skin on the left side of the lower back of the cat along the sacral spine. The battery can be charged by the charging circuitry in the stimulator that can be powered wirelessly across the skin by an external charging coil (not shown). At the beginning of each experiment, the battery was fully charged from 2.8 V to 3.7 V in about 15-20 minutes and it could be run for the entire experiment (5-6 hours) with repeated stimulation. At the end of the experiment, the battery, stimulator, and electrodes were removed from the animal.

A total of 5 cats (3 female and 2 male, 2.9 to 3.3 kg) were used in this study. Isoflurane (2-5% in O<sub>2</sub>) was used to anesthetize the animals during surgery and then replaced by  $\alpha$ -chloralose anesthesia (65 mg/kg i.v. and supplemented as needed) during data collection. The temperature of the animal was maintained at 35 °C to 37 °C using a heating pad. The ureters were cut and drained externally. A double lumen catheter (5F) was inserted into the bladder through a small incision in the proximal urethra and secured by a ligature (Fig.1B). One lumen of the catheter was attached to a pump to infuse the bladder with saline, and the other lumen was connected to a pressure transducer to monitor the bladder activity. Another catheter (5F) was also inserted at the same site in the proximal urethra but directed toward the distal urethra and secured by a ligature (Fig.1B). This catheter was attached to an infusion pump and to a pressure transducer via a T connector. The pudendal nerves were accessed posteriorly in the sciatic notch lateral to the tail. The three cuff electrodes (NCE112/113, MicroProbes Inc., Gaithersburg, MD) as shown in Fig.1A were

tunneled underneath the skin from the stimulator to the exposed pudendal nerves and were placed around the left and right pudendal nerves as shown in Fig.1B. After implanting the stimulator, the battery, and the cuff electrodes, the muscle and skin were closed by sutures.

Three tests were performed in this study to determine the ability for the implanted stimulator to: (1) block the pudendal nerve, (2) induce large bladder contraction, or (3) inhibit the micturition reflex. In the first test (N=5 cats), the urethra was infused continuously with saline at a rate of 1-2 ml/min. Back pressure in the urethral perfusion system caused by EUS contraction was recorded via the pressure transducer (Fig.1B). First, the high frequency biphasic pudendal nerve stimulation (PNS) at 10 kHz was applied to both Stim. A and Stim. B sites (see Fig.1B) at different intensities (0.5-10V) to determine the effective intensities for pudendal nerve block. Then, using an intensity effective in blocking the nerve at 10 kHz, different frequencies (5-20 kHz) were tested to determine the threshold and optimal frequencies for pudendal nerve block. Finally, the high frequency biphasic stimulation determined to be effective in blocking the pudendal nerve conduction was applied to block the maximal EUS contraction induced by the 20 Hz PNS applied at Stim. A (Fig.1B). In the second test (N=5 cats) a cystometrogram (CMG) was performed to determine the bladder capacity (i.e., the volume necessary to induce a large micturition contraction, >30 cm H<sub>2</sub>O). Then the bladder was infused to about 90% of its capacity and PNS (2-8 V, 0.2 ms) of different frequencies (5-40 Hz) was applied at Stim. A (Fig.1B) to determine the optimal frequency for inducing a large (>30 cmH<sub>2</sub>O) bladder contraction. In the

third test (N=4 cats), repeated CMGs were performed to determine the bladder capacity. Each CMG consisted of a slow infusion of saline (1-2 ml/min) starting with an empty bladder until the first micturition contraction occurred. Initially, two or three control CMGs were performed without PNS to determine the control bladder capacity and evaluate reproducibility. Then, PNS (5 Hz, 2-5 V, 0.2 ms) was applied at Stim. A (Fig.1B) during the CMG to increase bladder capacity. A control CMG without stimulation was also performed after the PNS CMG.

To quantify the PNS inhibitory effect, the bladder capacity measured during each CMG was normalized to the measurement during the first control CMG. Bladder contraction amplitude and area under bladder contraction curve were measured to determine the excitatory PNS effect. Urethral pressure induced by 20 Hz PNS was measured to determine the effect of high frequency block. The normalized data from different animals are presented as mean  $\pm$  standard error. Student T-test was used to detect statistical significance ( $P < 0.05$ ).

