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Award Number: W81XWH-12-1-0575

TITLE: Restoration of the Retinal Structure and Function after Injury

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REPORT DATE: October 2013

TYPE OF REPORT: Annual Report

PREPARED FOR: U.S. Army Medical Research and Materiel Command
Fort Detrick, Maryland 21702-5012

DISTRIBUTION STATEMENT: Approved for Public Release;
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REPORT DOCUMENTATION PAGE				Form Approved OMB No. 0704-0188	
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1. REPORT DATE October 2013		2. REPORT TYPE Annual Report		3. DATES COVERED 30September2012–29September2013	
4. TITLE AND SUBTITLE Restoration of the Retinal Structure and Function After Injury				5a. CONTRACT NUMBER W81XWH-12-1-0575	
				5b. GRANT NUMBER W81XWH-12-1-0575	
				5c. PROGRAM ELEMENT NUMBER	
6. AUTHOR(S) Prof. Daniel V. Palanker E-Mail: palanker@stanford.edu				5d. PROJECT NUMBER	
				5e. TASK NUMBER	
				5f. WORK UNIT NUMBER	
7. PERFORMING ORGANIZATION NAME(S) AND ADDRESS(ES) Stanford University Palo Alto, CA 94304-8445				8. PERFORMING ORGANIZATION REPORT NUMBER	
9. SPONSORING / MONITORING AGENCY NAME(S) AND ADDRESS(ES) U.S. Army Medical Research and Materiel Command Fort Detrick, Maryland 21702-5012				10. SPONSOR/MONITOR'S ACRONYM(S)	
				11. SPONSOR/MONITOR'S REPORT NUMBER(S)	
12. DISTRIBUTION / AVAILABILITY STATEMENT Approved for Public Release; Distribution Unlimited					
13. SUPPLEMENTARY NOTES					
14. ABSTRACT Shear forces inflicted by explosion or head impact may result in traumatic retinopathy due to damage of retinal pigment epithelium (RPE) and photoreceptors, leading to loss of sight. Similar injury to photoreceptors and RPE can be induced by exposure to a short pulse laser. Currently there is no therapy for such blind spots (scotomata), and the loss of sight is permanent. This study is focused on development of strategies for elimination or reduction of retinal scotomata and scarring based utilization of retinal plasticity. We established a model of traumatic retinopathy using selective laser coagulation of RPE and photoreceptors in rabbits, based on rapid scanning with a continuous laser. We explore the extent of migration of the photoreceptors from the adjacent non-damaged areas into the damage zone and rewiring of the migrating photoreceptors to local inner retinal neurons. The shift of the photoreceptors into the damage zone over time is monitored with optical coherence tomography and histology. The extent of rewiring is assessed using electrophysiology on a multielectrode array. Within the 4 weeks we observed complete recovery of the 100um damage zone and nearly complete recovery of the 200um zone. Longer follow-up studies with larger damage zone (400um) are in progress.					
15. SUBJECT TERMS none					
16. SECURITY CLASSIFICATION OF:			17. LIMITATION OF ABSTRACT	18. NUMBER OF PAGES	19a. NAME OF RESPONSIBLE PERSON
a. REPORT	b. ABSTRACT	c. THIS PAGE			USAMRMC
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Introduction

Shear forces inflicted by explosion or head impact may result in traumatic retinopathy due to damage of retinal pigment epithelium (RPE) and photoreceptors, leading to loss of sight. Similar injury to photoreceptors and RPE can be induced by exposure to a short pulse laser. Currently there is no therapy for such blind spots (scotomata), and the loss of sight is permanent. This study is focused on development of strategies for elimination or reduction of retinal scotomata and scarring based utilization of retinal plasticity. We established a model of traumatic retinopathy using selective laser coagulation of RPE and photoreceptors in rabbits, based on rapid scanning with a continuous laser. We explore the extent of migration of the photoreceptors from the adjacent non-damaged areas into the damage zone and rewiring of the migrating photoreceptors to local inner retinal neurons. The shift of the photoreceptors into the damage zone over time is monitored with optical coherence tomography and histology. The extent of rewiring is assessed using electrophysiology on a multielectrode array.

Results

The results of our research during the reporting period are presented below, listed by specific tasks:

1) Establish and characterize a model of traumatic retinopathy by creating large scotomata using selective laser coagulation of RPE and photoreceptors in pigmented rabbits. This model will create retinal condition similar to the traumatic retinopathy or retinal dystrophy, including the areas void of photoreceptors, while preserving the inner retinal neurons – inner nuclear layer and ganglion cell layer.

Creating a uniform area of selective damage to RPE and photoreceptors with multiple spot coagulation turned out to be rather challenging since the center of each spot typically exhibits deeper damage than its periphery. To overcome this difficulty and create large uniform and reproducible areas of selective damage to RPE and photoreceptors we developed a new methodology based on rapid scanning of a continuous laser. In this approach our proprietary software directly controls the scanner of a commercial pattern scanning laser (PASCAL, Topcon Medical Laser Systems). By adjusting the power, spot size and scanning speed one can easily control the depth of the retinal damage. By placing lines adjacent to each other one can create large areas of uniform and reproducible damage. Examples of the selective retinal damage produced by a single scan with 100 μm spot diameter and by 4 adjacent lines of the same spot size are shown in the Figure 1.

As one can see in these images, the damage is limited to RPE and photoreceptors, sparing the inner retina (INL and GCL) in both lesions, despite the very significant difference in the lesion width. One can resolve 4 “waves” of the coagulated outer segments of the photoreceptors in the wider lesion (bottom image in Figure 1). The optimal settings

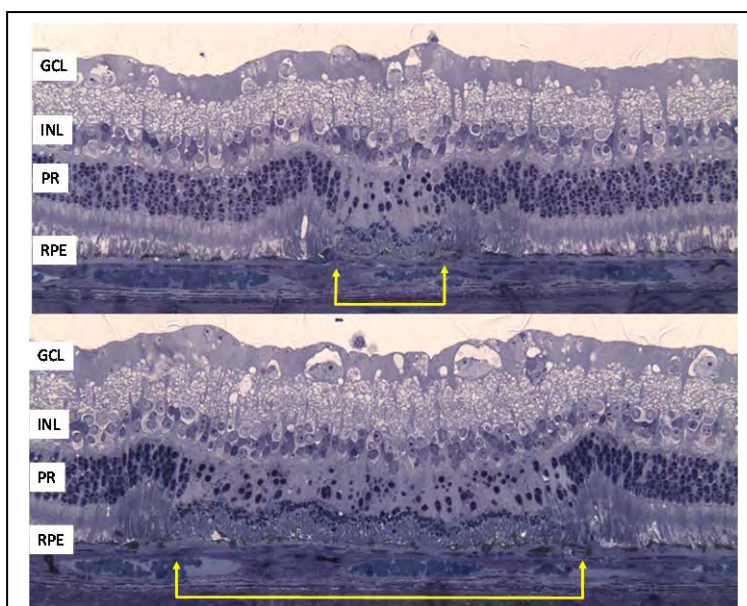


Figure 1. Selective damage to RPE and photoreceptors produced in the rabbit retina by line scanning, as seen 2 days after the treatment. Top: a single scan with 100 μm spot size. Bottom: 4 adjacent scans using the same spot size.

for producing selective retinal damage were determined to be: retinal spot size $d=100\text{ }\mu\text{m}$, power $P=2\text{ W}$, scanning velocity $V=1.6\text{ m/s}$. Green (532nm) or yellow (577 nm) wavelength could be used for this purpose. Dutch Belted pigmented rabbits have been utilized in these experiments.

At much lower velocity (0.1 m/s), scanning laser allows creating much more severe retinal damage, including choroidal rupture and bleeding, as illustrated in the Figure 2. Since the goal of this proposal is selective damage to photoreceptors and RPE, we focused our research on high speed scanning regime.

2) Apply selective laser treatment to shift photoreceptors from the adjacent non-damaged areas into the scotoma. Characterize the effects of the single spot laser exposure parameters on dynamics of the photoreceptors shift and the extent of residual scarring.

We assessed migration of the photoreceptors and restoration of the retinal function in the damaged areas using electrophysiological recordings from the retina by multielectrode arrays. Signals from the retinal ganglion cells (RGCs) in response to stimulation with spatiotemporal white noise were recorded, and receptive fields of each detected RGC mapped, as illustrated in Figure 3 (in pink). As expected, laser scanning destroyed photoreceptors and RPE, resulting in a scotoma, as can be seen on the left in Figure 3 (pointed by an arrow). At one month though, the scotoma corresponding to $100\mu\text{m}$ lesion almost completely disappeared due to migration of the photoreceptors from adjacent areas, leaving very narrow residual scotoma, as can be seen on the right (arrow) in Figure 3A. With $200\text{ }\mu\text{m}$ lesions though the recovery at 1 month was only partial, reducing the width of the scotoma from $170\text{ } \pm 7\text{ }\mu\text{m}$ to $53\text{ } \pm 4\text{ }\mu\text{m}$.

Areas of the missing photoreceptors in the healing lesions could also be seen using fluorescent marker of rhodopsin, as illustrated in the Figure 4. This Figure illustrates the narrow residual gap ($\sim 12\mu\text{m}$) in the photoreceptors coverage of the former $100\text{ }\mu\text{m}$ lesion at 1 month. Longer follow-up is required to see further progress of the photoreceptors migration into the lesion.

We are now monitoring longer follow-up of the lesion width over time, in order to determine when the maximum contraction of the lesion is achieved, and the residual scarring stabilizes. We monitor the lesions of 100, 200 and $400\text{ }\mu\text{m}$ in width.

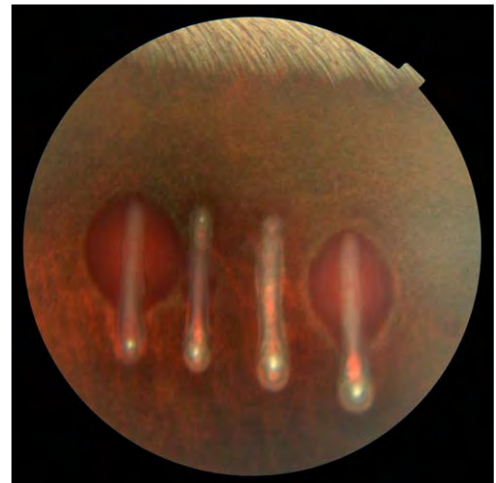


Figure 2. Fundus photo 1 hour after the treatment illustrates severe retinal damage and choroidal bleeding produced by line scanning with $100\text{ }\mu\text{m}$ spot size, 2W power and 0.1 m/s scanning speed.

