

Serial Number 09/678,897
Filing Date 4 October 2000
Inventor Normal L. Owsley
 Andrew J. Hull

NOTICE

The above identified patent application is available for licensing. Requests for information should be addressed to:

OFFICE OF NAVAL RESEARCH
DEPARTMENT OF THE NAVY
CODE 00CC
ARLINGTON VA 22217-5660

DISTRIBUTION STATEMENT A
Approved for Public Release
Distribution Unlimited

20010625 194

2
3 DEVICE FOR THE ACQUISITION OF CONTOURED
4 HUMAN BODY SURFACE VIBRATION SIGNALS

5
6 STATEMENT OF GOVERNMENT INTEREST

7 The invention described herein may be manufactured and used
8 by or for the Government of the United States of America for
9 Governmental purposes without the payment of any royalties
10 thereon or therefor.

11
12 BACKGROUND OF THE INVENTION

13 (1) Field of the Invention

14 The present invention relates to a device and a method for
15 the acquisition of contoured human body surface vibration
16 signals.

17 (2) Description of the Prior Art

18 Devices are known in the prior art to detect the contour of
19 shapes. Some of these devices are illustrated in U.S. Patent
20 Nos. 4,700,487 to Bogle; 4,956,924 to Hu; and 5,546,668 to
21 Ahdoot.

22 U.S. Patent No. 5,257,184 to Mushabac illustrates a device
23 for providing a computer with electrically encoded data
24 specifying curvilinear contours of an object. The device
25 comprises a manipulable frame member, componentry for
26 establishing a reference position, a plurality of stylus
27 elements, and means for measuring displacements of the stylus

1 elements along respective axes. The componentry for establishing
2 a reference position includes circuits transmitting an electrical
3 signal encoding a location of a reference point on the frame
4 member to the computer. The stylus elements are each slidably
5 mounted to the frame member for motion along respective axes
6 extending at least partially parallel to one another. The means
7 for measuring or detecting stylus displacements is operatively
8 connected to the stylus elements for transmitting to the computer
9 electrical signals encoding displacements of the stylii along the
10 respective axes. The Mushabac device may be used to determine
11 the contour of a human tooth.

12 U.S. Patent No. 5,957,868 to Case et al. illustrate a
13 surface contour measurement instrument in which back-to-back
14 hydraulically linked pistons are mechanically coupled to contact
15 probes and measurement sensors. The pistons are hydraulically
16 linked by small diameter flexible conduits which enable the
17 contact probes and the measurement sensors to be mounted and
18 moved independently of each other without affecting the ability
19 of the measurement instrument to simultaneously measure a
20 plurality of points on a selected predefined surface, such as a
21 human tooth.

22 23 SUMMARY OF THE INVENTION

24 It is a principal object of the present invention to provide
25 a device for the acquisition of contoured human body surface
26 vibration signals.

1 In accordance with the present invention, a device and a
2 method for acquiring contoured human body surface vibration
3 signals is provided. A flexible array of sensing elements is
4 used to measure displacements of a skin surface as a function of
5 time at multiple points on the human body. A contour estimation
6 component is used to measure the time average displacements of
7 the skin surface at nominal locations of the sensing elements in
8 the flexible array. A computer is used to correct the effect of
9 positional error determined by the contour estimation component
10 from a set of data gathered by the flexible array.

11 Other details of the device of the present invention, as
12 well as other objects and advantages attendant thereto, are set
13 forth in the following detailed description and the accompanying
14 drawings, wherein like reference numerals depict like elements.

15 16 BRIEF DESCRIPTION OF THE DRAWINGS

17 FIG. 1 is a perspective view of a first embodiment of a
18 fixed contour, flexible array component used in the device of the
19 present invention;

20 FIG. 2 illustrates the component of FIG. 1 placed on a human
21 body;

22 FIG. 3 is a perspective view of a mechanical body surface
23 contour estimation component used in the device of the present
24 invention;

25 FIG. 4 illustrates the component of FIG. 3 placed on a human
26 body; and

1 FIG. 5 illustrates an alternative embodiment of a
2 conformable array component wherein the body curvature is
3 accounted for in the shape of a replaceable head unit.
4