## **RESULTS**

### *Pudendal nerve block by high frequency biphasic stimulation*

The high frequency biphasic PNS waveform generated by the implanted stimulator successfully blocked pudendal nerve conduction and eliminated the PNS evoked EUS contraction when applied bilaterally on the pudendal nerves (Figs.2-5). The high frequency biphasic PNS applied bilaterally at 10 kHz for 60 sec at locations Stim. B1 and Stim. B2 (Fig.1B) activated the pudendal nerves, induced a strong EUS

contraction, and caused large increases in urethral pressure at intensities of 0.5-2 V (Fig.2A and Fig.3A). However, as the intensity was increased the urethral pressure response gradually decreased in amplitude and duration, and became minimal (<5 cmH<sub>2</sub>O) at the end of the 60 second high frequency stimulation when the intensity was 6-10 V (Fig.2A and Fig.3A). Within this range of intensities (6-10 V), the high frequency biphasic PNS also generated large urethral pressure responses at frequencies below 6 kHz, but the response was minimal (<5 cmH<sub>2</sub>O) at the end of the 60 second stimulation once the frequency was increased above 6 kHz (Fig.2B and Fig.3B).

In order to show that the high frequency biphasic PNS blocked pudendal nerve conduction when the urethral pressure response was diminished at the end of the 60 second stimulation, a 20 Hz PNS (2-5 V, 0.2 ms) was applied at Stim. A (Fig.1B) central to the high frequency stimulation site to induce a maximal (70-100 cmH<sub>2</sub>O) urethral pressure response (Fig.4 and Fig.5). This urethral response was completely blocked by the high frequency biphasic PNS (6-15 kHz, 6-10 V) (Fig.4 and Fig.5). The pudendal nerve conduction recovered quickly from the block once the high frequency PNS was terminated (Fig.5A).

#### *Bladder excitation or inhibition by PNS*

The implanted stimulator also generated rectangular pulses at the cuff electrode #1 (at Stim. A in Fig.1 A and B) that reflexively excited or inhibited the bladder depending on the frequency of stimulation (Fig.6 and Fig.7). Several CMGs were

performed in each animal to determine the bladder capacity. In one group of experiments, 20-30 Hz PNS (2-8 V, 0.2 ms) induced a large amplitude ( $45.9 \pm 13.4$  to  $52.0 \pm 22$  cmH<sub>2</sub>O) sustained bladder contraction (Fig.6) when the bladder was filled to 90% of capacity. When the frequency was changed to 5 Hz, PNS (2-5 V, 0.2 ms) applied during CMG inhibited reflex micturition and significantly ( $P < 0.05$ ) increased bladder capacity to  $176.5 \pm 27.1\%$  of the control capacity ( $8.2 \pm 1.9$  ml) (Fig.7).

## **DISCUSSION**

In this study we constructed and successfully tested an implantable, wireless controlled, rechargeable battery powered stimulator that can provide the required stimulation waveforms to: 1) block pudendal nerve conduction and relax the EUS (Figs.2-5), 2) induce a large sustained reflex bladder contraction (Fig.6), or 3) inhibit reflex bladder activity (Fig.7). These acute in vivo experiments in anesthetized normal cats establish the effectiveness of the device as well as stimulation parameters that will be used in future long term experiments to modulate abnormal lower urinary tract function in awake chronic SCI cats. In the chronic experiments, the 5 Hz PNS will be used to inhibit bladder overactivity and to promote urine storage. However to elicit voiding, the 5 Hz PNS will be switched to 20 Hz to induce a sustained bladder contraction and at the same time a high frequency (6-10 kHz) pudendal nerve block will be used to relax the EUS and prevent DSD, so that efficient, low pressure voiding can be induced.

The elimination of EUS contraction by the high frequency stimulation as shown in Figs.4-5 is due to the block of pudendal nerve conduction. It is not due to EUS fatigue caused by the stimulation, because a previous study <sup>9</sup> showed that the EUS could still contract if the Stim. A (Fig.1B) was moved to a location distal to the high frequency blocking stimulation. In the present study, the high frequency blocking stimulation was applied bilaterally on the pudendal nerves (Fig.1B) to block a possible excitatory pudendal-to-pudendal reflex <sup>10,11</sup> that can be triggered by afferent axonal volleys elicited by Stim. A that in turn can elicit efferent activity on the contralateral as well as the ipsilateral pudendal nerves to cause an EUS contraction. In addition, bilateral block of the pudendal nerves would be needed to control DSD after chronic SCI because afferent activity elicited by bladder contractions can generate pudendal efferent activity and EUS contractions bilaterally. Therefore, in this study we implanted the blocking electrodes bilaterally on the pudendal nerves (Stim. B1 and B2 in Fig.1B) to mimic the conditions when the implantable stimulator is used to restore bladder functions after chronic SCI.