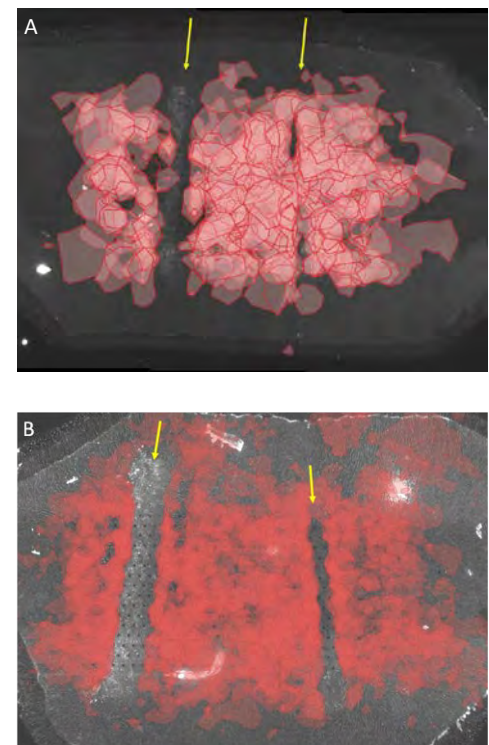


Figure 3. Maps of the RGC receptive fields in the rabbit retina with acute (left) and partially healed (right) lines of damage.

A. $100\text{ }\mu\text{m}$ wide lesions.

B. $200\text{ }\mu\text{m}$ wide lesions.

3) *Characterize the effects of repetitive laser treatment for shifting the photoreceptors over extended distances, as a function of the exposure parameters and time delay between the successive treatments.*

As a part of the study of the retinal response to selective destruction of RPE, we evaluated migration and restoration of the RPE monolayer after multiple laser treatments. Figure 5A illustrates destruction of the RPE cells along the line of laser scanning (6 m/s, 2W, 100 μ m spot size). RPE cells then stretch and migrate from the undamaged areas, filling the lesion with a few days, as illustrated in Figure 5B. At one month there is no difference in appearance of the RPE in the treated and untreated areas (Figure 5C). At one month after the first treatment a second laser exposure was applied over the same area, and with the same parameters. It resulted in a very similar dynamics of the RPE healing, and no signs of damage could be observed one month after the second treatment, as illustrated in Figure 5D. At one month after the second treatment a third laser exposure was applied over the same area, and with the same parameters.

Similar dynamics of the RPE healing was observed, with complete recovery of the RPE monolayer, without any residual damage observed one month after the 3rd treatment (result not shown).

Similar dynamics was observed in RPE lesions of 200 and

400 μ m in width. These findings provide reassurance that RPE layer itself can heal rapidly and completely, even after multiple laser treatments over the same area, so the limiting factor in the healing dynamics of the retinal lesions is migration and rewiring of the photoreceptors.

4) *Develop image-guided pattern laser treatment that will apply laser exposures along the perimeter of the damage zone.*

We are working on development of the automated treatment software together with a manufacturer of the scanning laser – Topcon Medical Laser Systems Inc. The software package is being developed as a part of the Synthesis Graphic User Interface. The diagnostic image will be displayed on one screen

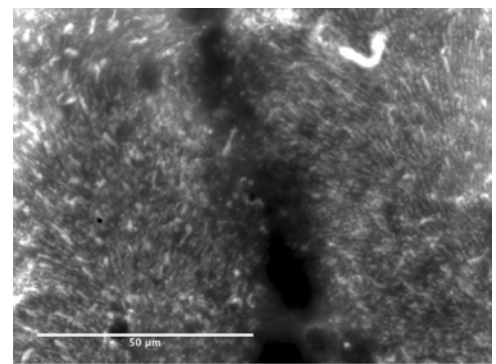


Figure 4. Fluorescent image of the photoreceptors covering the former 100 μ m lesion. Only a very narrow ($\sim 12\mu$ m) gap remains at 1 month. Scale bar is 50 μ m.

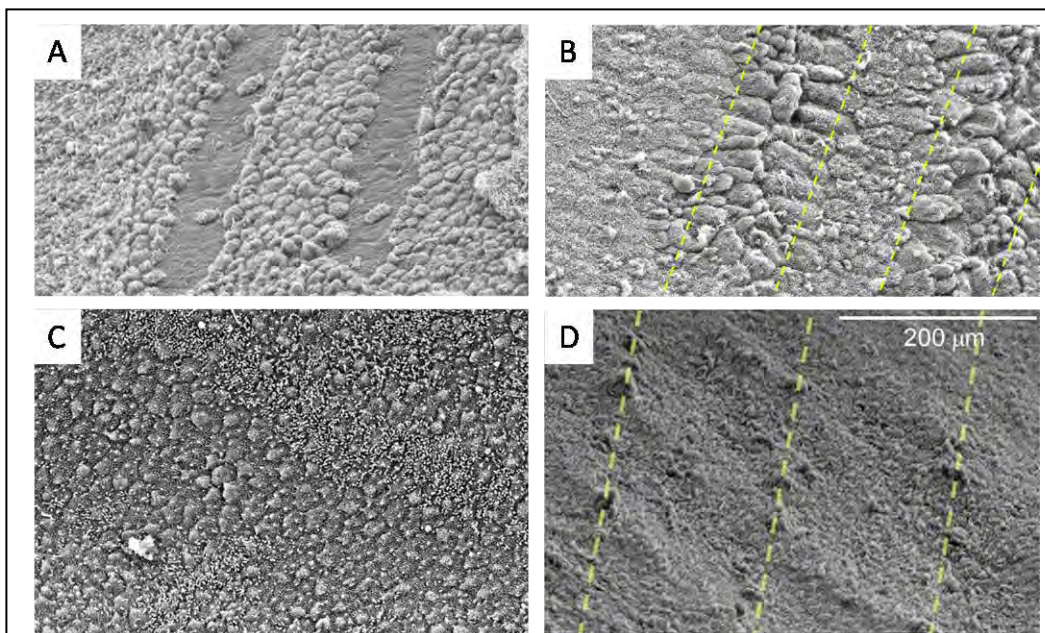


Figure 5. Fluorescent image of the photoreceptors covering the former 100 μ m lesion. Only a very narrow ($\sim 12\mu$ m) gap remains at 1 month. Scale bar is 50 μ m.

of the system, and the laser treatment parameters on the other. The planned treatment pattern will be then exported into the laser system, and applied relative to the fixation target projected onto the fovea by the aiming beam. Physician will maintain the fixation target on the patient's fovea, and parts of the treatment plan will be applied sequentially upon the press of the foot pedal. Every segment of the treatment pattern is applied within the eye fixation time – no longer than 200ms, so the pattern distortions due to eye motion could be avoided.

Key Research Accomplishments

- We developed a novel animal model of traumatic retinopathy using fast scanning of the retina with a continuous wave laser.
- Rapid scanning with a continuous laser can produce uniform areas of selective damage to the retina with adjustable size.
- The extent of the retinal damage can be adjusted by controlling the laser scanning velocity: damage limited to RPE layer ($v=6\text{m/s}$), damage limited to RPE and photoreceptors ($v=1\text{-}2\text{ m/s}$), or severe damage to the retina and choroid ($v=0.1\text{ m/s}$).
- RPE migrates and proliferates to fill the damage in the RPE monolayer within days, and completely restores normal anatomy within a month. Such recovery persists after multiple laser treatments of the same area.
- Photoreceptors migrate from the adjacent areas much slower: $100\text{ }\mu\text{m}$ lesion is almost completely recovered within a month, but $200\text{ }\mu\text{m}$ lesion is recovered only partially – by about 70%.
- Migrating photoreceptors rewire to the surviving local inner retinal neurons, thereby restoring normal retinal anatomy and function.
- Longer follow-up studies are in progress.

Reportable Outcomes

Refereed publications:

- Restoration of Retinal Structure and Function after Selective Photocoagulation. A. Sher, B.W. Jones, P. Huie, Y.M. Paulus, D. Lavinsky, L.S. Leung, H. Nomoto, C. Beier, R.E. Marc, and D. Palanker. *The Journal of Neuroscience* **33(16)**: 6800 – 6808 (2013).
- Subvisible Retinal Laser Therapy: Titration Algorithm and Tissue Response. D. Lavinsky, C. Sramek, J. Wang, P. Huie, R. Dalal, Y. Mandel, D. Palanker. *Retina*; published online July 2013.

Conference presentations:

- Optical Modulation of Transgene Expression in Retinal Pigment Epithelium. D. Palanker, D. Lavinsky, T. Chalberg, Y. Mandel, P. Huie, R. Dalal, M. Marmor. *Ophthalmic Technologies XXI, SPIE*, vol. 8567 (2013).
- Constructive Retinal Plasticity After Selective Ablation of the Photoreceptors Layer. A. Sher, B. Jones, P. Huie, Y. Paulus, D. Lavinsky, L.S. Leung, H. Nomoto, C. Beier, R. Marc, D. Palanker. ARVO Annual Meeting, Seattle, MAY 2013.

Funding Applied for:

NIH R01 grant # EY023020. Title: Restoration of retinal structure and function after selective

photocoagulation of photoreceptors. PI: A. Sher (UCSC), co-investigator: D. Palanker (Stanford U.).

Conclusion

Explosion or head impact may result in traumatic retinopathy due to damage of retinal pigment epithelium (RPE) and photoreceptors, leading to loss of sight. We developed a strategy for elimination or reduction of retinal scotomata and scarring using retinal plasticity. We established a model of traumatic retinopathy using selective laser coagulation of RPE and photoreceptors in rabbits, based on rapid scanning with a continuous laser. By adjusting the laser scanning speed one can precisely control duration of the exposure in each area, and thereby control the extent of tissue damage. This approach allows creating uniform areas of reproducible retinal damage with adjustable width and depth, mimicking the conditions of traumatic retinopathy.

We discovered that RPE migrates and proliferates to fill the damage in the RPE monolayer within days, and completely restores normal anatomy within a month. Such recovery persists after multiple laser treatments of the same area. Photoreceptors migrate from the adjacent areas much slower - within months. Migrating photoreceptors rewire to the surviving local inner retinal neurons, thereby restoring normal retinal anatomy and function. Longer follow-up of the healing, and studies of the effect of multiple treatments on sequential migration of the photoreceptors into the damaged zone are in progress.