5 DESCRIPTION OF THE PREFERRED EMBODIMENT(S)

6 The device for acquiring contoured human body surface
7 vibration signals in accordance with the present invention has
8 three components. The first component is a fixed contour,
9 flexible array component 10, see FIG. 1, containing multiple
10 transducer elements 14 for sensing vibrational displacements of
11 the skin surface at multiple points on the human body. The
12 flexible array component 10 is such that the contoured surface of
13 the body causes individual displacement sensors 14 in the array
14 aperture conforming to the exact variation of the surface
15 topology and producing electrical signals with amplitude in
16 proportion to the magnitude of the time varying displacements
17 about some zero displacement, time averaged reference. The
18 individual sensors 14 have sufficient positional flexibility in a
19 direction perpendicular to the body surface at the sensor 14 to
20 allow the array to conform to an irregular surface and maintain
21 the required level of displacement signal produced by each
22 displacement sensor.

23 The second component of the device is a mechanical body
24 surface contour estimation component 30 for measuring the
25 displacements of the skin at the nominal locations of the
26 elements in the flexible array. The contour estimation component
27 30 estimates and records the locations of the individual

1 displacement sensors in the flexible array component by, first,
2 positioning individual mechanical skin contacts and, second,
3 securing such contacts to record the contact time averaged
4 position.

5 The third component of the device comprises a contour
6 correction component 23. This can be a computer or other device
7 having a signal processing function that converts the estimated
8 contour shape provided by the contour estimation component 30
9 into a table of spatial location correction factors required for
10 the analysis of the acquired displacement sensor output signal
11 data. In the contour correction component 23, the estimated
12 surface contour geometry is then used in the correction of either
13 time delay or, equivalently, phases shifts at individual
14 frequency estimates used in an imaging process involving the time
15 delay alignment and weight summation of space and time sample
16 points on a propagating shear wave vibration front emanating from
17 an assumed focal point inside the body.

18 Referring now to FIG. 1, an embodiment of a flexible array
19 component 10 is illustrated. As shown therein, the flexible
20 array component 10 has a single rigid chassis 12 which provides a
21 stable mechanical frame and a relative spatial coordinate system
22 frame of geometric reference for the individual displacement
23 sensors 14 relative to chassis 12. The individual displacement
24 sensors 14 are such they can be attached securely to the
25 mechanical frame provided by the chassis 12 at either one or two
26 points, as disclosed below.

1 The individual displacement sensors 14 are preferably
2 piezoelectric strain gauge displacement sensors. In this
3 embodiment, sensor 14 is a flexible band 15 with a standoff foot
4 18 joined thereto. Flexible band 15 is fixed at each end to
5 chassis 12. A standoff foot 18 is fixed to the intermediate
6 portion of band 15.

7 In order to maintain piezoelectric flexible bands 15 at
8 optimum efficiency, bands 15 must operate with a low strain.
9 This strain would be exceeded if the flexible array component
10 were positioned on a chest with the bands 15 accommodating all of
11 the variation of different chests. In the first embodiment, this
12 variation is accommodated by thickening those feet 18 that will
13 be positioned on a region of the chest further away from chassis
14 12. The thicknesses of the feet 18 can be provided as a fixed
15 default body surface contour, as an individually tailored
16 contour, or as one of a set of contours determined by
17 measurement. The thickness of each foot is a known quantity and
18 can be incorporated in calculations that depend on the
19 positioning of the sensor relative to the chest. As an
20 alternative embodiment, the flexible array component 10 can have
21 the nominal body surface contour machined into the lower edge of
22 chassis 12. This lower chassis contour would permit the use of
23 feet 18 which are all the same height.

24 The rigid frame 10 contains the electrical leads carrying
25 the signal from each displacement sensor 14. The electrical
26 leads are coalesced into a single flexible cable bundle 22
27 attaching the leads to contour correction and recording

1 electronics 23 for acquisition of the output of the individual
2 sensors 14. In a preferred construction of the array, an
3 enclosure 24 is provided which houses electronic preamplifiers 25
4 for the strain gauge transducer output signals. The electronic
5 preamplifiers 25 can comprise any suitable preamplification means
6 known in the art and should be located as physically close to the
7 sensors 14 as possible. The chassis 12 and the enclosure 24 may
8 be formed as an integral unit if desired.

9 The sensors 14 need to be electrically isolated from the
10 body skin surface 20 because skin 20 may cause both electrical
11 short circuiting and electromagnetic interference. This
12 isolation can be accomplished with rubber strips 26 adhesively
13 joined to chassis 12. The strips 26 physically separate the
14 sensors 14 from the skin and allow only the feet 18 to contact
15 the skin surface 20.