The high frequency blocking stimulation generated by the implantable stimulator produced a reversible block of the pudendal nerve. Pudendal nerve conduction recovered quickly once the high frequency blocking stimulation was off (Fig.5), indicating that the stimulation was safe and no nerve damage was induced. It is worth noting that the quick recovery from pudendal nerve block as shown in Fig.5 was achieved even after repeatedly (>14 times, see Fig.2 and Fig.4) applying the high frequency blocking stimulation of 1-3 minute duration for a total duration greater than

15 minutes. In clinical applications to restore micturition function after SCI, the high frequency blocking stimulation will be applied about 3-5 times per day for only 1-2 minutes each time during voiding. Therefore, the possibility of pudendal nerve damage caused by the high frequency blocking stimulation is not a concern. In addition, the safety of high frequency blocking stimulation has also been verified by recent clinical studies to block the vagus nerve for diabetes treatment.<sup>12,13</sup> The reversibility from pudendal nerve block is not only important for safety reasons but also necessary for maintaining continence function during urine storage.

About 15-20 minutes were needed to fully charge the battery wirelessly across the skin. After each charging, the battery successfully powered the stimulator in the animal for the entire experimental period (5-6 hours). After removing the stimulator and battery from the animal at the end of experiment, the battery power lasted for about 2-3 days before the stimulator stopped functioning and lost communication with the USB controller due to a low battery level (<2.8 V). Although the stimulator was not used to stimulate/block the pudendal nerve once it was removed from the animal, it is estimated that the battery should still be able to power the stimulator for the same amount of time (2-3 days) if it were used for PNS/block. This is because the electrical power used by PNS/block is only a very small portion of the total power consumption by the electrical circuits including wireless communication, microprocessor, and the output amplifiers. Therefore, it is expected that the implantable stimulator will continuously function after chronic implantation in SCI cats as long as we continue to charge it for 15-20 minutes every day.

This study only tested the functionality of the implantable stimulator. The durability can only be tested when the stimulator is implanted in awake chronic SCI cats in future experiments. Although many improvements on this prototype stimulator may have to be implemented as our study progresses, this study is the first step of our long-term effort in designing an implantable pudendal nerve stimulator for restoring bladder functions after SCI.

### **ACKNOWLEDGEMENT**

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## **FIGURE CAPTIONS**

Fig.1. The implantable stimulator (A) and the locations of cuff electrodes implanted on the pudendal nerves in the cat (B). EUS – External Urethral Sphincter.

Fig.2. Urethral pressure induced by the high frequency biphasic electrical stimulation applied bilaterally on the pudendal nerves. A. Different intensities at 10 kHz frequency. B. Different frequencies at 6 V intensity. The urethral infusion rate is 1 ml/min. The black bars under the pressure traces indicate the stimulation duration. The calibration bars are for both A and B. The Y-calibration bar indicates the urethral pressure in 50 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 100 seconds.

Fig.3. Urethral pressure measured at the end of high frequency biphasic electrical stimulation. A. Different intensities at 10 kHz frequency. B. Different frequencies at

6-10 V intensity. N = 5 cats. The inserted figure in A shows the time point for urethral pressure measurement.

Fig.4. High frequency, biphasic electrical stimulation of the pudendal nerves bilaterally blocked the urethral pressure increase induced by 20 Hz unilateral pudendal nerve stimulation. A. High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely blocked the urethral pressure increase induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates urethral pressure in 100 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 50 seconds. B. Average urethral pressure measured during Stim. A when the high frequency stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 5 cats.

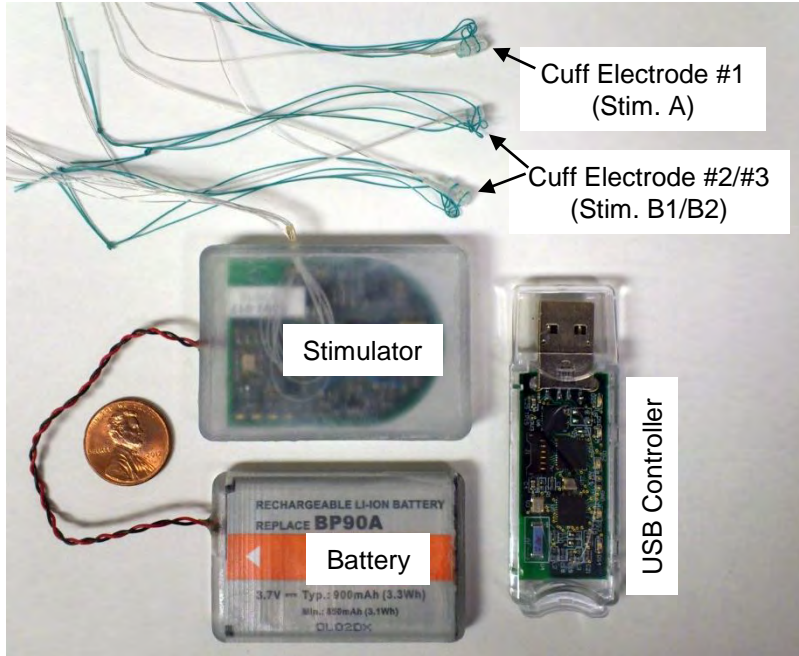
Fig.5. High frequency biphasic stimulation of the pudendal nerves bilaterally completely blocked the increase in urethral pressure induced by unilateral pudendal nerve stimulation. A. Records from one female cat showing the block of the response elicited by Stim. A during bilateral pudendal nerve stimulation (Stim. B1 and Stim. B2). High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely reduced the urethral pressure induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates the urethral pressure in 100 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 50 seconds. B. Average urethral pressure induced by Stim. A when the high frequency

stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 4 cats.

Fig.6. Bladder contractions induced by pudendal nerve stimulation at different frequencies. A. Increase in bladder pressure elicited by unilateral pudendal nerve stimulation (Stim. A). The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates bladder pressure in 50 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 100 seconds. B. Normalized area under bladder pressure curve during stimulation. The area under curve was normalized to the maximal response in each animal. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-8 V. N = 5 cats.

Fig.7. Increase in bladder capacity induced by 5 Hz unilateral pudendal nerve stimulation. A. Repeated CMG recordings (infusion rate 2 ml/min in a female cat) showing in the middle trace the reversible increase in bladder capacity during stimulation. The black bar under the CMG trace indicates the stimulation duration. The Y-calibration bar indicates the bladder pressure in 100 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 100 seconds. B. Normalized bladder capacity measured during different CMGs. The capacity was normalized to the measurement from control 1 CMG. \* indicates significantly different from the control 1. Stimulation: frequency 5 Hz, pulse width 0.2 ms, intensity 2-5 V. N = 4 cats.

## A. Implantable Stimulator



## B. Experimental Setup

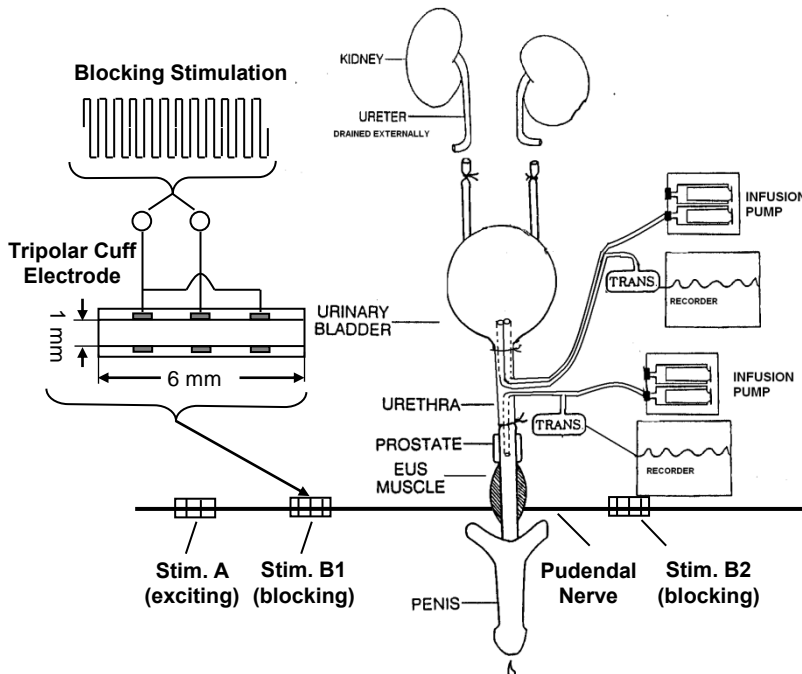
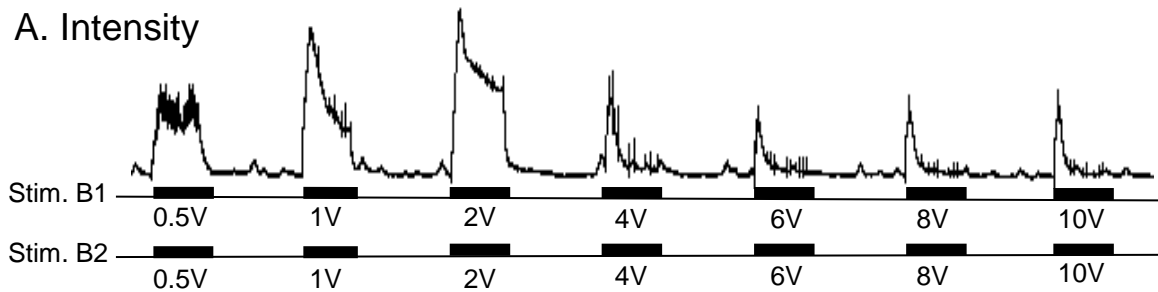


Fig.1. The implantable stimulator (A) and the locations of cuff electrodes implanted on the pudendal nerves in the cat (B). EUS – External Urethral Sphincter.