References

1. Restoration of Retinal Structure and Function after Selective Photocoagulation. A. Sher, B.W. Jones, P. Huie, Y.M. Paulus, D. Lavinsky, L.S. Leung, H. Nomoto, C. Beier, R.E. Marc, and D. Palanker. *The Journal of Neuroscience* **33(16)**: 6800 – 6808 (2013).
2. Subvisible Retinal Laser Therapy: Titration Algorithm and Tissue Response. D. Lavinsky, C. Sramek, J. Wang, P. Huie, R. Dalal, Y. Mandel, D. Palanker. *Retina*; *published online July* 2013.
3. Selective RPE Therapy Using Continuous Laser Scanning. D. Lavinsky, P. Huie, R. Dalal, M. Marmor, D. Palanker, in preparation.

Restoration of Retinal Structure and Function after Selective Photocoagulation

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CNS neurons change their connectivity to accommodate a changing environment, form memories, or respond to injury. Plasticity in the adult mammalian retina after injury or disease was thought to be limited to restructuring resulting in abnormal retinal anatomy and function. Here we report that neurons in the mammalian retina change their connectivity and restore normal retinal anatomy and function after injury. Patches of photoreceptors in the rabbit retina were destroyed by selective laser photocoagulation, leaving retinal inner neurons (bipolar, amacrine, horizontal, ganglion cells) intact. Photoreceptors located outside of the damaged zone migrated to make new functional connections with deafferented bipolar cells located inside the lesion. The new connections restored ON and OFF responses in deafferented ganglion cells. This finding extends the previously perceived limits of restorative plasticity in the adult retina and allows for new approaches to retinal laser therapy free of current detrimental side effects such as scotomata and scarring.

Introduction

Neural plasticity in the mammalian CNS underlies processes of learning, memory formation, and changes due to disease or injury. The retina is the beginning of the visual pathway and exhibits adult plasticity associated mostly with injury or disease (Jones et al., 2003), although some forms of adaptive plasticity have been reported (Baylor, 1987; Wade and Wandell, 2002; Dunn et al., 2007; Olveczky et al., 2007). It has been long accepted that the extensive changes in retinal circuitry triggered by disease or injury are negative, leading to abnormal retinal anatomy and function (Jones and Marc, 2005; Marc et al., 2007).

It was discovered recently that continuity of the photoreceptor layer in rabbit and rodent retina can be restored after selective photocoagulation (Busch et al., 1999; Paulus et al., 2008; Belokopytov et al., 2010). Unlike more intense conventional burns, selective photocoagulation destroys only photoreceptors and retinal pigment epithelium (RPE), leaving cells in the inner

retinal layers intact. After a few days, RPE coverage is restored and, after a few weeks, the photoreceptor layer regains its continuity (Paulus et al., 2008). The most likely origin of the photoreceptors filling the lesion is a shift of healthy photoreceptors from the adjacent untreated areas (Zwick et al., 2008). Although these results indicate that migrating photoreceptors can fill in the lesion, little is known about the extent of the functional restoration.

This study explores the extent of functional restoration of the retinal network, focusing on the synaptogenesis between migrating photoreceptors and the deafferented bipolar cells located inside the lesion and the extent of the functional restoration of the OFF and ON pathways (Dowling and Boycott, 1966; Kolb, 1979; Calkins et al., 1996). The restoration of normal retinal structure and responses would demonstrate the existence of constructive adult mammalian retinal plasticity after injury. Such plasticity has multiple significant implications. Many studies have relied on retinal laser lesions as a model for investigation of cortical plasticity (Wandell and Smirnakis, 2009), assuming that retinal function in the lesions is lost permanently. Restoration of retinal sensitivity in the lesions might affect the interpretation of these studies. Furthermore, the process of establishing new connectivity between photoreceptors and the inner retinal neurons is important for guiding studies aimed at restoring sight in degenerate retina through genetic manipulation of the existing or surgical reintroduction of new retinal cells (MacLaren et al., 2006). The effect of photoreceptor migration over the laser lesion opens the door to new clinical approaches to retinal photocoagulation therapy that would allow restoration of continuity of the photoreceptor layer, thereby avoiding the deleterious side effects of the current standard laser treatment: scotomata and retinal scarring.

This study used histology, computational molecular phenotyping, and multielectrode recordings of retinal activity to inves-

Received Feb. 28, 2012; revised Feb. 21, 2013; accepted March 10, 2013.

Author contributions: A.S. and D.P. designed research; A.S., B.W.J., P.H., Y.M.P., D.L., L.-S.S.L., H.N., R.E.M., and D.P. performed research; A.S., B.W.J., D.L., C.B., and D.P. analyzed data; A.S. and D.P. wrote the paper.

This work was supported by Burroughs Wellcome Fund Career Award at the Scientific Interface, Pew Charitable Trusts Scholarship in the Biomedical Sciences, and National Institutes of Health Grant EY023020–01 (A.S.); Research to Prevent Blindness Career Development Award, The Edward N. & Della L. Thome Memorial Foundation (B.W.J.); National Institute of Health Grants EY02576, EY015128, EY014800 Vision Core, and National Science Foundation Grant 0941717 (R.E.M.); National Institute of Health Grant EY18608–05, Air Force Office of Scientific Research Grant FA9550-10-1-0503, Department of Defense Grant W81XWH-12-10575, and Stanford University Bio-X Grant (D.P.). We thank K. Mathieson, M. Krause, and A. Ng for technical assistance, A. Litke, W. Dabrowski, P. Hottoway, K. Mathieson, and S. Kachiguine for technical development, and B.A. Wandell for comments on the manuscript.

D.P. holds a patent licensed from Stanford University to Topcon Medical Laser Systems. The remaining authors declare no competing financial interests.

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DOI:10.1523/JNEUROSCI.1044-12.2013

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tigate the healing process in the rabbit retina. We observed that after the selective photocoagulation, bipolar cells located inside the lesioned site and ON- and OFF-center ganglion cells above the lesion regained their light responses, indicating that the migrating photoreceptors formed new connections with the underlying retinal circuitry.

Materials and Methods

Retinal laser application. The PASCAL laser system (Topcon Medical Laser Systems) provided 532 nm optical radiation with a nominally flat-top intensity profile. At the aerial image plane of the slit lamp microscope, the laser spots measured 200 and 400 μm in diameter, with the laser intensity transition from 10% to 90% occurring over 6 μm . Pulse duration was maintained at 20 ms. Laser power was titrated to produce ophthalmoscopically “barely visible” lesions, defined as a faint but clearly visible lightening of the fundus pigmentation (Jain et al., 2008). The power range for 200 μm spot size was 60–90 mW and for 400 μm spots, 150–200 mW. A single masked observer graded the clinical appearance of the laser lesions within 1 min after the treatment.

Thirty-seven male Dutch Belted rabbits (weight 2–3 kg) were used in accordance with the Association for Research in Vision and Ophthalmology Statement Regarding the Use of Animals in Ophthalmic and Vision Research after approval from the Stanford University Animal Institutional Review Board. The rabbits were anesthetized using ketamine hydrochloride (35 mg/kg, i.m.), xylazine (5 mg/kg, i.m.), and glycopyrrolate (0.1 mg/kg, i.m.) administered 15 min before the procedure. Pupillary dilation was achieved by 1 drop each of 1% tropicamide and 2.5% phenylephrine hydrochloride. Topical tetracaine 0.5% was instilled in the eye before the treatment.

Retinal histology and immunohistochemistry. For histology, 20 male rabbits were killed either 2 d or 2 months after treatment with a lethal dose of pentobarbital (Beuthanasia, 150 mg/kg, i.v.) in the marginal ear vein. Eyes were enucleated and fixed in 1.25% glutaraldehyde/1% paraformaldehyde in cacodylate buffer, pH 7.2, overnight at room temperature. The eyes were then postfixed in osmium tetroxide, dehydrated with a graded series of ethanol, processed with propylene oxide, embedded in an epoxy resin, and sectioned into 1- μm -thick sections. Samples were stained with toluidine blue and examined by light microscopy. For transmission electron microscopy (TEM), the tissue was cut into 100 nm sections using an ultramicrotome (Reichert-Jung Ultracut E; Leica) and stained with uranyl acetate and lead citrate. TEM micrographs were captured with a JEM-1400 microscope (JEOL).

Serial sections of the retina were examined, and at least four burns from two different animals were analyzed for each time point. By visually scanning the serial sections, the widest lesions corresponding to each burn were identified as corresponding to the center of the lesion.

For GFAP immunohistochemical analysis, samples were formalin fixed and embedded in paraffin. Four- to 5- μm -thick sections were then deparaffinized and immunohistochemistry was performed using anti-GFAP antibody conjugated to fluorescein. The sections were also counterstained with DAPI. In addition, 6–12 lesions were analyzed per setting in 6 male rabbits with the following time points: 1, 3, 7, and 14 d and 1, 2, 3, and 4 months.

For cell proliferation tests, two rabbits (four eyes) were used. These rabbits were a subset of the six used for GFAP staining. Light laser burns were administered 7 and 3 d before enucleation (10 lesions per eye). BrdU labeling reagent (10 ml; Invitrogen) was infused slowly in the marginal ear vein 2 h before killing the animal. Eyes and control samples from small intestines were fixed in formalin, embedded in paraffin, and sectioned into 4- to 5- μm -thick sections. Sections were then incubated with BrdU antibody and stained with horseradish peroxidase/diaminobenzidine. The sections were bleached with hydrogen peroxide to remove RPE pigment before light microscopy.

Computational molecular phenotyping. Fixed and embedded tissues were processed with computational molecular phenotyping (CMP). Two male rabbits were used in these experiments. Retinal neurons were classified by CMP as described previously (Marc and Jones, 2002) using an array of small molecule signatures (L-aspartate, L[SCAP]-glutamate, gly-

cine, L-glutamine, glutathione, GABA, taurine) in addition to antibodies targeting rod opsin and long-wavelength-sensitive opsin. Briefly, isolated eyes were fixed in 1% paraformaldehyde, 2.5% glutaraldehyde, 3% sucrose, and 0.01% CaCl_2 in 0.1 M phosphate buffer, pH 7.4. Tissues were then resected, dehydrated in graded methanol and acetone, and embedded in epoxy resin. Tissues were then serial sectioned at 200 nm onto 12-spot Teflon-coated slides (Cel-Line; Fisher Scientific). Antibody exposure and silver intensification were performed using a silver-intensification protocol described previously (Kalloniatis and Fletcher, 1993). Incubation of all antibodies generated against small molecular targets and opsins was performed overnight at room temperature and visualized with goat anti-rabbit secondary IgG coated with 1 nm gold (GE Healthcare Corporation) and silver intensified. Adobe Photoshop CS5 was used for final image generation.