16 As shown in FIG. 2, the flexible array component 10 may be
17 stabilized on the body surface 20 using a light medical single-
18 sided adhesive tape 28.

19 As shown in FIG. 5, an alternative embodiment of a flexible
20 array component 10' can conform to the contoured body surface by
21 constructing the flexible array component chassis 12 in either
22 two or more subchassis 48 which are hinged 50 together. The
23 maximum angle between the units would be constrained so that the
24 internal amplifier electronics could remain rigidly affixed at
25 points only in one subchassis 48a. The position of the hinged
26 chassis units 48b and 48c is fixed with thumb dialed adjustment
27 screws 52a and 52b. A capability for a protractor type angle

1 setting between subchassis would be provided after the flexible
2 array component is located on the body and secured in the
3 contoured configuration with easily enabled set screws or a
4 functional equivalent. The entire multiple head unit 54 could be
5 replaceable.

6 One embodiment of the contour estimation component 30 is
7 illustrated in FIG. 4. As shown therein, the contour estimation
8 component 30 includes a rigid frame 31 that contains multiple
9 equal length mechanical members 32, such as pins, cylinders, wire
10 segments, and the like, that slide easily through holes 34 that
11 are located in the same relative positions in the lower surface
12 of the frame 30 as the geometric centers of feet 18 in the
13 flexible array component 10. With the body surface 20 for which
14 the contour is to be estimated oriented nominally in the
15 horizontal plane below component 30, members 32 are free to slide
16 up and down vertically with gravity such that each member 32
17 makes light contact with the skin surface 20 below hole 34.

18 The contour estimation component 30 is provided with a pin
19 capture mechanism 36 for retaining the positions of members 32 at
20 the position where each member 32 contacts the skin surface 20.
21 The points of contact conform to the surface contour under the
22 holes 34. As shown in FIGS. 3 and 4, this pin capture mechanism
23 36 comprises a hinged cover 38 with a surface 40 that, when swung
24 into the capture position, holds the members 32 in the contour
25 record position when the contour estimation component 30 is
26 removed from the body surface 20. Surface 40 can be soft, spongy
27 rubber or some other retaining material.

1 Having stabilized the members 32 in the contour sensing
2 configuration, a recording mechanism 42 which records the
3 location of the tops of the members 32 and therefore, because the
4 members 32 are of equal length, the sampled skin contour below
5 the contour estimation component 30. The recording mechanism 42
6 can be as simple as a cardboard tab 44 which can slide in behind
7 the tops of the members 32 and upon which a marking device 46 can
8 be used to manually record the relative locations of the tops of
9 all the members 32. The measured contour can then be transferred
10 to the contour correction component 23 by manual entry. Other
11 embodiments of contour estimation component 30 could provide
12 automatic transfer of measurements.

13 It is desirable to achieve a position location estimate at
14 the surface of the body that is accurate to within a nominal 0.1
15 wavelength, λ , referenced to the wavelength of a shear wave
16 propagating in the body and producing the vibrational excitation
17 at the body surface. As an example of this accuracy objective,
18 assume that the wave speed of a body shear wave at a frequency of
19 $f = 400$ Hz is $c = 6$ meters/second. The desired positional
20 accuracy is therefore $= (0.1)\lambda = (0.1)(c/f) = 0.15$ cm.

21 In the spatial focusing image function, hereinafter referred
22 to as focused beamforming, the contour correction component 50
23 concerns the electrical output of the n th of N displacement
24 sensors 14 which is denoted as $x_n(t)$. In a preferred embodiment
25 of the device of the present invention, N is equal to fourteen.

26 The contour correction component 50 has the function of
27 inserting an approximation to the time required for energy

1 emanating from a particular point internal to the body and which
2 point is an element in a volume of such points wherein the energy
3 distribution is to be estimated and recorded in the form of an
4 image. Because body tissue is a dispersive medium in a range of
5 frequency essential to the FB function, the wave speed is a
6 function of the frequency of interest. As such, the contour
7 correction component function is best performed in the frequency
8 domain according to the principles of the Fourier $F(\)$ transform
9 relationship:

$$10 \quad X_{n_CEC}(f) = F\{x_n(t - \tau_n), f\} = X_n(f) \exp(-j2\pi f\tau_n/c(f))$$

11 where $X_n(f)$ is the Fourier transform of the nth sensor output
12 $x_n(t)$, $\tau_n = d_n/c(f)$ is the time delay required to correct for the
13 deviation of the actual contour measured by the CEC from the
14 nominal contour at frequency f .