### A. Intensity



### B. Frequency

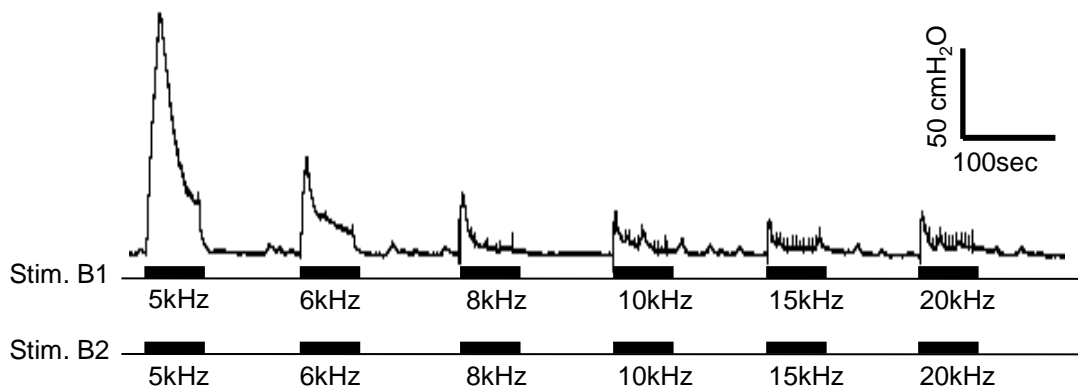


Fig.2. Urethral pressure induced by the high frequency biphasic electrical stimulation applied bilaterally on the pudendal nerves. A. Different intensities at 10 kHz frequency. B. Different frequencies at 6 V intensity. The urethral infusion rate is 1 ml/min. The black bars under the pressure traces indicate the stimulation duration. The calibration bars are for both A and B. The Y-calibration bar indicates the urethral pressure in 50 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 100 seconds.