Neural activity was assessed by detecting the ion-channel-mediated activity by probing permeation of the organic cation 1-amino-4-guanidobutane (AGB). AGB permeates activated α -amino-3-hydroxyl-5-methylisoxazole-4-propionic acid, kainate, and N-methyl-D-aspartate iGluR-gated channels as well as mGluR6-receptor-mediated channels on ON bipolar cells (Marc, 1999a; Marc, 1999b; Marc et al., 2005). These events are recorded as overall integrals of AGB flux through the channel revealing “snapshots” of neural activity (Marc, 1999a). Therefore, AGB renders a physiologic image of signaling of all neurons in the preparation. AGB signals are then multiplexed with the CMP data to reveal the extent of neural activity in the identified cell populations.

The AGB was prepared as described previously (Kalloniatis and Fletcher, 1993; Marc and Jones, 2002). In short, rabbits were anesthetized with a loading dose of ketamine hydrochloride (35 mg/kg, i.m.) and xylazine (5 mg/kg, i.m.). The eye was topically anesthetized with propacaine and dilated with 1% tropicamide and 2.5% phenylephrine hydrochloride. A standard three-port pars plana, partial vitrectomy was then performed and a 12 ml syringe was filled with O_2 -saturated AGB reagent (10 mg/ml) warmed to 37°C. The syringe containing AGB was attached to the infusion line and the contents infused into the eye over 30 min. A flash lamp was positioned over the eye at a distance of 8 inches and a 1 Hz alternating yellow and blue light was flashed for 30 min. The animal was killed by 1 ml of Beuthanasia-D (a solution of pentobarbital sodium and phenytoin sodium commonly used in dogs for painless and rapid euthanasia) delivered by cardiac puncture and the experimental eye infused with freshly prepared paraformaldehyde/glutaraldehyde fixative. The eye was fixed overnight, dehydrated, and embedded as described above in CMP methods.

Sequential 1- μm -thick slices were made, stained with toluidine blue, and examined by light microscopy. The center of the lesion was defined when the defective area visible in the photographs reached its maximum width. At this point, 200 nm slices for CMP were made. It usually takes a few sections before the full-width block face cuts are obtained. This procedure resulted in CMP analysis in slices that were within a few micrometers from the center of the lesion.

Electrophysiology. As described above, pattern of lesions was performed *in vivo* in nine male Dutch Belted rabbits 2 d and 2 months before the experiment. Eyes were then enucleated under terminal anesthesia under dim red light. The anterior portion of the eye and vitreous body were removed and a $4 \times 4 \text{ mm}^2$ piece of retina with 2–3 lesions was peeled from sclera and choroid under infrared microscope. This procedure resulted in most of the RPE granules remaining with the retina. The retinal piece was placed on the electrode array (512 electrodes; 1.7 mm^2 total area). During the experiment, the retina was perfused with oxygenated Ames’ solution, pH 7.4, and kept at 30°C. A computer-controlled CRT monitor displaying visual stimulus was focused on the photoreceptor layer by microscope objective. The image was delivered from below with the light passing through the transparent electrode array and the retina before reaching photoreceptors. After the experiment, photographs of the retina on the electrode array were taken in the transmitted light. These photographs showed locations of the lesions visible through hypopigmentation of RPE over the lesion relative to the recording electrodes. In addition, the observed pattern of hypopigmented spots was verified against the known pattern of lesions. The position of the visual stimulus relative to the electrodes was also measured, allowing us to

merge the spatial sensitivity profiles of the identified RGCs with the location of the lesions.

Voltage traces from individual electrodes were digitized at a 20 kHz sampling rate and used in the subsequent analysis to find spike times of individual RGCs (Litke et al., 2004). A few hundred RGCs were typically identified in a single retinal piece. The responses of the RGCs were characterized through their spike-triggered average (STA) response to a white noise black and white binary spatiotemporal white noise visual stimulus (checker size: 80 μ m; frame frequency: 60 Hz). For each identified RGC, the spatial sensitivity profile was characterized by isosensitivity contour. RGCs were classified as having ON- or OFF-set light sensitivity based on their STA time course (Litke et al., 2004).

Electrophysiological images (EIs) of an RGC consisted of voltage traces recorded on all 512 electrodes at the time of an RGC spike, and then averaged over all the spikes produced by the RGC (Petrusca et al., 2007). The location of the cell body was estimated by taking the center of mass of the EI voltage trace amplitudes on seven electrodes centered at the electrode with the largest signal.

Results

Continuity of the photoreceptor layer in

200 μ m lesions can be completely restored over 2 months after selective photocoagulation, with the RPE layer being restored in a few days (Fig. 1; Busch et al., 1999; Paulus et al., 2008; Paulus et al., 2011). In this procedure, the laser power and pulse duration are adjusted to damage only the RPE and photoreceptor layer. The inner retinal layers remain intact, with no signs of cell death detected at various time points (from 1 h to 4 months) after the procedure (Paulus et al., 2008). No significant difference ($p > 0.6$) was found between the density of the inner nuclear layer cells within the lesion and in untreated areas for either acute or healed (2-month-old) lesions. The comparison was done in three acute and three healed lesions by counting the number of cells per 100 μ m length of the retinal sections (toluidine blue staining). High-resolution imaging (Fig. 1C, TEM) of the healed lesion at 2 months revealed local synapses between photoreceptors and bipolar cells. The migrated photoreceptor exhibits normal nuclear anatomy with evidence of increased protein synthesis due to ribosomal upregulation, as well as normal ribbon synapses complete with vesicles. Nearby bipolar cell processes indicate local connection to the photoreceptor pedicle, as opposed to extended sprouting. This image does not exclude the possibility of the migrated photoreceptors also retaining their original synapses with bipolar cells outside of the lesion.

Functional consequences of the lesions were investigated using multielectrode recordings (Litke et al., 2004) of the rabbit retinal response to spatiotemporal white noise visual stimuli at various time points after photocoagulation. In each preparation, retinal activity was simultaneously recorded at the lesion and in the surrounding untreated retina. Each recording yielded several hundred identified RGCs, and their spatiotemporal properties were characterized through their STA response to a white noise stimulus (Chichilnisky, 2001). Recordings were performed at low photopic light levels. The resulting spatial sensitivity maps were

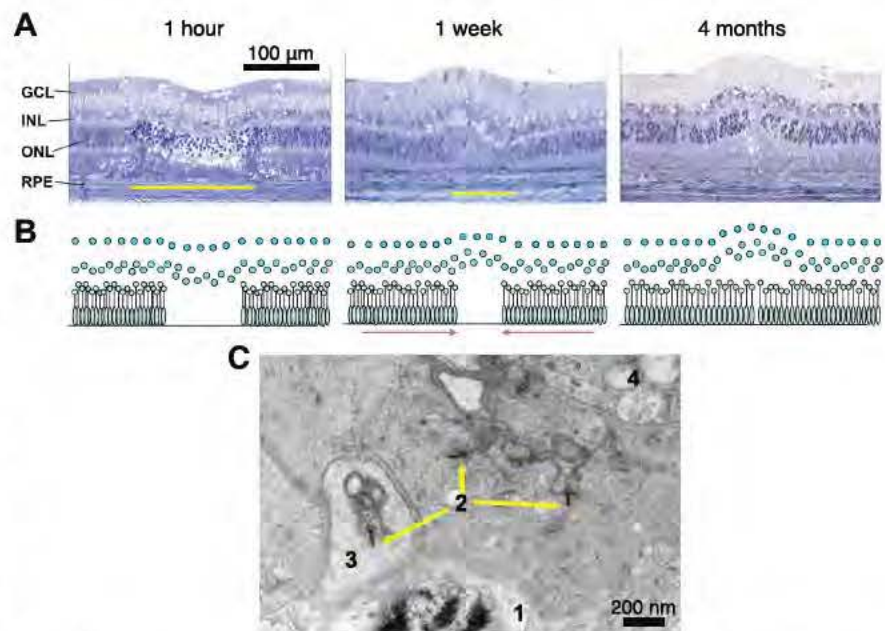


Figure 1. Restoration of retinal anatomy after photocoagulation. *A*, Toluidine-blue-stained retinal sections at various time points after the “barely visible” grade photocoagulation. Yellow bars show the lateral extent of the photoreceptor layer damage. *B*, Diagrammatic representation of the restoration of the photoreceptor layer continuity. *C*, TEM photograph of a central area of a healed 2-month-old lesion showing: (1) the photoreceptor nucleus, (2) photoreceptor ribbon synapses, (3) synaptic vesicles, and (4) bipolar cell processes.

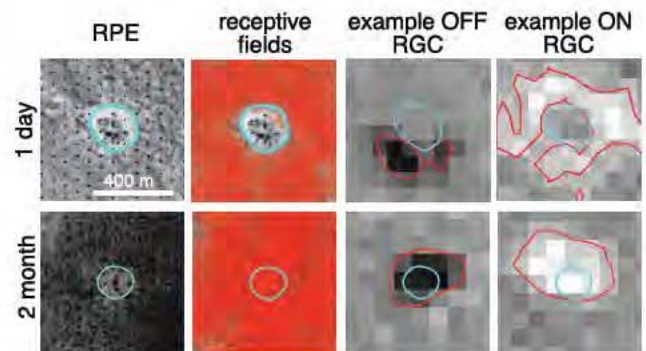


Figure 2. Restoration of retinal function after photocoagulation. Shown are 200 μ m lesions at 1 d (upper row) and 2 months (lower row) after the procedure. The first column on the left shows photographs of the retina on the multielectrode array taken after the recording. The regularly spaced black dots are electrodes and the grayish background shows RPE cells. The abnormal RPE zone is outlined by the cyan contour and indicates the lesion location. The second column from the left shows the photographs overlaid with the receptive fields of the recorded RGCs. The receptive field of each RGC is represented by an isosensitivity contour uniformly filled with semitransparent red color. The third and fourth columns from the left show spatial sensitivity profiles of example OFF and ON RGCs, as revealed through their STA response to the spatiotemporal white noise. The abnormal RPE zone (cyan contour) and the isosensitivity contours (red) are shown.

registered with respect to the lesion locations by photographing the retina on the array after each recording.

The extent of functional restoration of the inner retinal neurons was assessed using CMP (Marc and Jones, 2002) combined with probing of glutamatergic-driven response to flickering light using an AGB marker (Marc, 1999a).