15 In operation, the contour correction component 23 comprises
16 a processor which is programmed to carry out the various contour
17 correction component functions. For example, the estimated
18 contour shape recorded by the contour estimation component 30 is
19 entered into the contour correction component. This can be done,
20 for example, by scanning in the recording mechanism or manually
21 entering the numbers, or automatically entering the numbers.
22 Thereafter, the contour correction component 23 through its
23 programming converts the estimated contour shape into a table of
24 spatial location correction factors taken directly from the
25 contour estimation correction member displacements, which table
26 is stored in the processor.

1 As energy emanates from a particular point internally of the
2 human body, it will cause the body skin surface 20 to move. The
3 sensors 14 in the FAC 10 detect the movement of the body skin
4 surface 20. The output of each of the sensors 14 is fed to the
5 contour correction component 23.

6 As previously mentioned, the contour correction component 23
7 processes the output of each transducer and inserts a time delay
8 factor to account for the time required for the energy emanating
9 from the internal point to reach the surface of the skin at the
10 location of the transducer including the contour estimation
11 component measure correction . Using this information, it is
12 possible to estimate the internal energy distribution and record
13 it as an image. Details of this aspect are found in U.S. Patent
14 5,727,561 which is hereby incorporated by reference herein.

15 It is apparent that there has been provided in accordance
16 with the present invention a device for the acquisition of
17 contoured human body surface vibration signals which fully
18 satisfies the objects, means, and advantages set forth
19 hereinbefore. While the device of the present invention has been
20 described in the context of specific embodiments thereof, other
21 variations, modifications, and alternatives will become apparent
22 to those skilled in the art after reading the instant disclosure.

23 Therefore, it is intended to embrace such variations,
24 modifications, and alternatives.

2
3 DEVICE FOR THE ACQUISITION OF CONTOURED
4 HUMAN BODY SURFACE VIBRATION SIGNALS

5
6 ABSTRACT OF THE DISCLOSURE

7 In accordance with the present invention, a device for
8 acquiring contoured human body surface vibration signals is
9 provided. The device comprises a first component for sensing the
10 displacements of a skin surface as a function of time at multiple
11 points on the human body, with the first component having a
12 plurality of sensing elements, a second component for measuring
13 time average displacements of the skin surface at nominal
14 locations of the sensing elements in the first component; and a
15 third component for correcting for the effect of positional error
16 from a set of nominal displacement sensor locations.