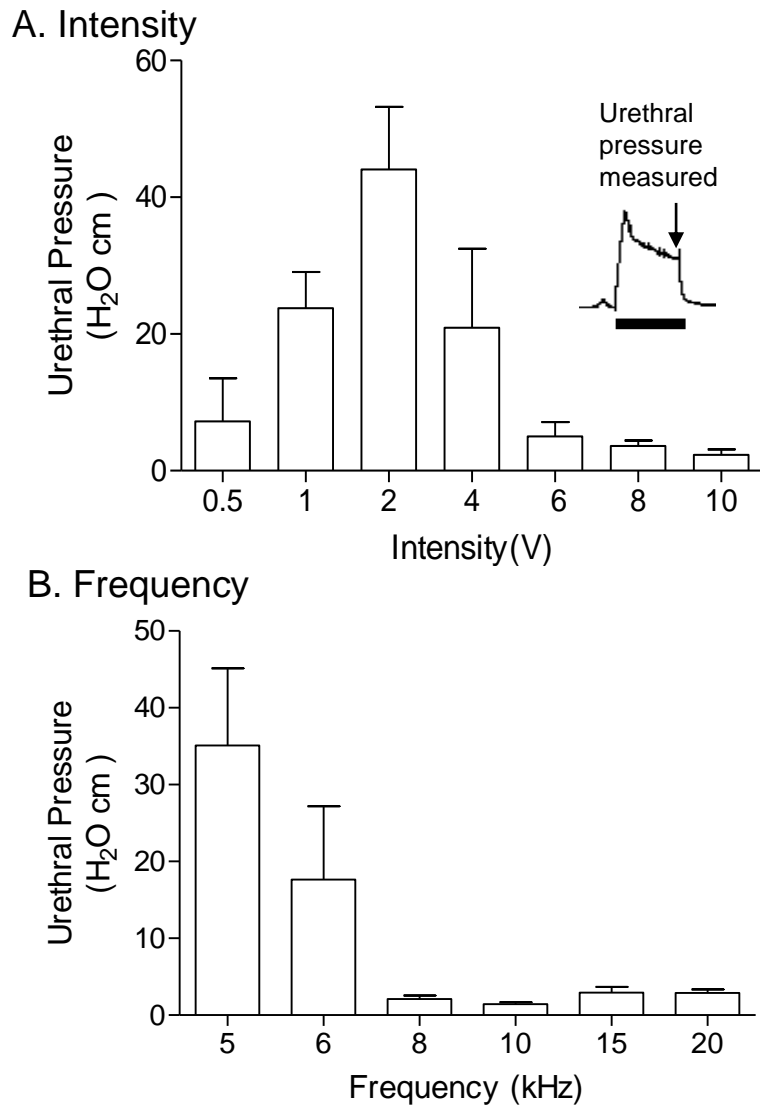


Fig.3. Urethral pressure measured at the end of high frequency biphasic electrical stimulation. A. Different intensities at 10 kHz frequency. B. Different frequencies at 6-10 V intensity. N = 5 cats. The inserted figure in A shows the time point for urethral pressure measurement.

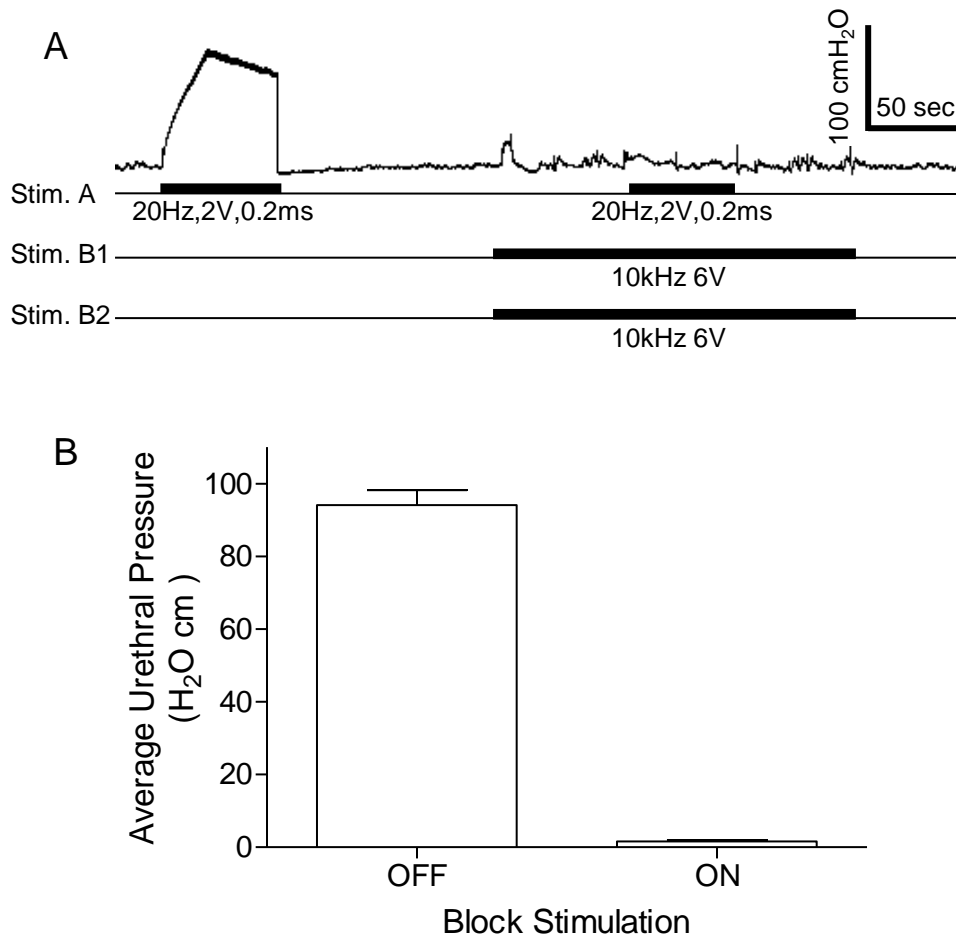


Fig.4. High frequency, biphasic electrical stimulation of the pudendal nerves bilaterally blocked the urethral pressure increase induced by 20 Hz unilateral pudendal nerve stimulation. A. High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely blocked the urethral pressure increase induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates urethral pressure in 100 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 50 seconds. B. Average urethral pressure measured during Stim. A when the high frequency stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 5 cats.