Restoration of visual sensitivity

Figure 2 compares acute 1-d-old and 2-month-old “barely visible” grade lesions made with 200- μ m-diameter laser beam. The photographs of the retina on the electrode array (left panels)

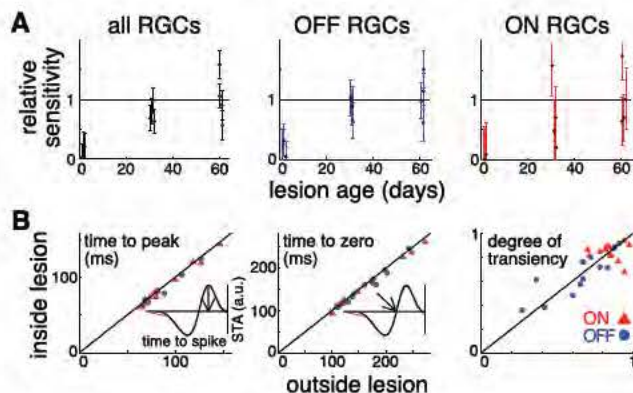


Figure 3. Restoration of retinal sensitivity and response kinetics in 200 μm lesions. **A**, Change in sensitivity over the lesion site with time. Sensitivity was calculated as a sum of STAs of all the RGCs recorded in a preparation. This sum within a lesion site was normalized to the average sensitivity over the healthy part of the retina. The uncertainties were estimated from the variability of the sensitivity over the healthy retinal regions. Plots for all RGCs and OFF- and ON-center RGCs are shown. Each point represents a separate lesion. Data from five retinal preparations are shown. **B**, Comparison of response kinetics between the inside and outside of the lesion portions of receptive fields of individual RGCs. Three aspects of the kinetics are shown: time to the first peak of the time course, time to the first zero crossing of the time course, and the degree of transiency measured through the relative areas of the first and second lobes of the time course. Inserts with a time course illustrate how the first two were measured. The red line in the example time course corresponds to the measured STA data and the smooth black line to the fit to that data. a.u. indicates arbitrary units. The plots include 27 cells that have receptive fields partially overlapping 4.2-month-old lesions in 2 retinal preparations. OFF-center RGCs are shown with blue circles; ON-center RGCs are shown with red triangles.

taken in transmitted light help identify the location of the lesion (blue outline) relative to the electrode array through changes in the RPE pigmentation. In the first days after the lesion, the receptive fields of the recorded RGCs were unresponsive over the acute lesions, resulting in a blind spot in the lesion zone. After 2 months, the blind spot was absent in the 200 μm lesion (Fig. 2). By 1 month, the average sensitivity over the lesion site measured through the STAs of the recorded RGCs approached that of the surrounding healthy retina and became indistinguishable ($p > 0.07$) from it by 2 months after the photocoagulation (Fig. 3A). This restoration occurred for both ON and OFF RGCs and in every healed 200 μm lesion located above the electrode array in our recordings, comprised of eight lesions across three retinal preparations. This measurement shows that the migrating photoreceptors had a functional connectivity to the inner retinal circuitry similar to that of the photoreceptors in the unaffected retinal area.

Details of connectivity between photoreceptors and various bipolar cell types play an important role in shaping the kinetics of retinal responses (Awatramani and Slaughter, 2000; DeVries, 2000; DeVries et al., 2006). Significant changes in response kinetics inside and close to the healed lesion indicate that this connectivity has been disturbed as a result of the photoreceptor migration. We quantified the kinetics of RGC responses through the STA time course, calculated as the average of the STA amplitude in the locations where the STA signal was above 3 SDs of the noise. The time course of each RGC was then fitted with a difference of low-pass filters (Chichilnisky and Kalmar, 2002) and three parameters were extracted from the fits. Each parameter reflects a different aspect of the cell's response assuming that the cell integrates information linearly over time. Time to the first peak of the STA characterizes the response latency, time to the first zero indicates the time it takes for the response to reach its maximum, and the degree of transiency predicts how close to the

baseline the spike rate returns long after the presentation of the light intensity step. The degree of transiency was calculated as $1 - \text{abs}(S)/S_{\text{abs}}$, where S and S_{abs} are integrals of the fitted time course and its absolute value, respectively. We did not observe a significant difference between the averages of each of these parameters over the cells that had receptive fields overlapping with the healed lesions and the cells that had receptive fields away from the lesions ($p > 0.1$). We then compared the kinetics of the individual RGC's visual responses driven by the photoreceptors that migrated inside the lesion to those that remained outside. A total of 27 RGCs that had their receptive fields overlapping with 4 healed 2-month-old 200 μm lesions were identified. The receptive field of each of the cells was divided into the inside- and outside-of-the-lesion parts. STA time courses were calculated separately for each part. The two time courses were then fitted independently. Figure 3B shows that the response kinetics were similar inside and outside of the healed lesions for each of the tested RGCs. Such similarity further strengthens the conclusion that the migrated photoreceptors had normal connectivity with the underlying retinal neurons, in particular with bipolar cells. Note that the data in Figure 3B show that the responses observed within the lesioned areas did not arise from intrinsically photosensitive RGCs (Dacey et al., 2005; Berson, 2007; Schmidt et al., 2011). Intrinsic responses of intrinsically photosensitive RGCs have longer latencies (order of seconds) compared with photoreceptor-mediated responses. The measured latencies of the visual responses within the lesioned areas were ~ 100 ms, which is consistent with a photoreceptor-driven response.

Migrating photoreceptors could retain functional connectivity to their postsynaptic bipolar cells. In such an event, receptive fields that were originally adjacent to the lesion would extend into the lesioned area after the healing. Such a process would result in the enlarged receptive fields overlapping the healed lesion. Contrary to this prediction, we did not observe a statistically significant difference ($p = 0.64$) between the average receptive field sizes of the RGCs overlapping with the healed lesions (275 ± 34 μm) and the ones overlapping with the same number of the similarly sized circles mapped over the healthy retina (299 ± 38 μm). Both numbers represent (mean $\pm$ SEM). The receptive field size of each cell was calculated as the diameter of a circle with the area equivalent to the $1-\sigma$ contour of a two-dimensional Gaussian fitted to the STA frame containing the largest signal (Petrusca et al., 2007).

These results show that restoring the anatomical continuity of the photoreceptor layer after selective photocoagulation leads to restoration of retinal sensitivity at the coagulation site. Furthermore, this restoration takes place in the two major visual pathways sensitive to the ON- and OFF-set of light and does not lead to any major distortions in either spatial or temporal response properties of RGCs. For larger (400 μm) lesions, the blind spot was greatly reduced at 2 months but did not disappear completely (2 lesions over 2 preparations). This suggests that the lateral distance the photoreceptors can shift during the healing process is limited to about 150 μm (Busch et al., 1999; Paulus et al., 2008).

Formation of new synapses between cone photoreceptors and bipolar cells

Three different mechanisms can account for the observed restoration of visual sensitivity over the lesion site. The migrating photoreceptors could: (1) retain their connections to their old postsynaptic partners without forming new ones, (2) abandon their old postsynaptic partners and form entirely new connections with the bipolar cells in the lesioned region, or (3) retain

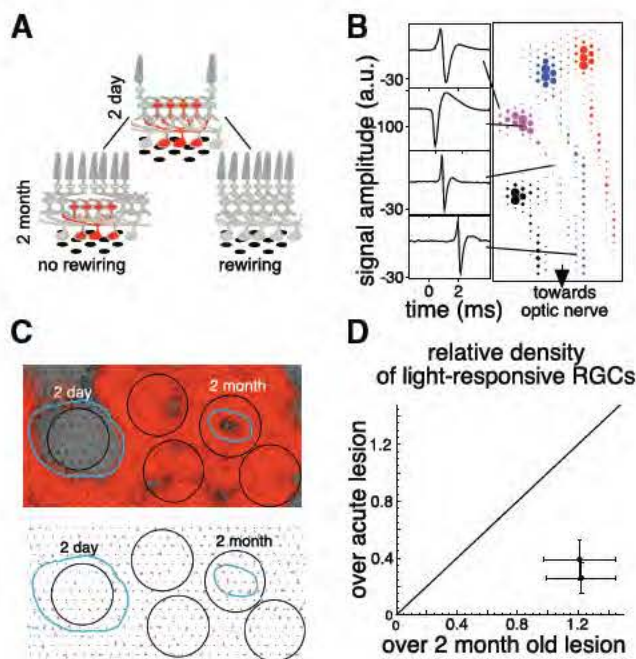


Figure 4. Restoration of retinal circuitry under the lesion. **A**, Schematic of two outcomes of the photoreceptor migration: “no rewiring,” which leaves this circuitry without the input of photoreceptors located above it, and “rewiring,” which leads to restoration of retinal circuitry under the lesion. **B**, EIs of four cells from one retinal preparation. Sample voltage waveforms corresponding to dendritic, cell body, and axon locations are shown for one cell on the left. **C**, Top: Photograph of retinal preparation with 2-d-old and 2-month-old lesions placed over the multielectrode array with the overlaid receptive field of the recorded RGCs. The RPE abnormality zones for the two lesions are outlined in cyan. Bottom: The soma locations of the RGCs that responded to visual stimulus (magenta dots). Two of the 400- μ m-diameter black circles are centered on the two lesions and the other three are located randomly over the healthy retina. **D**, The comparison of densities of RGCs responsive to visual stimulus located within the 400- μ m-diameter circle centered over the acute (1, 2 d) and healed (2 months) lesions for 2 retinas. The densities are relative to the RGC densities in the healthy regions of the same retinas.

some old connections and also form new ones. To distinguish between these possibilities, the density of light-sensitive RGCs was measured under the lesion site shortly after the photocoagulation procedure and after 2 months. Because of the vertical architecture of retinal connectivity, the density of the light-sensitive RGCs under the lesion is expected to decrease after the procedure. If no new connections are formed by the migrating photoreceptors (option 1 above), this reduced density should remain after the healing period. If new connections are formed (options 2 and 3 above), the density of light-responding RGCs above the lesions should increase. Figure 4A depicts these two possible outcomes.

To measure the density of light-sensitive RGCs, we estimated positions of the cell bodies of the recorded RGCs. The electrical footprint of an RGC, called an EI (Petrusca et al., 2007), is an average electrical activity recorded on the multielectrode array when the RGC produces an action potential (see Materials and Methods). The EI provides information about spatial location of the RGC's cell soma, axonal trajectory, and, in some cases, the dendritic arbor (Fig. 4B).