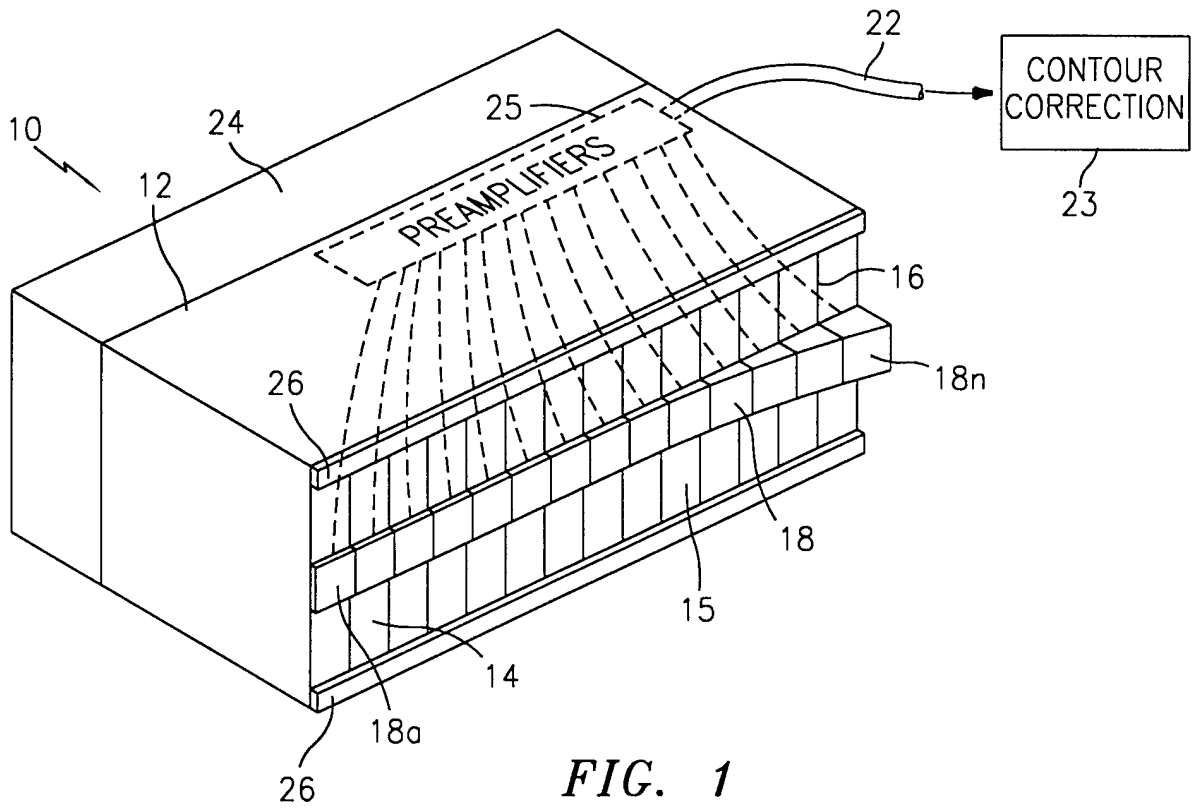


FIG. 1

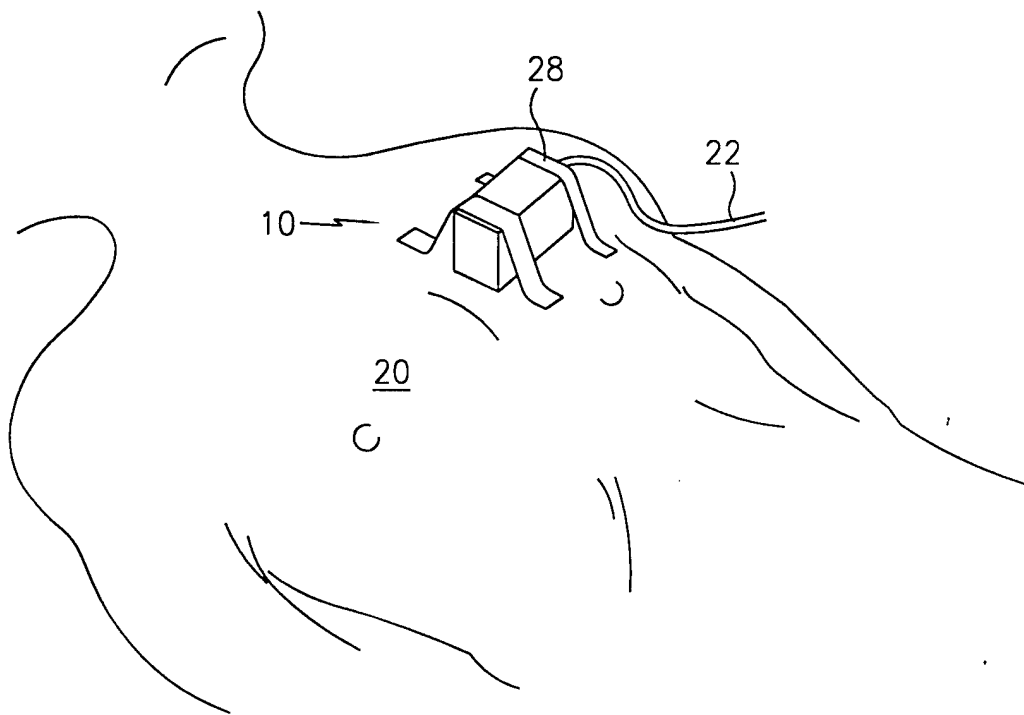