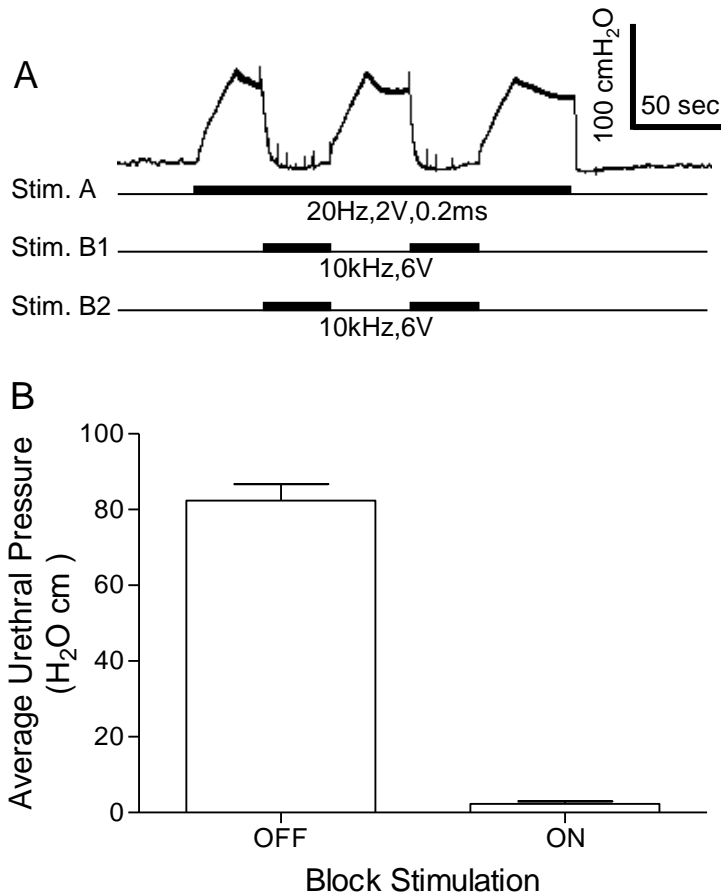


Fig.5. High frequency biphasic stimulation of the pudendal nerves bilaterally completely blocked the increase in urethral pressure induced by unilateral pudendal nerve stimulation. A. Records from one female cat showing the block of the response elicited by Stim. A during bilateral pudendal nerve stimulation (Stim. B1 and Stim. B2). High frequency stimulation delivered to Stim. B1 and Stim. B2 (see Fig.1B) completely reduced the urethral pressure induced by Stim. A. The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates the urethral pressure in 100 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 50 seconds. B. Average urethral pressure induced by Stim. A when the high frequency stimulation was either on or off. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-5 V. Stim. B1/B2: frequency 6-15 kHz, intensity 6-10 V. N = 4 cats.