The number of light-sensitive RGCs within 400- μ m-diameter circles centered on the lesion sites was compared with the number of cells within the same size circles located over untreated parts of the retina. Figure 4C shows one such measurement in a preparation in which 2-d- and 2-month-old 400 μ m diameter lesions were placed over the multielectrode array. The density of

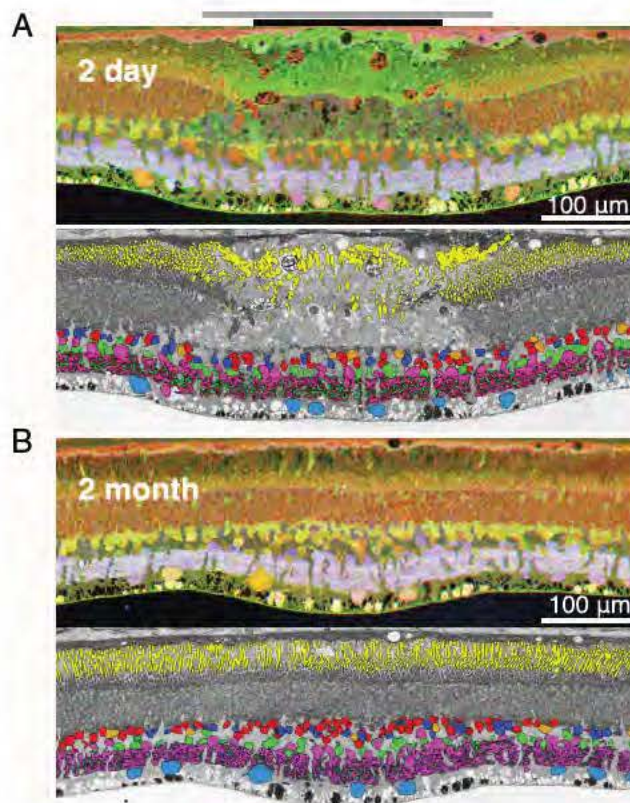


Figure 5. Restoration of the light-evoked activity in the inner retina. **A**, Top: Section traversing the center of the 2-d-old lesion stained for glutamate (red), AGB (green), and GABA (blue). Bottom: Same section with the major retinal cell types identified through CMP clustering. The color coding is as follows: horizontal cells are shown in orange, hyperpolarizing cone bipolar and depolarizing rod bipolar cells in red, depolarizing cone bipolar cells in dark blue, GABAergic amacrine cells in magenta, glycinergic amacrine cells in green, and ganglion cells in light blue. The black bar at the top of the panel indicates the area of destroyed photoreceptors; gray bar shows the zone of surviving photoreceptors with detached or damaged outer segments. **B**, Section traversing the center of the 2-month-old lesion. Same antibody staining and cell classifications as for the acute lesion are shown. Yellow color in both classification panels indicates location of rhodopsin.

light-responsive RGCs over acute lesions was 3 times lower than normal, but in the 2-month-old lesions, RGC density recovered to the same level as that found in untreated parts of the retina. This measurement was performed in two retinal preparations and yielded similar results (Fig. 4D). Note that the number of recorded RGCs did not vary significantly ($p = 0.24$ and $p = 0.29$ for the two preparations, respectively) between acute and healed lesions, indicating that the RGCs in the acute lesion site were active, but did not respond to the visual stimulus.

Additional evidence that the migrated photoreceptors were making new functional synaptic contacts to the bipolar cells over the lesion was obtained by performing AGB labeling of the photocoagulated retina exposed to flickering blue/yellow light *in vivo*. AGB permeates activated iGluR and mGluR6 channels and reveals glutamatergic neuronal activity in response to the light stimulus. Identities of individual cells were determined through CMP clustering. We identified hyperpolarizing and depolarizing bipolar cells, glycinergic and GABAergic amacrine cells, horizontal cells, and ganglion cells. Figure 5 shows CMP of the 200 μ m lesions at 2 d and 2 months after the photocoagulation. Two panels are shown for each time point: one summarizes the results of clustering and another shows overlay of three signals:

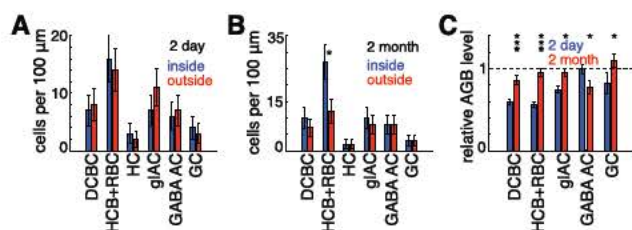


Figure 6. Presence of the neuronal cell types within acute and healed lesion sites. **A**, Number of cells per 100 μm length in 2-d-old lesion section shown in Figure 5A. Cell counts for the following six neuronal cell types are shown: depolarizing cone bipolar cells (DCBC), hyperpolarizing cone bipolar cells and rod bipolar cells (HCB+RBC), horizontal cells (HC), glycinergic amacrine cells (gIAC), GABAergic amacrine cells (GABA AC), and ganglion cells (GC). For each of these cell types, blue (left) and red (right) bars show cell numbers inside and outside the lesioned area, respectively. **B**, Number of cells per 100 μm length in the 2-month-old lesion section shown in Figure 5B. Abbreviations and color (order) scheme are the same as in **A**. **C**, AGB levels for different cell types inside the lesions in the sections shown in Figure 5. Blue (left) and red (right) bars correspond to the AGB levels in the 2-d-old and 2-month-old lesions, respectively. For each cell type, the average AGB level among the cells within the lesion was normalized by the average AGB level calculated over the cells of the same type located outside the lesion in the same section. In all plots, * $p < 0.05$, ** $p < 0.01$, and *** $p < 0.001$. Error bars correspond to counting uncertainties ($n^{1/2}$) for **A** and **B** and SEM for **C**.

L-glutamate, AGB, and GABA, marked with red, green, and blue, respectively.

At the 2 d time point (Fig. 5A), the photoreceptor layer was completely destroyed, whereas all of the inner retinal neuronal types were still present in the lesioned area. Because cells within the lesion exhibited normal small molecule signatures and the density of each cell type within the lesion was similar to that in the surrounding healthy retina (Fig. 6A), we conclude that the inner retinal cells within the lesion were not significantly affected. This confirms the previous histological assertion of highly selective destruction of photoreceptors based on toluidine blue staining. Outside of the lesion, the neurons, especially those in the inner nuclear layer, showed colocalization of glutamate (red) and AGB (green) signals, resulting in the yellow coloring of the cell bodies. Inside of the lesion, most of the inner nuclear layer cells showed glutamate signal but much lower AGB levels and appeared red in color, as one would expect, because this part of the retina no longer receives direct input from photoreceptors.

At 2 months, the retinal section across the center of the lesioned site (Fig. 5B) shows that the photoreceptors had filled in the damaged zone and that all of the major cell types are well represented inside the lesion (Fig. 6B). The light responsiveness of the cells in the inner nuclear layer is close to that of the cells outside of the lesion; that is, the AGB signal in the INL neurons is similar inside (Fig. 5B, center) and outside of the lesion compared with the stark differences observed in the 2-d-old lesion (Fig. 5A).

The light-evoked activity of inner-retinal neurons was further quantified by combining results of CMP clustering with AGB signaling. Average AGB concentration was measured in each of the major cell types inside the lesioned area and then normalized to the average AGB concentration of the same cell type in the surrounding tissue. Between the 2-d-old and 2-month-old lesions, this relative AGB concentration increased significantly for hyperpolarizing cone bipolar and rod bipolar cells ($p < 0.001$), depolarizing cone bipolar cells ($p < 0.001$), ganglion ($p < 0.05$), and glycinergic amacrine cells ($p < 0.05$) (Fig. 6C). It did not increase for the GABAergic amacrine cells. The largest increase was measured in bipolar cells, which have the smallest dendritic trees of all these cell types and would therefore be the most affected by the destruction of the photoreceptors; that is, the larger

portion of the wider field cells (ganglion and amacrine) would have inputs from outside the lesion. GABAergic amacrine cells are predominantly wide field and therefore would be the least affected by the photocoagulation of the small photoreceptor patch. The decrease in the AGB levels inside GABAergic amacrine cells in the healed lesion ($p < 0.05$) might be connected with real retinal restructuring or could be caused by a statistical fluctuation. Neither possibility can be excluded based on the data. We did not include horizontal cells in this analysis due to their small number. The apparent increase in the number of inner nuclear layer neurons in the CMP preparation (Fig. 5B) due to the increased number of hyperpolarizing cone and rod bipolar cells (Fig. 6C) in the healed lesion has not been confirmed statistically by histological analysis of a large number of lesions (Fig. 1; Paulus et al., 2008), and therefore should not be considered a typical occurrence.

The observed restoration of RGC visual sensitivity, physiological activity of the inner retinal neurons, and local synapses in the healed lesion (Fig. 1, TEM) strongly indicate that migrating photoreceptors make new functional connections to the bipolar cells that had their presynaptic photoreceptors destroyed by photocoagulation.

Discussion

We explored the extent of retinal functional restoration after selective destruction of the photoreceptors by laser photocoagulation in rabbits. Migration of the photoreceptors into the coagulated area resulted in restoration of visual sensitivity over the lesion site. The functional restoration was virtually complete for 200 μm lesions. The 400 μm lesions resulted in a reduced but persistent blind spot at 2 months. Both ON- and OFF-center RGCs exhibited the same degree of functional restoration. We detected no significant change in the receptive field size or response kinetics of the RGCs receiving inputs from the migrated photoreceptors. The RGCs located at the lesion regained light sensitivity after the healing. Inner retinal neurons at the lesion also normalized their integrated light-evoked activity as measured through AGB-mediated recording. These findings indicate that significant (and in some cases almost complete) restoration of retinal structure and function is possible through retinal plasticity evoked by the selective destruction of the photoreceptor layer in adult mammalian retina.

Mechanism of the photoreceptor layer restoration

The observed repopulation of the lesion with photoreceptors is most likely caused by photoreceptor redistribution in which healthy photoreceptors from outside of the lesion physically shift into the vacated space (Zwick et al., 2008). An alternative hypothesis would include large-scale neurogenesis of the new photoreceptors, which has never been observed in the adult mammalian retina (but see Osakada et al., 2007). To assess the extent of neurogenesis, we performed BrdU staining of retinal lesions at 3 and 7 d after photocoagulation (the time period with the fastest change in the lesion size). No BrdU expression was detected in the inner retina (data not shown), further supporting the migration hypothesis.