FIG. 2

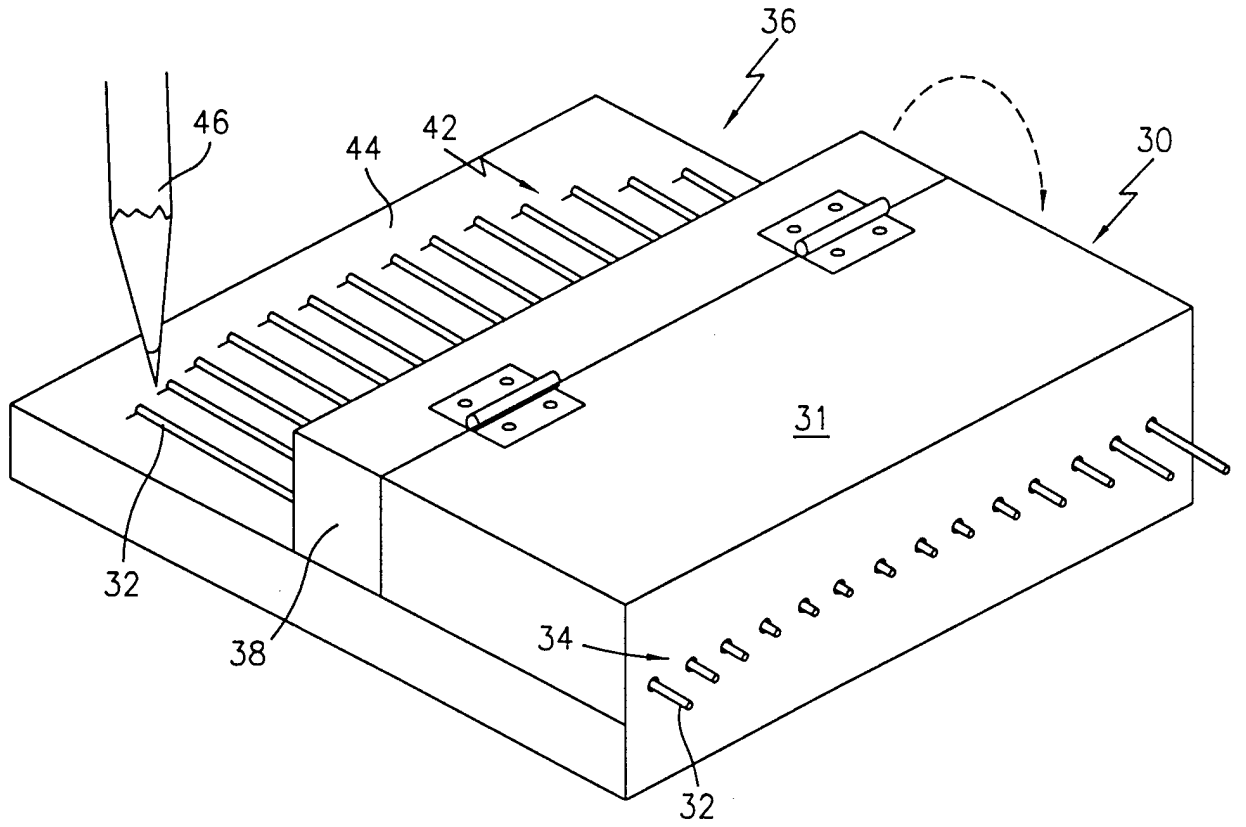


FIG. 3