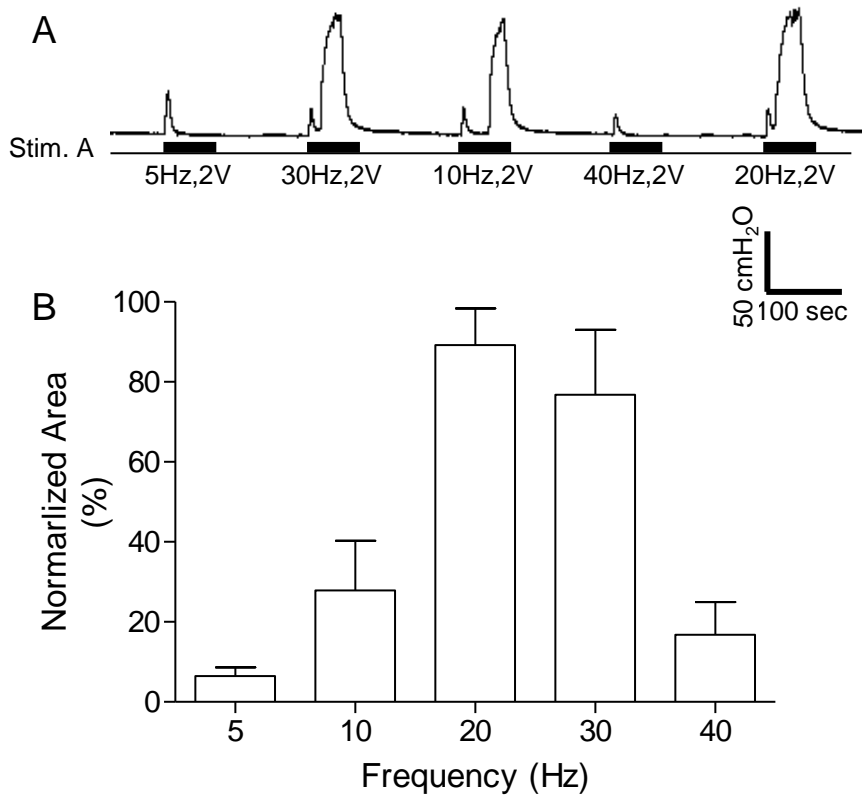


Fig.6. Bladder contractions induced by pudendal nerve stimulation at different frequencies. A. Increase in bladder pressure elicited by unilateral pudendal nerve stimulation (Stim. A). The black bars under pressure trace indicate the stimulation duration. The Y-calibration bar indicates bladder pressure in 50 cmH<sub>2</sub>O and the X-calibration bar indicates the time in 100 seconds. B. Normalized area under bladder pressure curve during stimulation. The area under curve was normalized to the maximal response in each animal. Stim. A: frequency 20 Hz, pulse width 0.2 ms, intensity 2-8 V. N = 5 cats.

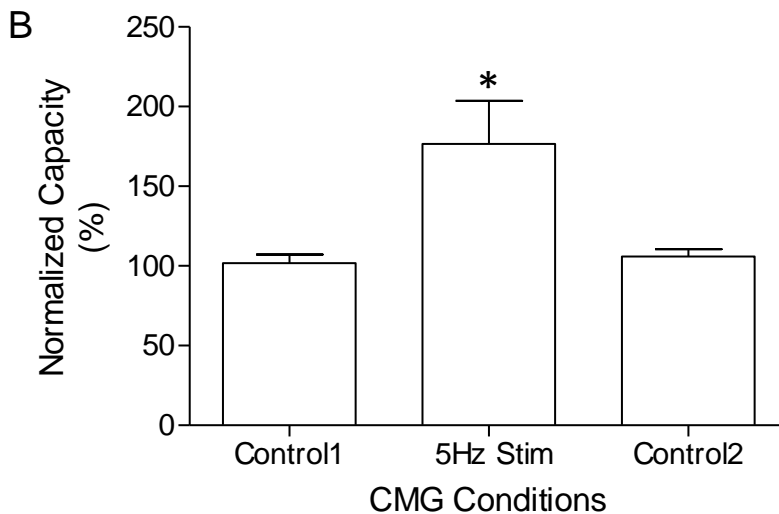
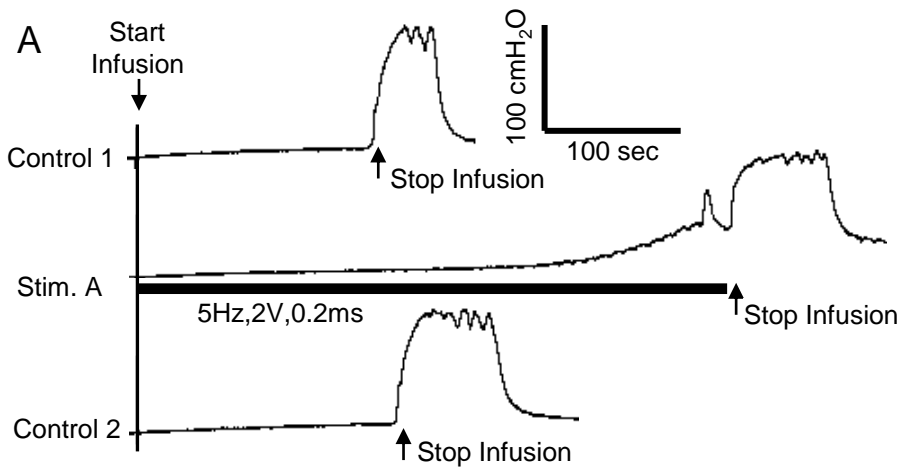


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## Simulation Analysis of Conduction Block in Unmyelinated Axon after High-Frequency Electrical Stimulation

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Nerve conduction block induced by high frequency (>5 kHz) electrical stimulation have many potential clinical applications. Although the original Hodgkin-Huxley model can successfully simulate the conduction block in unmyelinated axon during the stimulation, it failed to simulate the conduction block during the period after the stimulation. In this study, the Hodgkin-Huxley model was modified to include an electrogenic sodium-potassium pump and successfully simulated the post-stimulation conduction block. Simulation analysis indicates that high frequency electrical stimulation causes continuous sodium influx and increases intra-axonal sodium concentration that can only recover slowly after the stimulation, causing conduction block during the post-stimulation period. The duration of the post-stimulation block is proportional to the duration and intensity of high frequency electrical stimulation. Understanding the mechanisms underlying high frequency block is important to further promote its clinical applications.

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Index Terms—Na-K pump, recovery period, sodium concentration, High-frequency.