The mechanism of photoreceptor migration is unknown. One possibility is that it is mediated by Mueller cells that form a glial matrix filling the lesion in the photoreceptor layer shortly after photocoagulation, which then slowly contracts, bringing adjacent photoreceptor cell bodies with them. Activation of Mueller cells in and around the lesion and their dynamics can be observed through GFAP staining, as shown in Figure 7. Slight hypertrophy

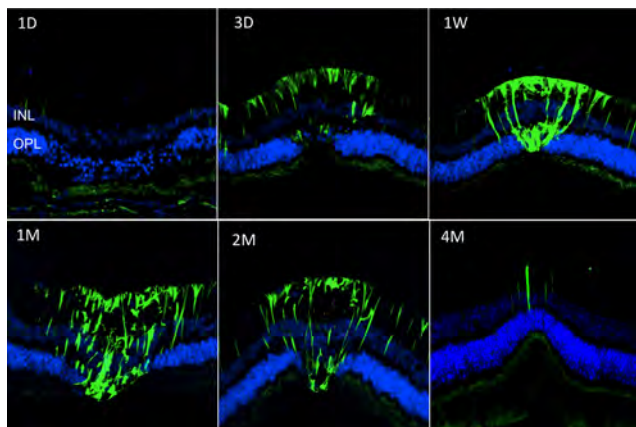


Figure 7. Mueller cell activation after photocoagulation. GFAP staining (green) shows activation of Mueller cells starting at 3 d (3D) and ending between 2 and 4 months (2M, 4M) after selective photocoagulation. DAPI staining (blue) shows outer and inner nuclear layers.

of Mueller glia also can be noticed in the inner nuclear layer in Figure 5A, where it is manifested by the slightly enlarged space between the cell bodies in the inner nuclear layer.

Restoration of retinal function and structure through synaptogenesis

The observed restoration of visual sensitivity over the lesion site shows that the migrated photoreceptors have functional connectivity to the retinal circuitry. In the healthy retina, cone photoreceptors synapse onto both hyperpolarizing and depolarizing bipolar cells creating two major retinal pathways responsive to ON- and OFF-set of light. The restoration of both retinal pathways strongly indicates that the migrated cone photoreceptors have functional synapses onto both broad types of bipolar cells. Moreover, the observed visual sensitivity of the retinal ganglion cells located directly under the lesion, combined with the activation of inner retinal neurons located in the same area, suggests that the migrated photoreceptors synapse onto the bipolar cells that had their previous presynaptic photoreceptors destroyed by photocoagulation. Therefore, photoreceptors not only migrate in space and retain their photosensitivity, but they also form new synapses with bipolar cells, thereby restoring retinal structure and function at the lesion site. The TEM photographs show normal synapses of the photoreceptors that have migrated into the lesion. The details of the synaptic connections between cone photoreceptors and bipolar cells have a significant influence on the kinetics of the RGC light responses (Awatramani and Slaughter, 2000; DeVries, 2000; DeVries et al., 2006). The absence of significant differences in the RGC response kinetics between the areas inside and outside of the healed lesion indicates that the structure of the newly formed synapses between photoreceptors and bipolar cells is similar to that found in the healthy retina. Previous studies of injury-evoked retinal plasticity report abnormal photoreceptor synapse formation (Pinaud et al., 2006). It is possible that the difference in the outcomes is due to the new synapses formed by the healthy photoreceptors migrating into the lesion in the case of selective retinal photocoagulation, as opposed to compromised photoreceptors going through synaptic sprouting, as in the case of retinal detachment.

How close is the resulting circuitry to the original? The exact answer to this question would require extensive further anatomical and functional studies. For example, the present study does not address directly the possibility that the migrating photore-

ceptors preserve some of their original connectivity to the bipolar and horizontal cells. We did not observe any anatomically obvious, human-fovea-like displacement between the photoreceptors and the cells in the inner nuclear layer. However, based on our measurements, we cannot exclude a possibility that some of the migrated photoreceptors retain their synapses with bipolar cells outside the lesion. One piece of evidence arguing against such remaining connections is that we did not observe significant enlargement of the receptive fields overlapping the healed lesions.

One of the hallmarks of negative retinal plasticity is somatic migration of various retinal cell types from their respective layers and changes in the inner retinal synaptic structure (Jones et al., 2003; Jones and Marc, 2005; Marc et al., 2007). We did not observe these well described traits of negative retinal plasticity: the major retinal cell types identified through CMP clustering remained in their respective layers and the overall pattern of the GABAergic and glycinergic amacrine cell processes was not disturbed throughout the healing process. This apparent absence of negative plasticity might be explained by a combination of the following factors. Fast photoreceptor migration and rewiring ensures that there is not enough time for the inner retinal rewiring and cell migration to take hold. In addition, the normal process of photoreceptor cell death in a retinal degenerative disease leaves some period of time (from hours to years) in which photoreceptor cells and their mitochondrial machinery have time to signal cell stress and potential inflammatory pathways. In photocoagulation, none of this is possible because the lesion is immediate and complete. In addition, the small size of the lesions allows at least some normal signaling, mostly through the wide field amacrine cells, to occur in the inner retina, thereby slowing down the negative plasticity. It would be interesting to test this hypothesis by observing larger lesions in which the photoreceptors do not fill the whole lesioned area. Over time, we would expect to observe negative plasticity in the persistent portion of the lesion. Even though we did not observe any obvious retinal restructuring, we cannot conclusively exclude a possibility of some changes in the inner retinal connectivity. Future functional and structural studies are needed to measure the exact extent of restoration of the complex retinal circuitry.

It is important to note that the functional measurements in this study were performed at photopic light levels; therefore, the degree to which rod photoreceptor pathway is restored remains to be investigated.

Laser photocoagulation of the retina provides a convenient model for studies of the mechanisms of retinal network response to injury or disease, potentially revealing processes responsible for its development and plasticity.

Potential improvement of retinal laser therapy

Since its introduction nearly 50 years ago, laser photocoagulation remains the standard of care for long-term therapy of several retinopathies. Laser treatment is thought to limit neovascularization by destroying retinal cells in the poorly perfused portions of the retina, thus limiting hypoxia and decreasing the production of angiogenic factors (Jennings et al., 1991; Matsumoto et al., 1994; Spranger et al., 2000; Sánchez et al., 2007). Because photoreceptors are the most numerous and metabolically active cells in the retina, pan-retinal photocoagulation for proliferative diabetic retinopathy involves the purposeful destruction of a significant fraction of photoreceptors (Little et al., 1970).

Although pan-retinal photocoagulation is a highly effective approach to halting angiogenesis, it results in permanent retinal scarring and decreased peripheral, color, and night vision

(Higgins et al., 1986; Shimura et al., 2005). Focal and grid laser photocoagulation is an effective treatment of macular edema, but also causes scotomata and scarring (Morgan and Schatz, 1989; Schatz et al., 1991; Early Treatment Diabetic Retinopathy Study Research Group, 1995). Laser burns can enlarge postoperatively and cause choroidal neovascularization (Lewen, 1988; Lewis et al., 1990), subretinal fibrosis (Guyer et al., 1992; Rutledge et al., 1993; Lövestam-Adrian and Agardh, 2000), and additional visual field loss (Striph et al., 1988; Hudson et al., 1998; Ishiko et al., 1998; Mainster, 1999; Sinclair et al., 1999). Over time, loss of one class of retinal cells may, by *trans*-synaptic degeneration and associated inflammation, result in the loss of other retinal neurons (Stone, 1950; Birnbach et al., 1994) and RPE remodeling (Framme et al., 2009) or retinal remodeling (Marc et al., 2007).

The discovered retinal plasticity holds promise for improved laser treatment based on smaller spot size and selective destruction of photoreceptors while avoiding damage to the inner retinal neurons. This modification of current clinical therapy retains the postulated therapeutic effect through a reduction in the number of photoreceptors, but avoids permanent scarring and restores normal retinal function over the lesion sites, thus ameliorating or even eradicating the side effects associated with the current standard of care.