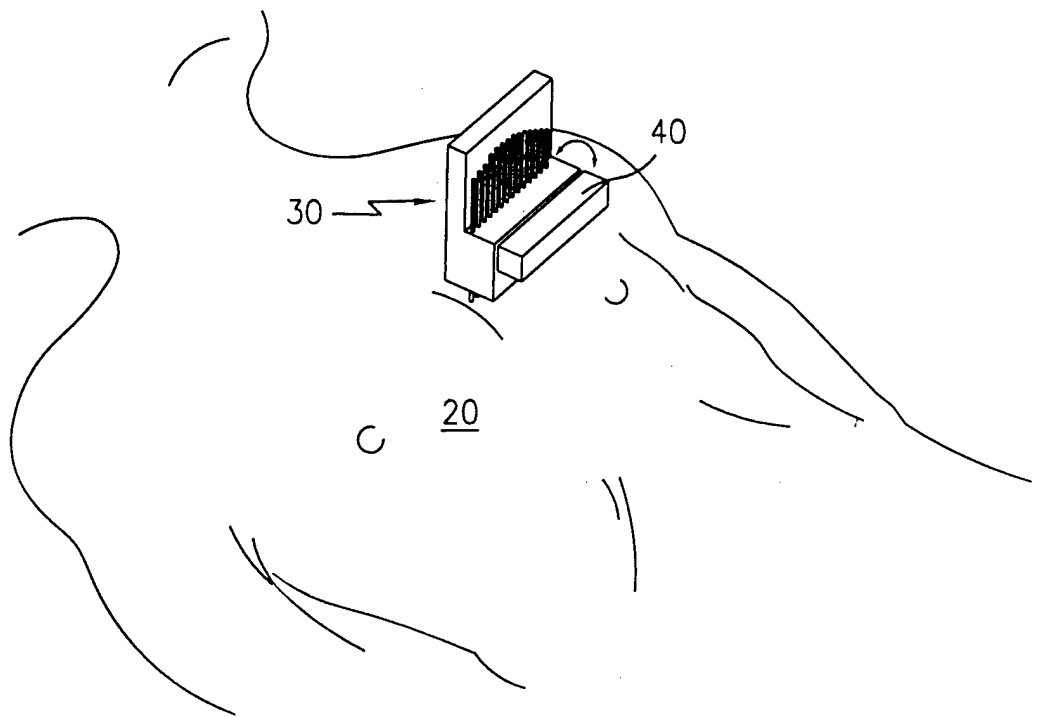


FIG. 4

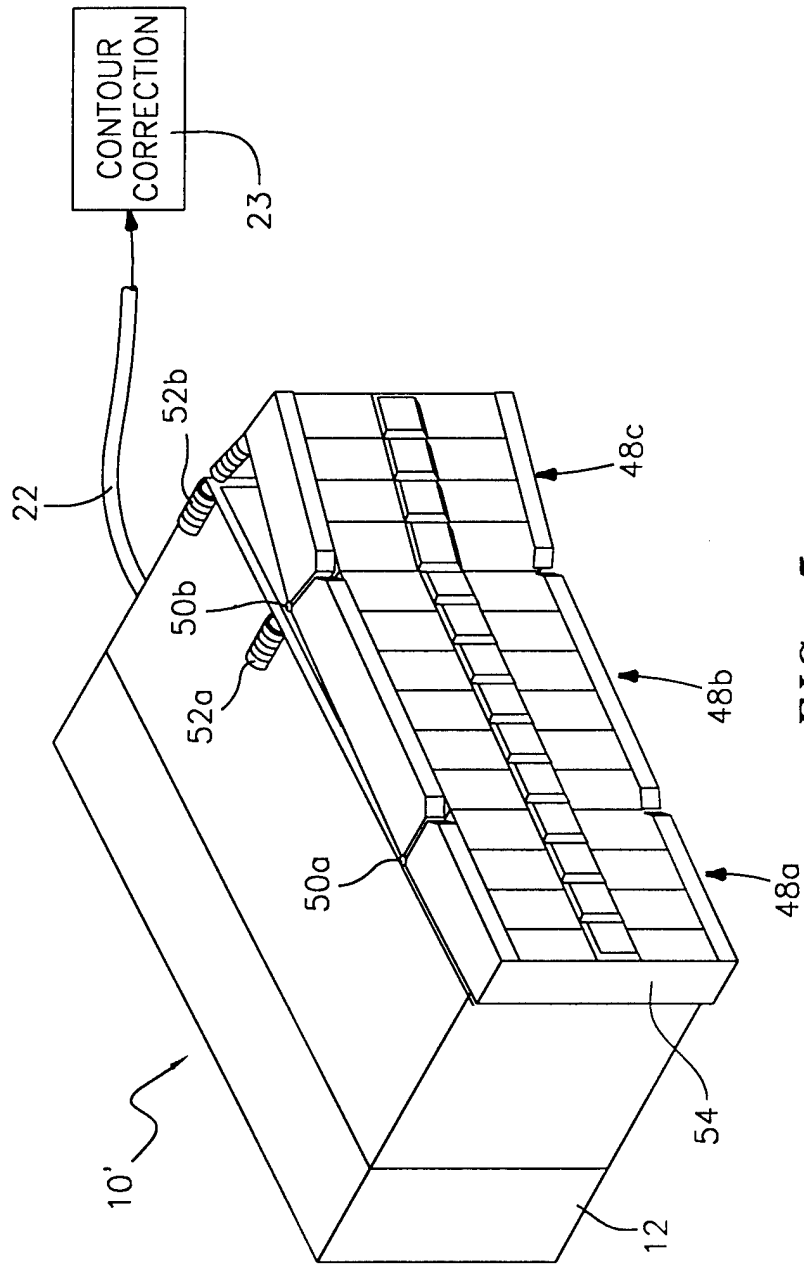


FIG. 5