References

- Early Treatment Diabetic Retinopathy Study Research Group (1995) Focal photocoagulation treatment of diabetic macular edema—relationship of treatment effect to fluorescein angiographic and other retinal characteristics at baseline: ETDRS report no. 19. *Arch Ophthalmol* 113:1144–1155. [Medline](#)
- Awatramani GB, Slaughter MM (2000) Origin of transient and sustained responses in ganglion cells of the retina. *J Neurosci* 20:7087–7095. [Medline](#)
- Baylor DA (1987) Photoreceptor signals and vision. Proctor lecture. *Invest Ophthalmol Vis Sci* 28:34–49. [Medline](#)
- Belokopytov M, Belkin M, Dubinsky G, Epstein Y, Rosner M (2010) Development and recovery of laser-induced retinal lesion in rats. *Retina* 30:662–670. [CrossRef Medline](#)
- Berson DM (2007) Phototransduction in ganglion-cell photoreceptors. *Pflügers Arch* 454:849–855. [CrossRef Medline](#)
- Birnbach CD, Järveläinen M, Possin DE, Milam AH (1994) Histopathology and immunocytochemistry of the neurosensory retina in fundus flavimaculatus. *Ophthalmology* 101:1211–1219. [Medline](#)
- Busch EM, Gorgels TG, Van Norren D (1999) Filling-in after focal loss of photoreceptors in rat retina. *Exp Eye Res* 68:485–492. [CrossRef Medline](#)
- Calkins DJ, Tsukamoto Y, Sterling P (1996) Foveal cones form basal as well as invaginating junctions with diffuse ON bipolar cells. *Vis Res* 36:3373–3381. [CrossRef Medline](#)
- Chichilnisky EJ (2001) A simple white noise analysis of neuronal light responses. *Network* 12:199–213. [Medline](#)
- Chichilnisky EJ, Kalmar RS (2002) Functional asymmetries in ON and OFF ganglion cells of primate retina. *J Neurosci* 22:2737–2747. [Medline](#)
- Dacey DM, Liao HW, Peterson BB, Robinson FR, Smith VC, Pokorny J, Yau KW, Gamlin PD (2005) Melanopsin-expressing ganglion cells in primate retina signal colour and irradiance and project to the LGN. *Nature* 433:749–754. [CrossRef Medline](#)
- DeVries SH (2000) Bipolar cells use kainate and AMPA receptors to filter visual information into separate channels. *Neuron* 28:847–856. [CrossRef Medline](#)
- DeVries SH, Li W, Saszik S (2006) Parallel processing in two transmitter microenvironments at the cone photoreceptor synapse. *Neuron* 50:735–748. [CrossRef Medline](#)
- Dowling JE, Boycott BB (1966) Organization of the primate retina: electron microscopy. *Proc R Soc Lond B Biol Sci* 166:80–111. [CrossRef Medline](#)
- Dunn FA, Lankheet MJ, Rieke F (2007) Light adaptation in cone vision involves switching between receptor and post-receptor sites. *Nature* 449:603–606. [CrossRef Medline](#)
- Framme C, Walter A, Prahs P, Regler R, Theisen-Kunde D, Alt C, Brinkmann R (2009) Structural changes of the retina after conventional laser photocoagulation and selective retina treatment (SRT) in spectral domain OCT. *Curr Eye Res* 34:568–579. [CrossRef Medline](#)
- Guyer DR, D'Amico DJ, Smith CW (1992) Subretinal fibrosis after laser photocoagulation for diabetic macular edema. *Am J Ophthalmol* 113:652–656. [Medline](#)
- Higgins KE, Meyers SM, Jaffe MJ, Roy MS, de Monasterio FM (1986) Temporary loss of foveal contrast sensitivity associated with panretinal photocoagulation. *Arch Ophthalmol* 104:997–1003. [CrossRef Medline](#)
- Hudson C, Flanagan JG, Turner GS, Chen HC, Young LB, McLeod D (1998) Influence of laser photocoagulation for clinically significant diabetic macular oedema (DMO) on short-wavelength and conventional automated perimetry. *Diabetologia* 41:1283–1292. [CrossRef Medline](#)
- Ishiko S, Ogasawara H, Yoshida A, Hanada K (1998) The use of scanning laser ophthalmoscope microperimetry to detect visual impairment caused by macular photocoagulation. *Ophthalmic Surg Lasers* 29:95–98. [Medline](#)
- Jain A, Blumenkranz MS, Paulus Y, Wiltberger MW, Andersen DE, Huie P, Palanker D (2008) Effect of pulse duration on size and character of the lesion in retinal photocoagulation. *Arch Ophthalmol* 126:78–85. [CrossRef Medline](#)
- Jennings PE, MacEwen CJ, Fallon TJ, Scott N, Haining WM, Belch JJ (1991) Oxidative effects of laser photocoagulation. *Free Radic Biol Med* 11:327–330. [CrossRef Medline](#)
- Jones BW, Marc RE (2005) Retinal remodeling during retinal degeneration. *Exp Eye Res* 81:123–137. [CrossRef Medline](#)
- Jones BW, Watt CB, Frederick JM, Baehr W, Chen CK, Levine EM, Milam AH, Lavail MM, Marc RE (2003) Retinal remodeling triggered by photoreceptor degenerations. *J Comp Neurol* 464:1–16. [CrossRef Medline](#)
- Kalloniatis M, Fletcher EL (1993) Immunocytochemical localization of the amino acid neurotransmitters in the chicken retina. *J Comp Neurol* 336:174–193. [CrossRef Medline](#)
- Kolb H (1979) The inner plexiform layer in the retina of the cat: electron microscopic observations. *J Neurocytol* 8:295–329. [CrossRef Medline](#)
- Lewen RM (1988) Subretinal neovascularization complicating laser photocoagulation of diabetic maculopathy. *Ophthalmic Surg* 19:734–737. [Medline](#)
- Lewis H, Schachar AP, Haimann MH, Haller JA, Quinlan P, von Fricken MA, Fine SL, Murphy RP. Choroidal neovascularization after laser photocoagulation for diabetic macular edema. *Ophthalmology* 97:503–510, 1990; discussion 510–501.
- Litke AM, Bezayiff N, Chichilnisky EJ, Cunningham W, Dabrowski W, Grillo AA, Grivich M, Grybos P, Hottowy P, Kachiguine S, Kalmar RS, Mathieson K, Petrusca D, Rahman A, Sher A (2004) What does the eye tell the brain?: Development of a system for the large-scale recording of retinal output activity. *IEEE Transactions on Nuclear Science* 51:1434–1440. [CrossRef](#)
- Little HL, Zweng HC, Peabody RR (1970) Argon laser slit-lamp retinal photocoagulation. *Trans Am Acad Ophthalmol Otolaryngol* 74:85–97. [Medline](#)
- Lövestam-Adrian M, Agardh E (2000) Photocoagulation of diabetic macular oedema—complications and visual outcome. *Acta Ophthalmol Scand* 78:667–671. [CrossRef Medline](#)
- MacLaren RE, Pearson RA, MacNeil A, Douglas RH, Salt TE, Akimoto M, Swaroop A, Sowden JC, Ali RR (2006) Retinal repair by transplantation of photoreceptor precursors. *Nature* 444:203–207. [CrossRef Medline](#)
- Mainster MA (1999) Decreasing retinal photocoagulation damage: principles and techniques. *Semin Ophthalmol* 14:200–209. [CrossRef Medline](#)
- Marc RE (1999a) Mapping glutamatergic drive in the vertebrate retina with a channel-permeant organic cation. *J Comp Neurol* 407:47–64. [CrossRef Medline](#)
- Marc RE (1999b) Kainate activation of horizontal, bipolar, amacrine, and ganglion cells in the rabbit retina. *J Comp Neurol* 407:65–76. [CrossRef Medline](#)
- Marc RE, Jones BW (2002) Molecular phenotyping of retinal ganglion cells. *J Neurosci* 22:413–427. [Medline](#)
- Marc RE, Kalloniatis M, Jones BW (2005) Excitation mapping with the organic cation AGB2+. *Vis Res* 45:3454–3468. [CrossRef Medline](#)
- Marc RE, Jones BW, Anderson JR, Kinard K, Marshak DW, Wilson JH, Wensel T, Lucas RJ (2007) Neural reprogramming in retinal degeneration. *Invest Ophthalmol Vis Sci* 48:3364–3371. [CrossRef Medline](#)
- Matsumoto M, Yoshimura N, Honda Y (1994) Increased production of transforming growth factor-beta 2 from cultured human retinal pigment

- epithelial cells by photocoagulation. *Invest Ophthalmol Vis Sci* 35:4245–4252. [Medline](#)
- Morgan CM, Schatz H (1989) Atrophic creep of the retinal pigment epithelium after focal macular photocoagulation. *Ophthalmology* 96:96–103. [Medline](#)
- Oliveczky BP, Baccus SA, Meister M (2007) Retinal adaptation to object motion. *Neuron* 56:689–700. [CrossRef Medline](#)
- Osakada F, Ooto S, Akagi T, Mandai M, Akaiki A, Takahashi M (2007) Wnt signaling promotes regeneration in the retina of adult mammals. *J Neurosci* 27:4210–4219. [CrossRef Medline](#)
- Paulus YM, Jain A, Gariano RF, Stanzel BV, Marmor M, Blumenkranz MS, Palanker D (2008) Healing of retinal photocoagulation lesions. *Invest Ophthalmol Vis Sci* 49:5540–5545. [CrossRef Medline](#)
- Paulus YM, Jain A, Nomoto H, Sramek C, Gariano RF, Andersen D, Schuele G, Leung LS, Leng T, Palanker D (2011) Selective retinal therapy with microsecond exposures using a continuous line scanning laser. *Retina* 31:380–388. [CrossRef Medline](#)
- Petrusca D, Grivich MI, Sher A, Field GD, Gauthier JL, Greschner M, Shlens J, Chichilnisky EJ, Litke AM (2007) Identification and characterization of a Y-like primate retinal ganglion cell type. *J Neurosci* 27:11019–11027. [CrossRef Medline](#)
- Pinaud R, Tremere LA, De Weerd P (2006) Plasticity in the visual system: from genes to circuits. New York: Springer.
- Rutledge BK, Wallow IH, Poulsen GL (1993) Sub-pigment epithelial membranes after photocoagulation for diabetic macular edema. *Arch Ophthalmol* 111:608–613. [CrossRef Medline](#)
- Sánchez MC, Luna JD, Barcelona PF, Gramajo AL, Juárez PC, Riera CM, Chiabrando GA (2007) Effect of retinal laser photocoagulation on the activity of metalloproteinases and the alpha(2)-macroglobulin proteolytic state in the vitreous of eyes with proliferative diabetic retinopathy. *Exp Eye Res* 85:644–650. [CrossRef Medline](#)
- Schatz H, Madeira D, McDonald HR, Johnson RN (1991) Progressive enlargement of laser scars following grid laser photocoagulation for diffuse diabetic macular edema. *Arch Ophthalmol* 109:1549–1551. [CrossRef Medline](#)
- Schmidt TM, Do MT, Dacey D, Lucas R, Hattar S, Matynia A (2011) Melanopsin-positive intrinsically photosensitive retinal ganglion cells: from form to function. *J Neurosci* 31:16094–16101. [CrossRef Medline](#)
- Shimura M, Yasuda K, Nakazawa T, Tamai M (2005) Visual dysfunction after panretinal photocoagulation in patients with severe diabetic retinopathy and good vision. *Am J Ophthalmol* 140:8–15. [Medline](#)
- Sinclair SH, Alaniz R, Presti P (1999) Laser treatment of diabetic macular edema: comparison of ETDRS-level treatment with threshold-level treatment by using high-contrast discriminant central visual field testing. *Semin Ophthalmol* 14:214–222. [CrossRef Medline](#)
- Spranger J, Hammes HP, Preissner KT, Schatz H, Pfeiffer AF (2000) Release of the angiogenesis inhibitor angiostatin in patients with proliferative diabetic retinopathy: association with retinal photocoagulation. *Diabetologia* 43:1404–1407. [CrossRef Medline](#)
- Stone W (1950) Ocular injuries in the armed forces. *J Am Med Assoc* 142:151–152. [CrossRef Medline](#)
- Strioph GG, Hart WM Jr, Olk RJ (1988) Modified grid laser photocoagulation for diabetic macular edema. The effect on the central visual field. *Ophthalmology* 95:1673–1679. [Medline](#)
- Wade AR, Wandell BA (2002) Chromatic light adaptation measured using functional magnetic resonance imaging. *J Neurosci* 22:8148–8157. [Medline](#)
- Wandell BA, Smirnakis SM (2009) Plasticity and stability of visual field maps in adult primary visual cortex. *Nat Rev Neurosci* 10:873–884. [CrossRef Medline](#)
- Zwick H, Edsall P, Stuck BE, Wood E, Elliott R, Cheramie R, Hacker H (2008) Laser-induced photoreceptor damage and recovery in the high numerical aperture eye of the garter snake. *Vis Res* 48:486–493. [CrossRef Medline](#)